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Advancements on IoT and AI applied to Pneumology

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Abstract

The objective of this work is the design of a technological platform for remote monitoring of patients with Chronic Obstructive Pulmonary Disease (COPD). The concept of the framework is a breakthrough in the state of medical, scientific and technological art, aimed at engaging patients in the treatment plan and supporting interaction with healthcare professionals. The proposed platform is able to support a new paradigm for the management of patients with COPD, by integrating clinical data and parameters monitored in daily life using Artificial Intelligence algorithms. Therefore, the doctor is provided with a dynamic picture of the disease and its impact on lifestyle and vice versa, and can thus plan more personalized diagnostics, therapeutics, and social interventions. This strategy allows for a more effective organization of access to outpatient care and therefore a reduction of emergencies and hospitalizations because exacerbations of the disease can be better prevented and monitored. Hence, it can result in improvements in patients' quality of life and lower costs for the healthcare system.

Keywords: Internet of Things, healthcare, machine learning, intelligible analytics, statistical validation, cyber-security

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1. Introduction

In the healthcare context, Chronic Obstructive Pulmonary Disease (COPD) affects about 5-10% of the adult population, although prevalence as low as 0.2% and as high as 37% has been reported, depending on country, population, COPD diagnosis and classification methods [1]. COPD is an important cause of mortality, comorbidity and social impact. The remote and continuous monitoring of treatments, as well as the collection of vital parameters (such as heart rate, blood oxygenation, sleep and patient movement), are necessary to allow for immediate and punctual medical and social interventions, to reduce short- and long-term clinical consequences of the disease, and, in general terms, to improve the quality of life of patients, families and population [2, 3].

In this contribution, we introduce a novel concept for an innovative platform, called Pneualytics, to monitor and manage patients with COPD. Pneualytics can be adopted by healthcare systems, clinical centers and Pneumology departments and clinics. Platforms which includes patients' devices to retrieve data about patients' routine are not widely adopted yet, but it is assumed that, by 2025, approximately 75.44 billion of IoT devices will be online [4].

The platform is built upon collection and integration of IoT data and clinical data (available from inpatient and outpatient visits) and the analysis and aggregation of such data using artificial intelligence (AI) algorithms.

This new concept of patient monitoring requires the inclusion of new services and technologies that will need to be developed and optimized for efficacy and usability. Such technologies will contribute to a more effective patient management and therefore will support healthcare providers in defining strategies to offer care for chronic respiratory pathology. To this end, our platform not only involves a thorough patient monitoring via a set of gold-standard devices, but it also seeks to minimize the invasiveness of the data collection by including a more comfortable wearable device like a smartwatch.

The remaining of the paper is structured as follows: Section 2 reports an overview of the current healthcare scenario in terms of technologies and investments, giving a clear context to the objectives of the work. Section 3 reports the current IoT devices and machine learning approaches adopted in the healthcare context. Section 4 describes in detail the different components of the proposed framework and considerations regarding security and privacy. Section 5 details the adopted explainable AI (XAI) algorithm,

38 i.e., the Logic Learning Machine (LLM), while Section 6 introduces a first
39 experimental study involving the integration of several devices involved in
40 PneuLytics platform and Section 7 discusses the effect of adversarial attacks
41 against the proposed XAI solution. Then, Section 8 reports a preliminary
42 study on smartwatch data. Finally, Section 9 concludes the paper and dis-
43 cusses possible next steps on the topic.

44 **2. IoT in healthcare scenarios**

45 Healthcare is a fertile ground for innovation through digital technology,
46 which has the potential to make the health system sustainable. For example,
47 Italian spending on health, even if population aging and increased life ex-
48 pectancy increase the need for care applications, is still decidedly lower than
49 that of other countries [5].

50 In recent years, digital healthcare has continued its positive development
51 trend. However, the expenditure commitment is not sufficient to bridge the
52 overall delay in the digitization of the sector yet. Federsanità, the Italian in-
53 stitutional entity that organizes local health authorities and hospitals, points
54 out that *the primary care management systems (which also include the In-*
55 *dividual Health Card) are present in almost all of the General Medicine and*
56 *Pediatricians' offices, but they are not integrated with hospital information*
57 *systems, in which the spread of electronic medical records is still very lim-*
58 *ited. In both areas there is also a considerable heterogeneity of the present*
59 *IT solutions.*

60 In particular, the technological paradigms enabling proximity and terri-
61 torial assistance logic are strictly related to the use of IoT and wearables
62 that enable remote monitoring and remote assistance services, as reported
63 in [6, 7, 8]. Globally, we are witnessing a rapid increase in the use of connected
64 and wearable devices both to improve the care of patients within hospitals
65 and to speed up recovery times at the patient's home, through continuous
66 remote monitoring of conditions and vital parameters or to delay the transi-
67 tion from independent living to assisted living [9]. The digital transformation
68 is enabled by some elements, including data security, big data, and AI. In
69 particular, the data security issue is closely related to the usage, transmis-
70 sion and sharing of health data. This topic is particularly felt in public and
71 industrial sectors, because of recent recommendations introduced by the EU
72 General Data Protection Regulation (GDPR) policies about personal data.

73 *2.1. Digital transformation in Pneualytics*

74 All these crucial elements are incorporated in the Pneualytics framework
75 by combining IoT and wearable technologies with innovative data processing
76 and AI algorithms, to extract sensitive, dynamic information. AI can be
77 used to generate predictive models of the patients' health status. Instead,
78 data collection from personal devices and sensors can be used to monitor
79 the patients' vital parameters, generate alerts, and keep a detailed record
80 of patients' history and state of health. The concept originates from the
81 paradigm of the patient's centrality within the healthcare processes and the
82 need to adopt innovative technologies to facilitate daily monitoring of health
83 conditions.

84 The idea is to renovate the whole patients' journey experience by inte-
85 grating conventional clinical procedures with the innovation brought by new
86 technologies, which means combine daily monitoring data with data from
87 an optimized hospital or extra-hospital healthcare. Specifically, relevant
88 monitoring data in respiratory pathologies include vital parameters, phys-
89 ical activity and pharmacological compliance. Some clinical trials, although
90 conducted on limited cases, have shown that tools for the administration of
91 therapy integrated with ICT platforms are able to improve adherence to the
92 treatment and reduce hospital admissions of patients suffering from COPD
93 [10].

94 Clearly, personalized home therapy, constant monitoring of COPD evolu-
95 tion and prevention of possible exacerbations represent fundamental aspects
96 in future clinical practice.

97 *2.2. Aim and Scope*

98 The main objective of the proposed framework is to create a hardware
99 and software platform able to provide improvement of:

- 100 ● treatment and assistance related to respiratory pathologies, supporting
101 the definition of follow-up plans and promoting personal care;
- 102 ● effectiveness of therapy as related to the administration of drugs through
103 non-intrusive monitoring of the patient's behavior and adherence to
104 therapy;
- 105 ● clinical practice, making it possible to customize and optimize the stag-
106 ing of diseases and the areas of intervention over time.

107 The innovation of this platform can ease the workflow in hospital and
108 medical contexts, especially considering that the resources allocated to pub-
109 lic health are decreasing concerning a rapidly increasing demand. In the long
110 term, the proposed technological solution has the potential to generate sig-
111 nificant developments in terms of: i) new business opportunities related to
112 infrastructures for remote monitoring, technologies and devices for advanced
113 biomedical sensors; ii) new generation communication technologies, AI solu-
114 tions for data processing and clinical decision support; and iii) improvement
115 of the quality of care, medical treatment of COPD, and patient outcomes.

116 **3. Survey of medical IoT platforms and machine learning approaches**

117 *3.1. Internet of Things*

118 The state of the art of medical IoT platforms shows a variety of tools
119 and interfaces, as briefly summarized below. For our aim, our focus is on
120 open source approaches, highlighting progresses will lead to the proposed
121 framework. Widespread use of open source health platforms and sensors
122 has led to the development of simple, inexpensive and easy to use biometric
123 devices, thus, these technologies impact not only from a medical point of
124 view, but also in terms of business models for SMEs.

125 For instance, Bitalino¹ is a popular open source biomedical development
126 platform that has a variety of biometric sensors. These sensors include an
127 ElectroMyoGraphic sensor (EMG), a sensor for ElectroCardioGraphy (ECG),
128 a LUX sensor (to monitor blood volume pulse data), an Electro-Dermal Ac-
129 tivity (EDA), and an accelerometer sensor (for dynamic and biomechanical
130 motion analysis). In addition, the platform offers an Atmega328 microcon-
131 troller for processing sensor readings and a Bluetooth module for wireless
132 communication. The LUX sensor can be used together with a light source to
133 monitor blood pulse data, while the accelerometer can be used in dynamic
134 and biomechanical motion analysis. The heterogeneity of Bitalino sensors is
135 a good reference for Pneualytics, even if we intend to specialize our analysis
136 on a specific pathology.

137 Similar considerations apply to E-Health², an open source sensor platform

¹More information are available at the following address: <http://www.bitalino.com>, accessed on November 2023.

²More information are available at the following address: <https://www.postscapes.com/open-source-e-health-sensor-platform>, accessed on November 2023.

138 that offers a wide range of features for detecting biological signals for open
139 source hardware platforms. E-Health is one of the few, perhaps the only, IoT
140 health platforms compatible with both the Arduino and Raspberry Pi archi-
141 tectures. E-Health focuses mainly on heart disease, creating many dedicated
142 solutions e.g. ECG devices. Several open-source ECG sensors are available:
143 they are not invasive and can be used comfortably at home. Their function-
144 ing is based on different mechanisms, for example, on photoplethysmography,
145 which is frequently used in wearable devices, including fitness trackers.

146 Ticuro³ is a closed system for the user and acts as a collector of a vari-
147 ety of commercial sensors/devices (to be purchased separately) as well as a
148 tele-consultation platform. The ARM⁴ and Kaa⁵ architectures allow health-
149 care system integrators to establish connectivity between heterogeneous IoT
150 devices and implement intelligent features in the devices themselves and the
151 related software systems. Regarding the IoT protocols related to network
152 connection (e.g., with MQTT and CoAP protocols), these architectures are
153 of interest to Pneulytics, but still inadequate in terms of artificial intelligence
154 engine.

155 An open architecture to developers and manufacturers of sensors and
156 devices, as Mysignals⁶, is particularly suited for building Pneulytics because
157 of its flexibility.

158 *3.2. Adopted IoT devices*

159 Our research focuses on examining the adoption of smart health solu-
160 tions to monitor various personal and environmental variables, particularly
161 those related to quality of life and wellbeing. One key aspect we explore
162 is Indoor Environmental Quality (IEQ), collecting different measurements
163 to assess the indoor environment quality. To achieve this goal, we set up
164 an intelligent monitoring system capable of observing, capturing, and pro-
165 cessing environmental and body measurements. The integration of Internet

³More information are available at the following address: <https://www.reply.com/ticuro-reply>, accessed on November 2023.

⁴More information are available at the following address: <https://www.arm.com/glossary/medical-iot>, accessed on November 2023.

⁵More information are available at the following address: <https://www.kaaproject.org/healthcare>, accessed on November 2023.

⁶More information are available at the following address: <http://www.my-signals.com>, accessed on November 2023.

166 of Things sensors facilitates the seamless retrieval and exchange of data,
167 thanks to the interconnected relationship between the sensors and a shared
168 data storage platform.

169 Regarding the IoT sensors adopted for the platform, our emphasis has
170 been on accessing the raw data captured by these sensors. Specifically, we
171 have focused on two categories: wearable devices, which are connected and
172 actively managed by the patients themselves, and environmental devices that
173 are physically installed in the patients' homes.

174 Concerning wearable devices, the adoption of the H&S cloud platform en-
175 ables us to access aggregated monitoring data and grant authorized access to
176 end-users. Particularly, H&S offers services through its proprietary platform,
177 HealthPlatform v3 - medical device CE IIA. Such platform is equipped with
178 a data center certified ISO 27001 and ISO 13485. The data management
179 activities adhere to GDPR regulations and comply with CE Medical Device
180 5/2020 standards.

181 Among the available devices, our choice includes (i) a dedicated smart-
182 phone with the proprietary app (Mhealth, certified IIA class) running on it,
183 (ii) an electrocardiogram (ECG) also providing day/night movement moni-
184 toring, (iii) a pulse meter providing oximetry monitoring, (iv) a weight scale,
185 and (v) a sphygmomanometer for blood pressure monitoring.

186 In our tests, we also included surveys for the patients, such as the COPD
187 assessment test.

188 Instead, regarding environmental monitoring activities, for each environ-
189 ment (home, office, etc.), we included in our setup (i) a central node receiving
190 data from the other nodes, (ii) a physical device combining multiple sensors,
191 (iii) a set of modules demanded to provide connectivity to analog equipment
192 like windows or radiators, and, optionally, (iv) an outdoor weather station.

193 Particularly, while the central node is represented by a Raspberry Pi 4
194 Model B, following sensors types and models have been considered:

- 195 • temperature and humidity (Sparkfun, SI7021)
- 196 • atmospheric pressure (AZ Delivery, BMP180)
- 197 • air speed (Modern Device, Wind Sensor Rev. C)
- 198 • CO measurement (Sparkfun, MQ7)
- 199 • CO2 measurement (Sparkfun, CSS811)

- 200 • formaldehyde concentration (Seedstudio, Grove HCHO)
- 201 • concentration of fine dust (Honeywell, HPMA115S0-XXX)
- 202 • redundancy (Bosch, BME680)
- 203 • weather station (PCE Italia, PCE FWS 20)

204 To conclude, regarding analog equipment monitoring, we adopted AZDe-
205 livery, ESP8266 plus ESP-01 and DHT22 plus AM2302.

206 With the sensors we've implemented, we can observe and process a vari-
207 ety of metrics related to both the patients' conditions and the surrounding
208 environment. Moreover, through AI methodologies, the aggregation and pro-
209 cessing of data not only allow for the integration of information from diverse
210 components for a comprehensive analysis but also enable the identification
211 of potential relationships among the data.

212 3.3. Smartwatch-based explainable data analytics

213 Nowadays, smartwatches are becoming very popular in smart health mon-
214 itoring, being able to measure multiple indicators inherent to different do-
215 mains, such as cardiovascular and respiratory health, physical activity sleep
216 habits, all in scaled-down devices that can be comfortably wrist-worn by
217 people, without being invasive nor requiring dedicated training [11]. Con-
218 sequently, these wearables are an important data source for healthcare XAI
219 applications, designing transparent models that can provide clinical decision-
220 making support to users, either these are clinicians in making diagnosis,
221 prognosis or planning therapies. The patients themselves may become more
222 aware of their health status as well.

223 3.4. Artificial Intelligence

224 Noticeably, none of these platforms integrates AI solutions, whereas Pneu-
225 lytics, by using AI on integrated patients' clinical data (e.g., spirometry,
226 blood analysis) and sensor data, is able to support personalized healthcare.

227 The adoption of statistical methods in medical scenarios is widespread.
228 In recent years, with the evolution of big data, the importance of AI in health
229 scenario has increased. For example, [12] proposed to extract rules for pleural
230 mesothelioma diagnosis. Malignant Pleural Mesothelioma (MPM) is a rare
231 highly fatal tumor where the correct diagnosis of MPM is often hampered

232 by the presence of atypical clinical symptoms: these may cause misdiagno-
233 sis with either other malignancies (especially adenocarcinomas) or benign
234 inflammatory or infectious diseases (BD) causing pleurisies. Cytological Ex-
235 amination (CE) may allow to identify malignant cells, but sometimes a very
236 high false negative proportion may be encountered due to the high prevalence
237 of non-neoplastic cells. Moreover, in most cases a positive result from CE ex-
238 amination only does not allow to distinguish MPM from other malignancies
239 [13]. Another interesting work is focused on the extraction of a simplified gene
240 expression signature for neuroblastoma prognosis [14]. [15] instead proposed
241 a convolutional neural network (CNN) algorithm in order to verify if deep
242 learning could detect the COPD stage and predict Acute Respiratory Disease
243 (ARD) events and mortality in smokers by using a training dataset composed
244 by more or less 8000 patients. The results are interesting since the approach
245 shows that CNN is able to identify and predict individuals with COPD. [16]
246 implemented a decision tree forest classifier able to predict COPD based on
247 symptoms by monitoring 16 patients for six months. Another approach is
248 adopted in [17], where AI is used to analyze X-Ray dataset in order to recog-
249 nize and locate the common disease patterns. In [18], authors implemented
250 a recurrent neural networks (RNN) on 260K patients to predict diagnosis by
251 performing a multilabel prediction. Artificial intelligence is also applied to
252 predict the Parkinson, with interesting results [19].

253 4. Pneulytics framework

254 4.1. Context and approach

255 COPD is a common, preventable and treatable disease characterized by
256 persistent respiratory symptoms (dyspnea, cough, expectoration) and airway
257 obstruction due to lung damage induced for example by cigarette smoking
258 and environmental pollutants. The course of COPD is generally progressive
259 and is characterized by recurrent exacerbations and by the presence of con-
260 current conditions (e.g. cardiovascular pathology) that increase morbidity
261 and mortality (estimated as the 3rd cause of death in 2020 by the WHO⁷).

262 COPD patients typically get benefit from topically administered drugs to
263 reduce exacerbations and to relieve symptoms, reducing exercise intolerance

⁷More information is available at the following address: https://www.who.int/healthinfo/global_burden_disease/projections/en/, accessed on November 2023.

264 and increasing pulmonary function and life quality. There is still a clear
265 discrepancy between patients' outcomes in clinical research and outcomes in
266 real life due to poor adherence to treatments and wrong use of drug inhalers
267 [20]. The number of critical errors in the use of inhalers is associated with
268 increased risk of COPD exacerbations and the combination of poor adherence
269 and misuse of inhalers may increase the risk of death up to three times
270 [20, 21].

271 Technological improvements have recently led to the creation of new de-
272 vices that allow remote monitoring [22, 23], patient engagement and remote
273 interaction with the healthcare providers.

274 Smart inhalers are capable to record and digitize key aspects of care, such
275 as drug intake and inhaler mode of use (inspiratory peak flow, duration of
276 the inspiratory phase, inhaler's orientation). Thanks to these smart inhalers,
277 doctors are able to acquire information on adherence to the treatment and
278 on proper/improper use of the inhaler.

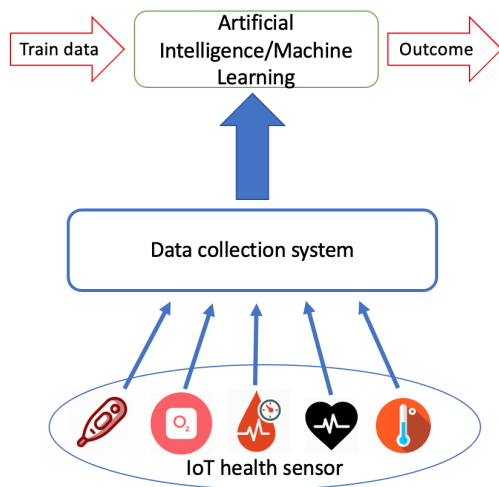


Figure 1: The concept of the PneuLytics platform

279 Unfortunately, the use of these devices is not widespread and currently
280 this type of intervention is highly managed by a direct doctor-patient (or ser-
281 vice center-patient) relationship, thus missing the opportunity to implement
282 continuous monitoring, multivariate/multimodal clinical evaluation, remote
283 monitoring, remote consultation on large patient cohorts. Moreover, the ac-
284 cessibility to the data recorded by the devices is perhaps one of the most
285 important aspects regarding data integration.

286 The PneuLytics framework aims to contribute by addressing these issues
287 and by increasing patients' involvement in the treatment plan and support
288 interaction (including remote interaction) with the healthcare providers. The
289 prototype hardware architecture for the collection and management of data,
290 obtained with different IoT devices, is based on the available types of sig-
291 nals and communication protocols available, their size and, consequently, the
292 processing capacity necessary for the correct application of the specific AI
293 algorithms.

294 The proposed technological platform is composed of different technologies
295 and algorithms, as the conceptual scheme in Fig. 1 illustrates.

296 Candidate patients will be equipped with wearable sensors that monitor
297 relevant biomedical parameters both indoor and outdoor throughout their
298 daily life. Additional sensors will be installed in the patients' home envi-
299 ronment to detect relevant environmental parameters, such as air quality,
300 humidity, temperature and pressure, and a sleep quality monitoring system.
301 In the outdoor environment, contextual information related to the level and
302 type of patient's activity will be collected by using consumer devices, such
303 as smartphones or smartwatches.

304 Using ad-hoc AI algorithms, the platform will monitor functional and
305 physiological parameters, such as blood oxygenation, heart rate, physical
306 activity, sleep and lung function, as well as adherence to therapy through
307 smart inhalers. The data collected will be also exploited to develop predictive
308 models that will be useful to define follow-up plans and interventions.

309 *4.2. Personal health records*

310 The system will integrate all the data from sensors and personal devices
311 with the medical history and clinical data, as available from the hospital
312 databases and will be able, in future developments, to interact directly with
313 existing systems of Personal Health Records and with information extracted
314 from biomedical images recorded in the hospital information systems and
315 Picture Archiving and Communication System (PACS).

316 Two aspects need to be addressed here: on one hand, a management
317 and decision support system has to be designed, where all the internal and
318 external heterogeneous data are organized and accessed. On the other hand,
319 analysis techniques from computer vision and graphics (some of them based
320 on AI approaches) may be applied in order to characterize and measure
321 specific areas of biomedical images and 3D reconstructed models that are
322 useful for the diagnosis, monitoring and follow-up of COPD. Annotation

323 methods may also be used to code such extracted information, index 2D
324 and 3D resources in compliance with semantic web paradigms, and finally
325 integrated into Pnelytics platform. A similar approach has been applied to
326 musculoskeletal pathologies in [24, 25].

327 *4.3. Cyber-security and privacy considerations*

328 IoT devices provide the ability to automate and enhance people’s daily
329 lives. Being a pervasive technology embedded in critical locations, the IoT
330 phenomenon is often coupled with privacy issues: as such sensors often pro-
331 cess sensitive information, security becomes a very critical topic. In particu-
332 lar, if IoT sensors are adopted to monitor and control the health parameters
333 of patients, data security becomes extremely critical due to potential expo-
334 sure to privacy leaks. For the scope of the proposed work, patients’ health
335 parameters are managed and manipulated through IT systems. For this
336 reason, it is crucial to guarantee appropriate security and privacy, especially
337 because of potential cyber-attacks able to steal, retrieve or infer clinical data.

338 In order to guarantee user data privacy, different data anonymization
339 techniques are available, also considering ethical aspects of sensitive data
340 management. Indeed, in literature, several anonymization algorithms are
341 found, while some of them exploit different techniques that make the data
342 difficult to de-anonymize [26, 27, 28, 29]. Instead, in the context of data
343 re-identification and de-anonymization, machine learning methods can be
344 adopted. From one side, a well-known and “classic” (unsupervised) cluster-
345 ing approach to data privacy is k-anonymity [30, 31, 32, 33]. In this case,
346 the k-mean algorithm can be used for different applications: [34] adopts it to
347 de-anonymize and extract geo-localization data from mobility traces, while
348 [35] makes use of the k-mean to extract potentially sensitive information
349 from social networks. Similarly, [36] adopts the k-mean to profile Facebook
350 users, analyzing the interaction of their account, in terms of reactions, likes,
351 or other social interactions. [37] makes instead use of the k-mean algorithm
352 to preserve privacy when datasets are composed of different attributes, while
353 [38] proposes a variant of the k-means algorithm to preserve the privacy of
354 information by using as input encoded data. [39] also extends the k-means,
355 by proposing M-Shuffle, a novel algorithm, based on k-means, to avoid infor-
356 mation de-anonymization. By considering the same approach, a clustering
357 approach based on k-means could be adopted to theorize a privacy breaking
358 attack, aimed to reveal potentially sensitive information from anonymized
359 data.

360 From another side, a different and more advanced (unsupervised) method
361 could be inherited from the topic of the neural network, in order to conceptu-
362 alize a novel attack against data privacy. Particularly, Restricted Boltzmann
363 Machines (RBM) could potentially be used for data breaking purposes. Even
364 in this case, RBM is nowadays adopted for different scopes: for instance, for
365 simulations [40], to identify multivariate geochemical anomalies [41], or to
366 categorize users [42]. In addition, they could be adopted similarly to its
367 usage for user categorization: while known applications focus on the cate-
368 gorizations of users, for instance for marketing purposes (e.g. if a user U1
369 bought A, and previous users also bought B, hence, U1 may also be inter-
370 ested to purchase B), it is potentially possible to adopt RBM to categorize
371 users due to their belonging of categories including other (not-anonymized)
372 users. This is accomplished in RBM by relating each user to the belonging
373 of one or more hidden features.

374 Instead, regarding security of Internet of Things systems, devices may
375 communicate through standard networks, such as Wi-Fi or ethernet, or build
376 a dedicated network to communicate with other sensors, called Wireless Sen-
377 sor Network (WSN). In this regard, a real standard is not commonly adopted
378 yet [43]. Currently, there are different protocols providing communication
379 between sensors: some of them are based on pre-existing protocols (Wi-Fi,
380 6LowPan, MQTT or LoRa), while others provide the creation of new ad-hoc
381 infrastructures (ZigBee, Z-Wave). Although different IoT protocols may be
382 adopted, IoT devices are often exposed to security attacks since the data
383 exchanged in this context are sensitive. Being exchanged information ex-
384 tremely sensitive due to the nature of devices and networks, the security
385 about IoT devices and networks should be investigated in order to identify
386 possible vulnerabilities and to protect the IoT context from them.

387 In order to protect IoT devices and network, well-known [44] and inno-
388 vative [45, 46] attacks against IoT ad-hoc communication protocol are in-
389 vestigated to protect sensitive information from malicious purposes. Also,
390 [47] considers hardware and software limitations of IoT systems, by creating
391 a taxonomy of weaknesses. Instead, [48] analyzes the security of IoT net-
392 works by identifying crucial aspects related to common vulnerabilities, while
393 [49] focuses on the security challenges to be addressed in the IoT field, also
394 proposing protection solutions. Similarly, [50] focuses on security issues on
395 environments such as healthcare, smart home or vehicles management.

396 In the context of this work, security and privacy aspects affecting IoT
397 devices and networks need to be analyzed in detail to avoid possible loss of

398 sensitive information and to ensure a secure exchange of information between
399 the devices and the platform developed.

400 5. The adopted explainable AI approach

401 The data collected from the mentioned set of sensors is analysed via
402 the lens of *explainable Artificial Intelligence (XAI)*. This term refers to a
403 broad category of techniques aimed at providing intelligible interpretations
404 to machine learning-based decisions [51], thus allowing anyone to enter their
405 logic and increase trust in the knowledge inferred: one of the main XAI
406 categorizations distinguishes between post-hoc XAI, where interpretations
407 are provided to a previously trained black-box model, and transparent-by-
408 design XAI, where the model making predictions is natively explainable. In
409 this work, our focus is on the latter group, and in particular on rule-based
410 models [52].

411 The setting considered here is that of a supervised machine learning clas-
412 sification task. The dataset is represented as the set $\mathcal{X} \times \mathcal{Y} = \{(\mathbf{x}_i, y_i)\}_{i=1}^N$
413 where $\mathbf{x}_i \in \mathcal{X} \subseteq \mathbb{R}$ is the set of input measurements for sample i and
414 $y_i \in \mathcal{Y} = 0, \dots, K - 1$ is a label associated to it. The objective is to learn
415 the best function $f : \mathcal{X} \rightarrow \mathcal{Y}$ able to separate the input points according
416 to their labels. In our study, the derivation of f is made through a specific
417 rule-based model, called Logic Learning Machine (LLM) [53], which is the
418 fast implementation of Switching Neural Networks.

419 In the LLM algorithm, the classification function f is learnt through three
420 steps, as described in [53]. In the first phase (*discretization* and *latticeization*)
421 each input is converted into a string of binary data in a proper Boolean lat-
422 tice, using the inverse only-one code binarization. All the generated strings
423 are then concatenated into a single large string per each sample. In the
424 second phase (*shadow clustering*) a set of binary structures, namely the *im-*
425 *plicants*, are individuated, allowing the identification of groups of samples
426 associated to a specific class. During the third phase (*rule generation*), all
427 implicants are converted back to the original feature space, forming a collec-
428 tion of conditions, and eventually are combined into a set of if-then rules.

429 The LLM classifier is thus described by a set of m intelligible rules $r_k, k =$
430 $1, \dots, m$, of the type **if** (*premise*) **then** (*consequence*), where (*premise*) is the
431 logical conjunction (AND, \wedge) of d_k conditions c_{l_k} , with $l_k = 1_k, \dots, d_k$,
432 and (*consequence*) provides the class label \hat{y} associated to the rule.

433 A condition c_{l_k} of rule r_k can have one of the following forms:

- 434 1. $x_{\pi(l)} > \lambda$
 435 2. $x_{\pi(l)} \leq \mu$
 436 3. $\lambda < x_{\pi(l)} \leq \mu$

437 being $\lambda, \mu \in \mathcal{X}$ and $\pi : \mathbb{N} \rightarrow \mathbb{N}$ denotes the permutation of the indexes
 438 of feature vector \mathbf{x} that maps rule l_k -th condition with the corresponding
 439 feature component.

440 For each rule generated by the model, a confusion matrix can be com-
 441 puted, showing true and false positives, $TP(r_k)$ and $FP(r_k)$, defined as the
 442 number of examples (\mathbf{x}_i, y_i) which satisfy all the conditions in rule r_k with
 443 $\hat{y} = y_i$ and $\hat{y} \neq y_i$, respectively, and true and false negatives, $TN(r_k)$ and
 444 $FN(r_k)$, being the number of examples (\mathbf{x}_i, y_i) which do not satisfy at least
 445 one condition in rule r_k , with $\hat{y} \neq y_i$ and $\hat{y} = y_i$, respectively. Useful
 446 quantities can be derived from the confusion matrix, such as the covering
 447 $C(r_k) = \frac{TP(r_k)}{TP(r_k)+FN(r_k)}$ and the error $E(r_k) = \frac{FP(r_k)}{FP(r_k)+TN(r_k)}$. The covering
 448 may also be adopted as a measures of relevance for a rule r_k ; as a matter of
 449 fact, the larger is the covering, the higher is the generality and the correctness
 450 of the corresponding rule.

451 5.1. Feature and value ranking

452 Some preliminary results, reported in [54], have shown that the LLM is
 453 more performing than most of the known learning techniques of the same
 454 kind. Moreover, the computational complexity of the method is kept low
 455 thanks to the adoption of proper greedy procedures. Therefore the LLM
 456 model may be adopted also in the analysis of large datasets (i.e. having
 457 many inputs and/or examples). Notice that the LLM approach presents
 458 further interesting features such as the possibility of dealing with categorical
 459 inputs and the determination of the relevance of each variable. This last
 460 property allows the identification and elimination of redundant attributes.

461 *Feature ranking (FR)* deals with ranking the input variables based on their
 462 influence in determining the model's prediction, as calculated by an impor-
 463 tance measure. The starting point is to compute a relevance value $R(c_{l_k})$ for
 464 a single condition, by measuring the difference in the rule error by including
 465 and excluding that condition, i.e., it holds that $R(c_{l_k}) = (E(r'_k) - E(r_k))C(r_k)$,
 466 where r'_k denotes the rule without condition c_{l_k} . As previously stated, each
 467 condition c_{l_k} refers to a specific input variable $x_{\pi(l)}$ and is satisfied by some
 468 values $\nu_{x_{\pi(l)}} \in \mathcal{X}$. The importance $R_\nu(\nu_{x_{\pi(l)}})$ of these values is given by:

$$R_\nu(\nu_{x_{\pi(l)}}) = 1 - \prod_k (1 - R(c_{l_k})) \quad (1)$$

469 where the product is over rules r_k that include a condition c_{l_k} verified
 470 when $x_{\pi(l)} = \nu_{x_{\pi(l)}}$. Taking values in $[0, 1]$, it can be thought as the probability
 471 that value $\nu_{x_{\pi(l)}}$ occurs to predict \hat{y} . A ranking in descending order of R_ν for
 472 all possible intervals $\nu_{x_{\pi(\cdot)}}$ is referred to as *Value Ranking (VR)*.

473 Also, by aggregating the relevances for all different intervals $\nu_{x_{\pi(\cdot)}}$ of the
 474 variable of interest, an overall measure of its importance can be computed.
 475 Finally, the descending ordering of these importance metrics generates the
 476 feature ranking.

477 5.2. Classification scoring

478 In the inference phase, when applied to a generic input \mathbf{x} , the LLM model
 479 computes a score for each output class. Let us recall that any condition c_{l_k} of
 480 a rule defines a domain D_{l_k} in the input space, corresponding to an interval
 481 for feature $x_{\pi(l)}$. Let us consider the set of rules verified by \mathbf{x} and predicting
 482 a label y , i.e., $\mathcal{R}_\mathbf{x}^y = \{r_k | x_{\pi(l)} \in D_{l_k} \text{ for each } l_k \text{ and } \hat{y} = y\}$. A score for y is
 483 then defined as:

$$w_y = \frac{\sum_{r_k \in \mathcal{R}_\mathbf{x}^y} C(r_k)(1 - E(r_k))}{\sum_{r_k \in \mathcal{R}^y} C(r_k)(1 - E(r_k))}, \quad (2)$$

484 where \mathcal{R}^y is the set of all rules generated for class y . A label is thus assigned
 485 to \mathbf{x} by solving the following problem:

$$\hat{y} = \arg \max_y w_y \quad (3)$$

486 6. Multi-Sensor Application

487 6.1. Previous results

488 In our previous work on the topic [6], we have shown the usage of the LLM
 489 as a prediction tool for following therapy in respiratory diseases. Patients
 490 with COPD are subjected to a monitoring period, using an inhalation tracker.
 491 The data obtained include the daily measurements taken by the inhalation
 492 tracker and patients' characteristics. The CAT⁸ has been taken as a reference.

⁸More information are available in the following address: <https://www.mdcalc.com/copd-assessment-test-cat>, access on November 2023.

493 It is a self-report questionnaire that assesses the impact of COPD on health
494 status. The higher the CAT score, the higher the perceived impact of the
495 disease. Observing the LLM rules, we provided inference about adherence to
496 treatment over time in terms of CAT.

497 6.2. Data Collection

498 Here, we show results with respect to monitoring through the devices out-
499 lined in subsection 3.2. Moreover, we show how adversarial machine learning
500 may be used to provide fake indications that are still deemed plausible and
501 suitable for further analysis by the clinical experts. Our first analysis regards
502 the original dataset, without any adversarial machine learning corruption,
503 and aims at providing the *baseline* rules generated by the LLM model.

504 The following quantities were daily collected for two consecutive months,
505 and structured in a database for further LLM training⁹.

506
507 oxygen, body temperature, heart rate (from oximeter), heart rate
508 master (from sphygmomanometer), weight, Body Mass Index, FEV1, PEF,
509 MAP, diastolic blood pressure , systolic blood pressure

510
511 In detail, oxygen is the blood oxygen saturation (i.e., the SpO₂). Heart
512 rate is measured via both the oximeter and the sphygmomanometer: the
513 feature corresponding to the latter device is denoted by the suffix 'master'
514 (i.e., heart rate master). The Forced Expiratory Volume in 1 second (FEV1)
515 is the amount of air (in liters) that can be exhaled in the first second during
516 forced exhalation after maximal inspiration. MAP, or mean arterial pressure,
517 is defined as the average blood pressure in a patient's arteries during one
518 cardiac cycle. It is considered a better indicator of perfusion to vital organs
519 than systolic blood pressure.

520 Peak Expiratory Flow (PEF) is the maximum flow (or velocity) that can
521 be achieved when performing a forced exhalation that is initiated after a full
522 inspiration, measured in liters per minute or liters per second. This variable
523 is used to set the target of the classification problem. Specifically, the dataset
524 was labelled with 'low' for $PEF \leq 400$ L/min or 'high' for $PEF > 400$ L/min.
525 The threshold of 400 was determined under suggestion of the clinical expert.

⁹The Rulex platform has been used, <http://www.rulex.ai>

526 The dataset here described is available at [https://github.com/saranrt95/](https://github.com/saranrt95/Medical_IoT_ML)
 527 `Medical_IoT_ML`, along with smartwatch data presented later in Section 8.

528 6.3. Statistical validation

Table 1: Contingency frequencies matrix between the output variable (classification) and a rule R

Contingency Matrix	Output	
	output	output
Rule R	$y R$	$\neg y R$
not Rule R	$y \neg R$	$\neg y \neg R$

529 We use the Fisher’s Exact Test (FET) to test the statistical significance
 530 of rules obtained. The FET, indeed, is more accurate than other test of
 531 independence when the expected numbers are small, and it can be adopted
 532 to overcome the small sample size problem. The FET, in general, examines
 533 the significance of the association between two kinds of classification. In our
 534 case, we compare the distribution of a rule R, and its complementary $\neg R$,
 535 in the output classes $y, \neg y$, obtaining a contingency matrix, as in Table 1
 536 above. Then, considering the independence between the distribution of the
 537 Output and the distribution of the rule R as null hypothesis, we compute the
 538 p-value. If the p-value is greater than 0.05, we accept the null hypothesis,
 539 otherwise, we prove the significance of rule R in detecting the output classes.

540 6.4. Baseline

541 The following rules are inferred by the LLM and validated by the FET
 542 test:

543
 544 **if** $((\text{heart rate} < 74) \wedge (\text{diastolic pressure} > 67))$ **then** high (C=43%) (E=4.5%)

545 **if** $(FEV1 < 2.23)$ **then** low (C=41%) (E=4.7%),

546
 547 where C and E denote their covering and error expressed in percentage.

548 Both rules provide clear indications about the status of the breath (through
 549 the PEF classification): one may argue that the knowledge extracted from
 550 them is trivial, since it puts in relation a good or bad breath performance

551 with blood pressure and heart rate, which may be expected even by non ex-
552 perts. However, we highlight the following elements about the role of XAI.
553 First of all, its adoption reveals useful to determine which of the several
554 devices the monitoring path should focus on, by analyzing which variables
555 more frequently occur within the rules. Moreover, it is difficult even for an
556 expert to find the exact thresholds describing the output classes, jointly with
557 all the input variables involved. In this perspective, XAI acts as an artificial
558 predictor, namely, the rules map the measurements into the output class at
559 the end of the observation period. Once the rules are available, they may be
560 used by the medical staff at any time as predictors of the quality treatment
561 in the near future and may drive proper decisions, such as contact the patient
562 at home when the measurements lie in the outlined ranges of bad treatment.

563 7. Adversarial machine learning

564 In this section, we introduce further analysis with respect to adversarial
565 machine learning (AML). Although known to experts in the sector, in recent
566 years it had an exponential growth due to the continuous development of new
567 machine learning applications in various sectors. As for many other fields,
568 in the healthcare sector it plays a key role, for this reason we decided to
569 consider possible AML attacks within Pneualytics project framework.

570 A very important aspect in the healthcare context is data security. An
571 increasingly present thread in the security landscape is linked to attacks on
572 the machine learning algorithm. Specifically, these attacks are called adver-
573 sarial machine learning [55] where the aim of adversarial machine learning
574 is to fool models by supplying deceptive input to cause a malfunction in a
575 machine learning model. The problem is motivated by the fact that machine
576 learning techniques were not originally designed to compete with adaptive
577 and intelligent adversaries; therefore, in principle, the security of the entire
578 system could be compromised by exploiting specific vulnerabilities of these
579 algorithms, through a careful manipulation of the data that are supplied. A
580 classic example of an adversarial machine learning attack is related to the
581 context of image classification. The algorithm learns to classify images dur-
582 ing the training phase based on the dataset used. An attacker could insert
583 noise into the image to be classified (invisible to the human eye) to make the
584 machine learning algorithm classify the image incorrectly. Several examples
585 of image adversarial machine learning were studied and presented [56, 57, 58].

586 As previously described, in the healthcare sector, data is of primary im-
587 portance as it can be used to predict a disease or manage remotely treatments
588 and cures by using machine learning algorithms. An attack of this nature
589 could lead to serious consequences as the manipulation by an attacker of the
590 data could lead to an incorrect classification of the disease or to the admin-
591 istration of a drug when necessary. In the extreme case, the identification of
592 a fatal disease only in an advanced state when the medical treatments are
593 no longer effective.

594 For these reasons we decided to investigate the adversarial machine learn-
595 ing in our project in order to verify if the machine learning system developed
596 in Pneulytics is able to resist the variations of the dataset and to equally
597 correctly classify the disease. In order to achieve this results, we imple-
598 mented a simple adversarial machine learning algorithm on the dataset used
599 in Section 6.2 and compared the results. The adversarial machine learning
600 attack works by adding a Gaussian noise $\mathcal{Z} \sim \mathcal{N}(0, 0.8)$ to the original
601 data. We selected this small range since the variation of the dataset must be
602 invisible (or not simply identifiable) by the statistician analyzing the data.
603 Subsequently, the data were processed again with the techniques used in Sec-
604 tion 5, to verify how the algorithm behaves with the dataset affected by the
605 adversarial attack. The following rules are obtained.

606

607 **if** ((*heart rate master* $\in [62, 75]$) \wedge (*diastolic pressure* > 67)) **then** high (C=77%) (E=5%)

608 **if** ((*oxygen* < 96) \wedge (*heart rate* $\in [66, 93]$) \wedge ((*FEV1* $\in [1.11, 2.39]$))) **then** low (C=43%) (E=4%)

609 **if** ((*systolic pressure* $\in [98, 103]$)) **then** low (C=38%) (E=4%)

610

611 They are similar to the baseline in terms of features and reference inter-
612 vals, in a such a way that the medical staff does not recognize the presence
613 of an adversarial inside the machine learning engine. A subtle question nat-
614 urally arises: how to set the adversarial setting in order to move the medical
615 staff to a wrong diagnosis? This would lead to further investigation with
616 clinicians. Moreover, how to prevent an attack like this? Is it possible to
617 circumvent the behaviour of legitimate rules in order to understand the pres-
618 ence of an adversarial attack? All of these issues are argument of our ongoing
619 research.

620 8. Smartwatch example

621 A Fitbit Versa 3 smartwatch was considered, which is equipped with many
622 sensors, e.g., among others, GPS, red/infrared sensors for SpO2 registration,
623 and movement sensors (3-axis accelerometer, gyroscope), which make it a
624 very versatile instrument. Data are transmitted via Bluetooth Low Energy
625 (BLE) technology to the dedicated smartphone app associated to the device
626 and are stored into the Fitbit user account, remaining available for data
627 query.

628 8.1. Dataset collection and clinical problem definition

629 From the Fitbit smartwatch, we collected one month of measurements
630 from a subject who was following a pharmaceutical therapy for COPD.
631 Specifically, these quantities were:

632 1. Heart-related daily measurements:

- 633 • Average heart rate `HRmean` and standard deviation `HRstd`.
- 634 • amount of time spent in different heart-rate zones, which are
635 defined as percentage ranges of the maximum heart rate esti-
636 mated for the subject (`maxHR` hereon): `below zone`, i.e., $< 50\%$
637 `maxHR`; `fat burn zone` ($50\text{-}69\%$ `maxHR`); `cardio zone` ($70\text{-}84\%$
638 `maxHR`); `peak zone` ($> 85\%$).
- 639 • heart rate variability (HRV) during sleep: `rmssd-HRV`, `NonREM-HR`
640 and `entropy-HRV` are values aiming at describing different aspects
641 of the beat-to-beat intervals variations.

642 2. Respiratory measures during sleep:

- 643 • Blood oxygen saturation, `average SpO2`, and its lower and upper
644 bounds.
- 645 • Infrared to red ratio average `IRtoRedMean` and its standard devi-
646 ation `IRtoRedMeanStd`, which reflect the estimated oxygen varia-
647 tion via pulse oximetry principles [59].
- 648 • Average `respiratory rate`.

649 3. Daily minutes of activity performed at different levels of intensity: 650 `sedentary minutes`, `lightly active minutes`, `moderately active` 651 `minutes`, `very active minutes`.

652 These quantities were then used to build a comprehensive dataset for a
 653 period of 32 days of observation.

654 The aim of our preliminary study was to assess which of the considered
 655 measurements exhibited the main variations when the involved patient was
 656 treated with 1 puff/day of the COPD drug or 2 puffs/day. To this end,
 657 we decided to disregard the activity-related measurements from the input
 658 variables, since they were related to the subject’s behavior and not to its
 659 physiological status. To make the dataset suitable for supervised machine
 660 learning-based analysis, we labelled the samples with labels resembling the
 661 **therapy** followed by the patient, i.e., assigning ‘1’ for 1 puff/day or ‘2’ for
 662 2 puffs/day. Lastly, we selected a rule-based binary classifier to predict the
 663 dose of therapy, specifically a Logic Learning Machine model. Due to the
 664 limited size of the dataset, statistical validation of rules was carried out
 665 through Fisher Exact Test. In addition, several random shuffles of the data
 666 were performed and a separate LLM classifier was trained on them.

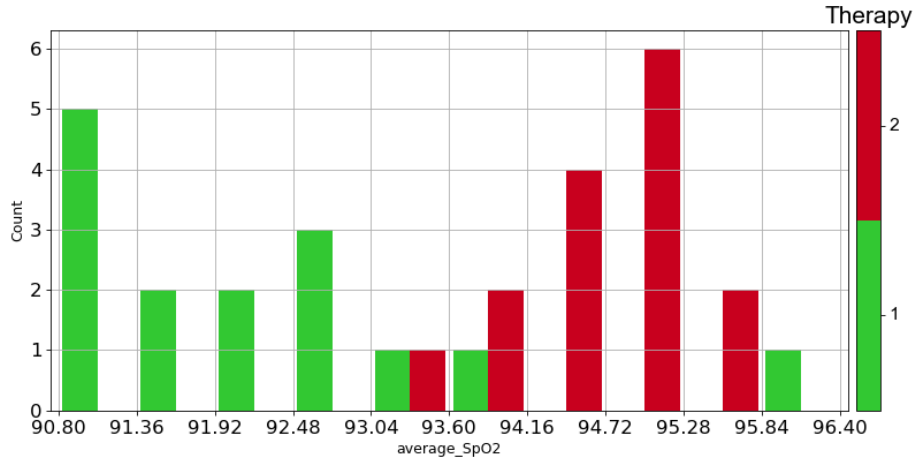
667 *8.2. Preliminary results*

668 As a first step in the analysis, features distributions were explored to as-
 669 sess the feasibility of adopting a rule-based model to discriminate the classes.
 670 As an example, we show the histograms related to the **average SpO2** and
meanHR quantities (Fig. 2).

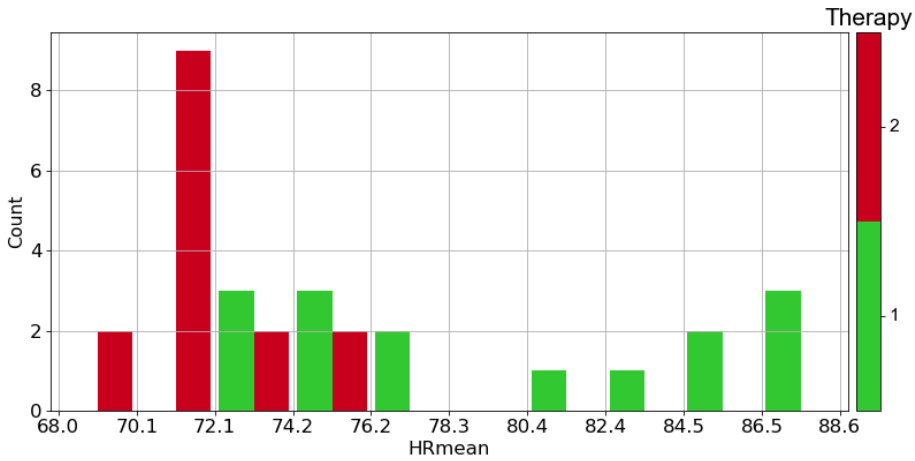
Table 2: LLM rules obtained on 5 random shuffles of the Fitbit dataset, after their statistical validation via FET test, along with their covering (C [%]) and error (r [%])

Shuffle	Validated Rules	C [%]	E [%]
1	if $averageSpO2 \leq 93.25$ then therapy = 1	77	0
	if $averageSpO2 > 92.80 \wedge 11.064 < HRstd \leq 15.040$ then therapy = 2	89	0
2	if $HRmean > 71.252 \wedge IRtoRedMean \leq 0.404$ then therapy = 1	100	0
	if $89.5 < LowerBoundSpO2 \leq 94.7 \wedge HRmean \leq 74.696$ then therapy = 2	90	0
3	if $rmssd-HRV \leq 46.065 \wedge HRmean > 71.83$ then therapy = 1	91	0
	if $averageSpO2 > 93.1 \wedge 11.249 \leq HRstd \leq 17.383$ then therapy = 2	91	0
4	if $HRmean > 71.570 \wedge IRtoRedMean \leq 0.404$ then therapy = 1	100	0
	if $HRmean \leq 72.551$ then therapy = 2	92	0
5	if $averageSpO2 \leq 93.25$ then therapy = 1	100	0
	if $averageSpO2 > 93.25$ then therapy = 2	91	0

671 The figures show that in both cases the two classes are pretty well distin-
 672 guishable: also, as expected, a higher dose of therapy improves the average
 673 SpO2 and lowers the heart rate. However, specific cut-off values on these
 674



(a) Average SpO2



(b) Average Heart Rate

Figure 2: Class distributions for two exemplary features

675 measurements and further knowledge were discovered through the usage of
 676 XAI. The LLM model was then trained on 5 random shuffles of the dataset,
 677 and, after the FET statistical validation, 2 rules were generated for each
 678 shuffle, as reported in Table 2. The average model accuracy over the shuffles
 679 reached the 74%. The feature rankings reported below give an idea about
 680 the most important variable for decision making as well as how the ranking
 681 may be sensitive to data variations (shuffles). Future research include larger

682 time horizon of patient monitoring to achieve stable assessment of model
 683 suggestions.

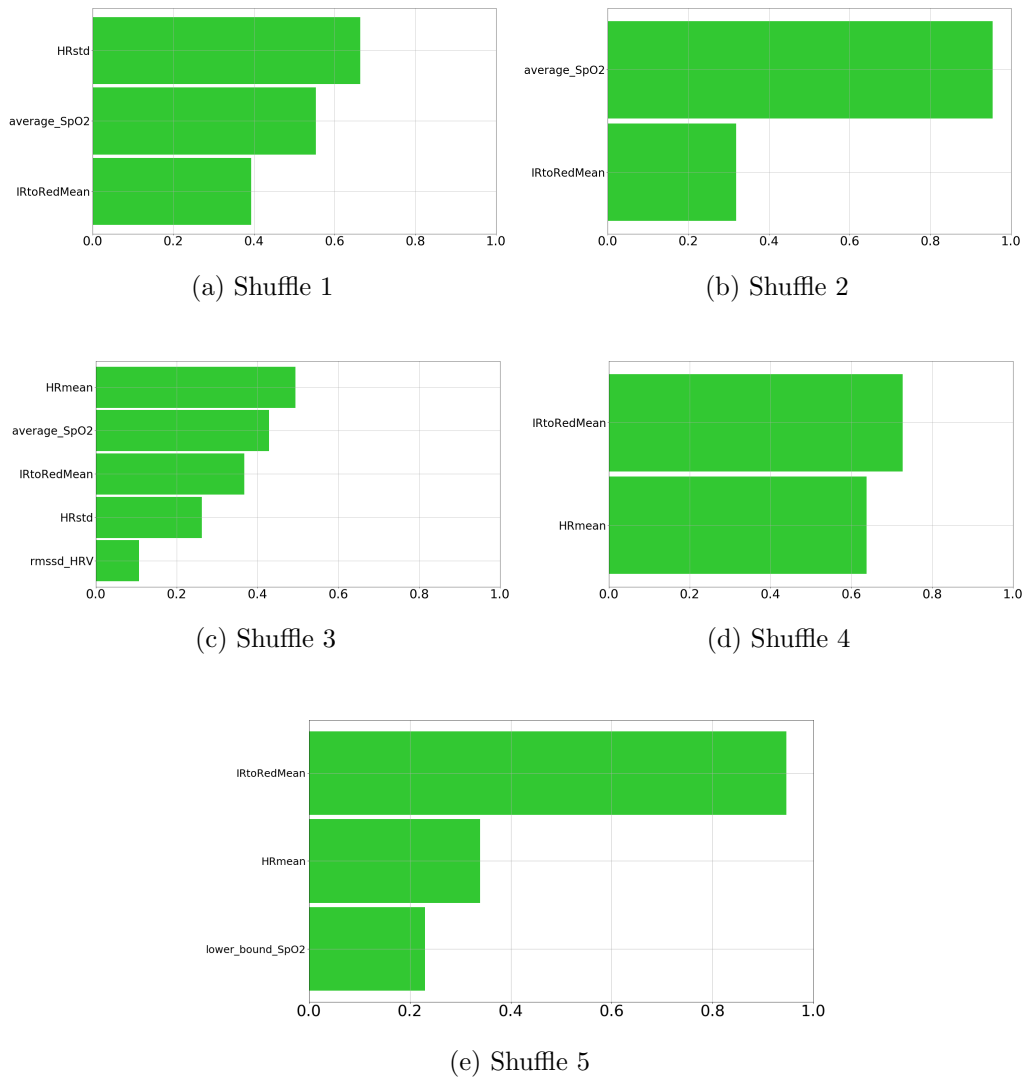


Figure 3: LLM feature rankings for the 5 data shuffles

684 Despite the ranking sensitivity to data variations, as well as the 15 fea-
 685 tures given in input to the LLM, the model generated short rules, with no more
 686 than 2 conditions each. This would improve their interpretability. Over-

687 all, a few factors emerged as the most influent in predicting the therapy,
688 namely `averageSpO2`, `HRmean` and `IRtoRedMean`. Indeed, these attributes
689 were present in the feature ranking for at least 3 out of 5 shuffles (Fig. 3).
690 Overall, the XAI approach gives interesting insight into the problem, thus
691 providing promising indications for future research.

692 9. Conclusions and future work

693 In this paper, we introduce Pnelytics, a novel framework designed to
694 use innovative technologies such as the Internet of Things (IoT) and Artifi-
695 cial Intelligence (AI), combined with security and privacy aspects, to collect
696 and process heterogeneous data from environmental and wearable sensors to
697 monitor patients' health. We believe that the approach is feasible and can
698 be used to monitor patients' outcomes and adherence to treatment and to
699 better understand the factors that influence individual outcomes.

700 Preliminary tests in [6] and in this paper show that the combination of
701 clinical data and IoT allows to monitor the therapy and to understand the
702 factors that influence it.

703 Future works may be focused on the operative development of the plat-
704 form, while exploring new directions, spanning from extending the sensing
705 scenario to the environment (e.g., how air quality may impact the treatment?)
706 to the joint study of AI and privacy. The last relevant topic is General Data
707 Protection Regulation (GDPR) EU regulation¹⁰ and involves brand new ap-
708 proaches, as accurate statistical models of correlation may accidentally reveal
709 more information about the patients than intended¹¹.

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¹⁰More information is available on the ICO portal, access in November 2023.

¹¹More information is available at: <https://github.com/frankmcsherry/blog/blob/master/posts/2016-06-14.md>, access in November 2023.

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