

On the modelling of brain fibers in the EEG Forward Problem via a New Family of Wire Integral Equations

Original

On the modelling of brain fibers in the EEG Forward Problem via a New Family of Wire Integral Equations / Rahmouni, Lyes; Merlini, Adrien; Pillain, Axelle; Andriulli, Francesco P.. - In: JOURNAL OF COMPUTATIONAL PHYSICS: X. - ISSN 2590-0552. - 5:(2020), p. 100048. [10.1016/j.jcp.2019.100048]

Availability:

This version is available at: 11583/2781732 since: 2020-03-24T10:15:14Z

Publisher:

Elsevier

Published

DOI:10.1016/j.jcp.2019.100048

Terms of use:

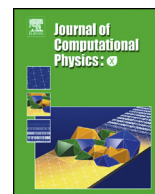
This article is made available under terms and conditions as specified in the corresponding bibliographic description in the repository

Publisher copyright

Elsevier postprint/Author's Accepted Manuscript

© 2020. This manuscript version is made available under the CC-BY-NC-ND 4.0 license
<http://creativecommons.org/licenses/by-nc-nd/4.0/>. The final authenticated version is available online at:
<http://dx.doi.org/10.1016/j.jcp.2019.100048>

(Article begins on next page)



On the modeling of brain fibers in the EEG forward problem via a new family of wire integral equations

Lyes Rahmouni^a, Adrien Merlini^a, Axelle Pillain^b, Francesco P. Andriulli^{a,*}

^a Department of Electronics and Telecommunications, Politecnico di Torino, Turin, Italy

^b IMT Atlantique, Brest, France

ARTICLE INFO

Article history:

Received 14 March 2019

Received in revised form 11 December 2019

Accepted 16 December 2019

Available online 30 December 2019

Keywords:

Electroencephalography

EEG forward problem

Anisotropy

Integral equations

Boundary Element Method

ABSTRACT

Source localization based on electroencephalography (EEG) has become a widely used neuroimaging technique. However its precision has been shown to be very dependent on how accurately the brain, head and scalp can be electrically modeled within the so-called forward problem. The construction of this model is traditionally performed by leveraging Finite Element or Boundary Element Methods (FEM or BEM). Even though the latter is more computationally efficient thanks to the smaller interaction matrices it yields and near-linear solvers, it has traditionally been used on simpler models than the former. Indeed, while FEM models taking into account the different media anisotropies are widely available, BEM models have been limited to isotropic, piecewise homogeneous models. In this work we augment standard BEM with a new wire integral equation to account for the anisotropy of the white matter. The new formulation combines the efficiency of BEM discretization of the boundaries only and modeling of the fibrous nature of the white matter as one-dimensional basis functions which limits the computational impact of their modeling. We compare our scheme against widely used formulations and establish its correctness in both canonical and realistic cases.

© 2019 The Author(s). Published by Elsevier Inc. This is an open access article under the CC BY license (<http://creativecommons.org/licenses/by/4.0/>).

1. Introduction

Electroencephalography (EEG) based source localization has gained an increasing popularity as a reliable neuroimaging modality in research and medical practice [1–3]. Using scalp measured potentials, various algorithms have been proposed for the retrieval of the location of the neuro-generators [4]. Many of these algorithms rely on an accurate solution of the associated forward problem which maps a given setting of sources and head model to the corresponding scalp potential distribution. The complexity of the head geometry and its underlying conductivity, however, precludes the use of analytical methods and one has to adopt numerical approximations. With their renowned high accuracy and robustness, integral equations-based methods remain the preferred choice for researchers [5,6]. In particular, the boundary element method (BEM) only requires the discretization of the boundaries, thus reducing the overall dimensionality. Moreover, given the smoothness of its underlying kernel, it is possible to augment BEM with fast algorithms such as the adaptive cross approximation (ACA) or the fast multipole method (FMM) [7,8], which further reduce its computational complexity. The three most widely employed BEM formulations for the EEG forward problem are the adjoint double layer (ADL), the double layer (DL) and the symmetric (SY) approaches [9–11]. By leveraging on methods of layer potentials, these formulations solve Poisson's

* Corresponding author.

E-mail address: francesco.andriulli@polito.it (F.P. Andriulli).

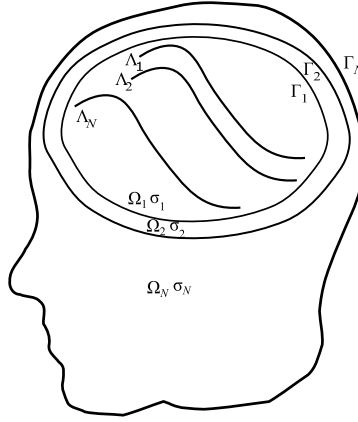


Fig. 1. Volume conductor with nested geometry.

equation under the assumption of isotropic media [12]. The DL formulation is a direct approach in which the potential is obtained directly while the ADL formulation solves first for an auxiliary unknown before integrating it to obtain the electric potential. Differently from the two previous approaches, the SY formulation simultaneously involves two surface unknowns. Despite its larger system of equations, it has a block diagonal structure [12]. For more details on these methods, their relative merits and disadvantages, the reader is referred to [10,11,13].

Despite their advantages, BEM-based formulations are restricted to isotropic and piece-wise homogeneous problems. This is a significant limitation since the white matter anisotropy has a considerable impact on the accuracy of source localization procedures [14,15]. These early results have been obtained with differential based methods and entire volume discretization [14,15], which is computationally expensive. More recently, integral techniques accounting for the white matter anisotropy have been introduced [13,16]; they do however also require the discretization of the entire head volume.

The anisotropy of the white matter tissue arises from its underlying assembly of bundles of parallel-oriented axons [17,18]. This suggests that the apparent inhomogeneous anisotropy is actually structured and may be expressed in terms of these axons' fibers. This observation has been leveraged on in [19] by replacing a single fiber by dipolar sources of constant magnitude. The forward problem was subsequently solved iteratively with the symmetric formulation. However, this work does not account for the coupling and interactions between different fibers which is essential for a precise forward solution. The structured assembly of the white matter has also been exploited for different settings in [20,21].

The work presented in this paper aims at extending the three main BEM (EEG) formulations to take into account the anisotropic and inhomogeneous conductivity of the white matter. This is achieved by a modelization of the white matter connectivity. Indeed, using diffusion weighted MRI (DW-MRI) it is possible to track axon fibers and reveal the underlying network of the white matter [22]. One-dimensional basis functions are used for the modelization of the fibers, which results in efficient and accurate forward solutions. As a byproduct, the new technique we present could further improve the recently introduced approaches exploiting the brain connectivity patterns in source estimation [23,24]. Some preliminary results have been presented in [25]. Several numerical experiments validate the new schemes in canonical and realistic settings.

The reader should note that 1D formulations have been extensively studied in the context of high frequency electromagnetic modeling of wire-like structures [26–28], although those schemes, for perfect electrically conducting wires, are only mildly related to the ones presented here.

The paper is organized as follows: the notations is set and some background is recalled in Section 2; the new equations and their discretizations are then derived in Section 3 and Section 4, respectively. The new schemes are validated with various simulations and tests in Section 5 before closing with conclusions in Section 6.

2. Background and notations

Consider an electric volume current density \mathbf{J} residing in a conducting medium $\Omega \subset \mathbb{R}^3$. This domain is composed of N nested, piecewise homogeneous sub-regions Ω_i such that $\Omega = \bigcup_{i=1}^N \Omega_i$ with Ω_1 being the innermost layer. Each sub-region is associated with an isotropic conductivity σ_i and delimited by the Lipschitz surface Γ_i with $\Gamma = \bigcup_{i=1}^N \Gamma_i$ and $\Gamma_i \cup \Gamma_{i-1} = \partial \Omega_i$ (Fig. 1).

Let Λ_j be a curve modeling a bundle of parallel white matter fibers and $\Lambda = \bigcup_{j=1}^{N_f} \Lambda_j$ their union. These fibers assume a thin cylindrical shape of circular section a [29,30] and give rise to a tensorial conductivity profile in which the conductivity along the fiber σ_f is different from the conductivity in the transversal direction σ_1 . In the quasi-static regime, the electric potential ϕ is related to the current density \mathbf{J} via Poisson's equation

$$\nabla \cdot (\underline{\underline{\sigma}}(\mathbf{r}) \nabla \phi(\mathbf{r})) = \nabla \cdot \mathbf{J}(\mathbf{r}), \quad \mathbf{r} \in \Omega, \quad (1)$$

where the local electric conductivity $\underline{\underline{\sigma}}$ is described by a 3×3 symmetric tensor [31]. For the sake of simplicity in explaining our new method, we neglect the anisotropy of the skull and thus, given that the neuron fibers are only present in the innermost region Ω_1 , eq. (1) can be rewritten as

$$\nabla \cdot (\underline{\underline{\sigma}}(\mathbf{r}) \nabla \phi(\mathbf{r})) = \nabla \cdot \mathbf{J}(\mathbf{r}), \quad \mathbf{r} \in \Omega_1, \quad (2)$$

$$\sigma_i \Delta \phi(\mathbf{r}) = 0, \quad \mathbf{r} \in \Omega_i, i = 2, \dots, N, \quad (3)$$

where it was assumed that the current sources are present only in the innermost layer that corresponds to the brain. Two transmission conditions are associated with each of these equations: (i) a Dirichlet condition that enforces the continuity of the electric potential across interfaces and (ii) a Neumann condition that enforces the continuity of the electric current flux, i.e.

$$[\phi]_j = 0 \quad \text{on } \Gamma_j, \text{ for } j = 1 \dots N, \quad (4)$$

$$[\sigma \partial_{\hat{\mathbf{n}}} \phi]_j = 0 \quad \text{on } \Gamma_j, \text{ for } j = 1 \dots N, \quad (5)$$

where the bracket notation $[g]_j$ denotes the jump of a function g across Γ_j and $\partial_{\hat{\mathbf{n}}} g = \hat{\mathbf{n}} \cdot \nabla g$ with $\hat{\mathbf{n}} = \hat{\mathbf{n}}(\mathbf{r})$ the unit vector normal to Γ_j pointing outward of Ω_j . Note that the fibers do not come into contact with the inner surface. In the context of the EEG forward problem, brain sources are commonly modeled as current dipoles [32,33], i.e.

$$\mathbf{J}(\mathbf{r}) = \mathbf{P} \delta(\mathbf{r} - \mathbf{r}_0), \quad (6)$$

in which \mathbf{P} and δ respectively denote the dipole moment and the Dirac delta function. The electric potential induced by this elementary source in an infinite homogeneous domain of conductivity σ_1 reads

$$V_{\text{dip}}(\mathbf{r}) = \frac{\mathbf{P} \cdot (\mathbf{r} - \mathbf{r}_0)}{4\pi \sigma_1 |\mathbf{r} - \mathbf{r}_0|^3}. \quad (7)$$

3. Integral equation based formulations

By transforming Poisson equation into an integral equation, conventional BEM formulations (SL, DL and SY), have been particularly attractive as they offer computational savings in comparison with other alternatives. In general, reformulating a partial differential equation as an integral expression requires knowledge of its fundamental solution. When considering the anisotropy of the white matter however, eq. (2) involves position and orientation dependent tensors for which the corresponding fundamental solution does not exist in closed form, for general geometries. Equation (2) should then be recast into an equivalent one at a reduced dimensionality by extracting the Laplacian operators and using Green's identities. In particular, this choice not only allows for a unified treatment of eqs. (2) and (3), but also reduces the effect of the anisotropy to a one-dimensional apparent volume current density along the fibers. Consequently, the framework of standard BEM formulations can be extended to handle the anisotropy of the white matter. To that end, eq. (2) can be re-expressed as

$$\Delta \phi(\mathbf{r}) = \nabla \cdot \left(\frac{\mathbf{J}(\mathbf{r})}{\sigma_1} + \underline{\underline{\kappa}}(\mathbf{r}) \mathbb{J}_f(\mathbf{r}) \right), \quad \mathbf{r} \in \Omega_1, \quad (8)$$

where $\mathbb{J}_f = \underline{\underline{\sigma}} \nabla \phi$ is the apparent volume current density along the fibers and $\underline{\underline{\kappa}}$ is the conductivity contrast defined as

$$\underline{\underline{\kappa}}(\mathbf{r}) = \left(\underline{\underline{\sigma}}^{-1}(\mathbf{r}) - \sigma_1^{-1} \underline{\underline{I}} \right), \quad (9)$$

in which $\underline{\underline{I}}$ is the identity tensor. Note that $\underline{\underline{\kappa}}$ is zero everywhere except on the fibers where it has the form

$$\underline{\underline{\kappa}}(\mathbf{r}) = (\sigma_f^{-1} - \sigma_1^{-1}) \hat{\mathbf{t}}(\mathbf{r}) \hat{\mathbf{t}}^T(\mathbf{r}) \quad (10)$$

with $\hat{\mathbf{t}}(\mathbf{r})$ being the unit vector tangential to Λ_j . Therefore, the matrix-vector product $\underline{\underline{\kappa}}(\mathbf{r}) \mathbb{J}_f(\mathbf{r})$ reduces, locally, to a scalar-vector product. We remind the reader that, in the above settings, it is assumed that the conductivity of the fibers is σ_1 in the transversal direction and σ_f in the longitudinal direction. Therefore, even though we are modeling only the tangential part of the apparent volume current density, we are not making any assumption on the total current density on the fibers. In particular, the transversal part of the total current density is not assumed to be constant.

In order to derive an integral representation for the potential and its flux using Green's second identity, the following well known operators are introduced:

- the single layer operator

$$(Su|_{\Gamma_i})(\mathbf{r}) = \int_{\Gamma_i} G(\mathbf{r} - \mathbf{r}') u(\mathbf{r}') ds(\mathbf{r}'), \quad \mathbf{r} \in \Omega, \quad (11)$$

- the double layer operator

$$(\mathcal{D}u|_{\Gamma_i})(\mathbf{r}) = \int_{\Gamma_i} \partial_{\mathbf{n}'} G(\mathbf{r} - \mathbf{r}') u(\mathbf{r}') \, ds(\mathbf{r}'), \quad \mathbf{r} \in \Omega, \quad (12)$$

- the adjoint double layer operator

$$(\mathcal{K}u|_{\Gamma_i})(\mathbf{r}) = \int_{\Gamma_i} \partial_{\mathbf{n}} G(\mathbf{r} - \mathbf{r}') u(\mathbf{r}') \, ds(\mathbf{r}'), \quad \mathbf{r} \in \Gamma_j, \quad (13)$$

- the hypersingular operator

$$(\mathcal{N}u|_{\Gamma_i})(\mathbf{r}) = \int_{\Gamma_i} \partial_{\mathbf{n}} \partial_{\mathbf{n}'} G(\mathbf{r} - \mathbf{r}') u(\mathbf{r}') \, ds(\mathbf{r}'), \quad \mathbf{r} \in \Gamma_j, \quad (14)$$

where

$$G(\mathbf{r} - \mathbf{r}') = \frac{1}{4\pi |\mathbf{r} - \mathbf{r}'|} \quad (15)$$

is the fundamental solution associated with the Laplacian. In addition, a new operator is introduced to handle the fiber contributions

$$(\mathcal{V}u)(\mathbf{r}) = \int_{\Lambda} g(\mathbf{r} - \mathbf{r}') \nabla \cdot (\underline{\kappa} u(\mathbf{r}')) \, dl(\mathbf{r}'), \quad \mathbf{r} \in \Omega, \quad (16)$$

where the associated wire kernel is defined as

$$g(\mathbf{r} - \mathbf{r}') = \int_0^a \int_0^{2\pi} G(\mathbf{r} - \mathbf{r}') \rho' \, d\rho' \, d\theta', \quad (17)$$

and ρ and θ are the usual polar coordinates in the fiber's transverse plane.

The starting point of our development is Green's second identity, which states that

$$(\mathcal{D}\phi|_{\partial\Omega_i})(\mathbf{r}) - (\mathcal{S}\xi|_{\partial\Omega_i})(\mathbf{r}) = \int_{\Omega_i} \phi(\mathbf{r}) \Delta G(\mathbf{r} - \mathbf{r}') - G(\mathbf{r} - \mathbf{r}') \Delta \phi(\mathbf{r}), \quad \mathbf{r} \in \Omega_i \setminus \Gamma_i, \quad (18)$$

where $\xi = \partial_{\mathbf{n}} \phi$ is the derivative of the potential in the normal direction. Using eqs. (3) and (8) and the property of the fundamental solution, eq. (18) reduces to the following

$$(\mathcal{D}\phi|_{\partial\Omega_i})(\mathbf{r}) - (\mathcal{S}\xi|_{\partial\Omega_i}^{\pm})(\mathbf{r}) = -\phi(\mathbf{r}) + \begin{cases} v_{\text{dip}}(\mathbf{r}) - \sum_{k=1}^{N_f} \mathcal{V} \mathbb{J}_{\Lambda_k}(\mathbf{r}) & \mathbf{r} \in \Omega_i \setminus \Gamma_i, i = 1, \\ 0 & \mathbf{r} \in \Omega_i \setminus \Gamma_i, i = 2 \dots N. \end{cases} \quad (19)$$

Taking the limit $\mathbf{r} \rightarrow \partial\Omega$, the following integral representation for the electric potential is derived

$$(\mathcal{D}\phi|_{\partial\Omega_i})(\mathbf{r}) - (\mathcal{S}\xi|_{\partial\Omega_i}^{\pm})(\mathbf{r}) = -\frac{1}{2} \phi|_{\partial\Omega_i}(\mathbf{r}) + \begin{cases} v_{\text{dip}}(\mathbf{r}) - \sum_{k=1}^{N_f} \mathcal{V} \mathbb{J}_{\Lambda_k}(\mathbf{r}) & \mathbf{r} \in \partial\Omega_i, i = 1, \\ 0 & \mathbf{r} \in \partial\Omega_i, i = 2 \dots N, \end{cases} \quad (20)$$

where the $\frac{1}{2}$ stems from the Cauchy principal value. By differentiating eq. (19) with respect to \mathbf{r} in the direction normal to the boundary, an integral representation for the potential flux can be obtained

$$(\mathcal{N}\phi|_{\partial\Omega_i})(\mathbf{r}) - (\mathcal{K}\xi|_{\partial\Omega_i}^{\pm})(\mathbf{r}) = -\frac{1}{2} \xi|_{\partial\Omega_i}^{\pm}(\mathbf{r}) + \begin{cases} v_s(\mathbf{r}) - \sum_{k=1}^{N_f} \mathcal{W} \mathbb{J}_{\Lambda_k}(\mathbf{r}) & \mathbf{r} \in \partial\Omega_i, i = 1, \\ 0 & \mathbf{r} \in \partial\Omega_i, i = 2 \dots N, \end{cases} \quad (21)$$

where

$$(\mathcal{W}u)(\mathbf{r}) = \int_{\Lambda} \partial_{\mathbf{n}} g(\mathbf{r} - \mathbf{r}') \nabla \cdot (\underline{\kappa} u(\mathbf{r}')) \, dl(\mathbf{r}') \quad (22)$$

and

$$v_s(\mathbf{r}) = \partial_{\mathbf{n}} v_{\text{dip}}(\mathbf{r}). \quad (23)$$

It is worth noting that eqs. (20) and (21) are written for a normal vector pointing outward. A consistent change of signs should be made when the normals are pointing inward, which is the case for Γ_{i-1} . In the inner most layer Ω_1 the last term of the right-hand side in eqs. (20) and (21) represents the effect of the fibers; it describes the local anisotropic conductivity.

3.1. Double layer-wire formulation

Equations (20) and (21) have two surface unknowns, one of which could be discarded by using the boundary conditions eqs. (4) and (5); depending on the variable discarded two different formulations can be obtained. The double layer-wire formulation is obtained if the surface electric potential $\phi(\mathbf{r})$ is the remaining unknown. This formulation can be derived after multiplying eq. (20) with the local conductivity and summing the contribution of all the regions Ω_i

$$\sigma_1 v_{\text{dip}}(\mathbf{r}) - \sigma_1 \sum_{k=1}^{N_f} \mathcal{V} \mathbb{J}_{\Lambda_k}(\mathbf{r}) = \frac{\sigma_j + \sigma_{j+1}}{2} \phi(\mathbf{r}) - \sum_{i=1}^N (\sigma_{i+1} - \sigma_i) (\mathcal{D}\phi|_{\Gamma_i})(\mathbf{r}), \quad \mathbf{r} \in \Gamma_j, j = 1 \dots N, \quad (24)$$

where the \mathcal{S} operator term cancels out by enforcing the transmission condition (5).

Equation (24) simultaneously involves the surface potential ϕ and the current density \mathbb{J} as unknowns, and therefore needs to be complemented with a second equation. The second equation is obtained by applying the gradient operator to eq. (24)

$$\sigma_1 \nabla v_{\text{dip}}(\mathbf{r}) - \sigma_1 \nabla \sum_{k=1}^{N_f} \mathcal{V} \mathbb{J}_{\Lambda_k}(\mathbf{r}) = \sigma_1 \underline{\underline{\sigma}}_{\Lambda_n}^{-1} \mathbb{J}_{\Lambda_n}(\mathbf{r}) - \nabla \sum_{i=1}^N (\sigma_{i+1} - \sigma_i) (\mathcal{D}\phi|_{\Gamma_i})(\mathbf{r}), \quad \mathbf{r} \in \Lambda_n, n = 1 \dots N_f. \quad (25)$$

Combining eqs. (24) and (25) constitutes the first new formulation and will be referred to as the double layer-wire (DLW) formulation.

3.2. Single layer-wire formulation

Differently from the DLW that is formulated in terms of surface potentials, the single layer-Wire (SLW) formulation is derived from eq. (21) and solves for the jump of the potential's normal derivative across an interface. Thus, applying eq. (21) to each region Ω_j and summing up their contributions yields

$$v_s(\mathbf{r}) - \sum_{k=1}^{N_f} \mathcal{W} \mathbb{J}_{\Lambda_k}(\mathbf{r}) = \frac{1}{2} (\xi|_{\Gamma_j}^- + \xi|_{\Gamma_j}^+)(\mathbf{r}) - \sum_{i=1}^N \mathcal{K}(\xi|_{\Gamma_i}^- - \xi|_{\Gamma_i}^+)(\mathbf{r}), \quad \mathbf{r} \in \Gamma_j, j = 1 \dots N, \quad (26)$$

where the \mathcal{N} operator term cancels out by enforcing the transmission condition (4). After introducing

$$q_{\Gamma_j} = \xi|_{\Gamma_j}^- - \xi|_{\Gamma_j}^+ = \left(\frac{\sigma_{j+1} - \sigma_j}{\sigma_{j+1}} \right) \xi|_{\Gamma_j}^-, \quad (27)$$

the sum of the normal derivatives can be expressed as

$$\xi|_{\Gamma_j}^- + \xi|_{\Gamma_j}^+ = \left(\frac{\sigma_{j+1} + \sigma_j}{\sigma_{j+1} - \sigma_j} \right) q|_{\Gamma_j}. \quad (28)$$

Substituting back eq. (28) in eq. (26) forms the single layer formulation

$$v_s(\mathbf{r}) - \sum_{k=1}^{N_f} \mathcal{W} \mathbb{J}_{\Lambda_k}(\mathbf{r}) = \frac{\sigma_j + \sigma_{j+1}}{2(\sigma_{j+1} - \sigma_j)} q|_{\Gamma_j}(\mathbf{r}) - \sum_{i=1}^N (\mathcal{K}q|_{\Gamma_i})(\mathbf{r}), \quad \mathbf{r} \in \Gamma_j, j = 1 \dots N. \quad (29)$$

Similarly to the DLW eq. (29) exhibits two unknowns and needs to be complemented. The complementary equation will be derived from eq. (20) by summing the contributions of all regions

$$\phi(\mathbf{r}) = v_{\text{dip}}(\mathbf{r}) - \sum_{k=1}^{N_f} \mathcal{V} \mathbb{J}_{\Lambda_k}(\mathbf{r}) + \sum_{i=1}^N (\mathcal{S}q|_{\Gamma_i})(\mathbf{r}), \quad (30)$$

where \mathcal{D} vanishes due to condition eq. (4). A current equation is obtained by applying the gradient operator to eq. (30)

$$\nabla v_{\text{dip}}(\mathbf{r}) - \nabla \sum_{k=1}^{N_f} \mathcal{V} \mathbb{J}_{\Lambda_k}(\mathbf{r}) = \underline{\sigma}_{\Lambda_n}^{-1} \mathbb{J}_{\Lambda_n}(\mathbf{r}) - \nabla \sum_{i=1}^N (S q|_{\Gamma_i})(\mathbf{r}), \quad \mathbf{r} \in \Lambda_n, n = 1 \dots N_f. \quad (31)$$

Subsequently to finding q , the electric potential can be computed via eq. (30).

3.3. Symmetric-wire formulation

The symmetric formulation leverages on a combination of eq. (20) and eq. (21) applied, in contrast with the two previous formulations, to adjacent regions only. Summing these contributions yields

$$\begin{aligned} (\mathcal{D}\phi|_{\partial\Omega_{i-1}})(\mathbf{r}) - (\mathcal{D}\phi|_{\partial\Omega_i})(\mathbf{r}) - (S\xi|_{\partial\Omega_{i-1}}^{\pm})(\mathbf{r}) + (S\xi|_{\partial\Omega_i}^{\pm})(\mathbf{r}) \\ = \begin{cases} -v_{\text{dip}}(\mathbf{r}) + \sum_{k=1}^{N_f} \mathcal{V} \mathbb{J}_{\Lambda_k}(\mathbf{r}) & \mathbf{r} \in \partial\Omega_i, i = 1, \\ 0 & \mathbf{r} \in \partial\Omega_i, i = 2 \dots N. \end{cases} \end{aligned} \quad (32)$$

The current flux $d|_{\Gamma_i} = \sigma_i \xi|_{\Gamma_i}^- = \sigma_{i+1} \xi|_{\Gamma_i}^+$ (by virtue of condition eq. (5)), can be substituted in eq. (32)

$$\begin{aligned} (\mathcal{D}\phi|_{\partial\Omega_{i-1}})(\mathbf{r}) - (\mathcal{D}\phi|_{\partial\Omega_i})(\mathbf{r}) - \sigma_{\Omega_{i-1}}^{-1} (Sd|_{\partial\Omega_{i-1}})(\mathbf{r}) + \sigma_{\Omega_i}^{-1} (Sd|_{\partial\Omega_i})(\mathbf{r}) \\ = \begin{cases} -v_{\text{dip}}(\mathbf{r}) + \sum_{k=1}^{N_f} \mathcal{V} \mathbb{J}_{\Lambda_k}(\mathbf{r}) & \mathbf{r} \in \partial\Omega_i, i = 1, \\ 0 & \mathbf{r} \in \partial\Omega_i, i = 2 \dots N. \end{cases} \end{aligned} \quad (33)$$

This expression constitutes the first equation of the symmetric formulation. It has three unknowns, the surface potential, the normal component of the surface current density and the fibers current density. Therefore, two other equations are needed. In order to derive a second equation, eq. (33) is multiplied by the local conductivity and applied to adjacent domains, yielding

$$\begin{aligned} -\sigma_{\Omega_{i-1}} (\mathcal{N}\phi|_{\partial\Omega_{i-1}})(\mathbf{r}) + \sigma_{\Omega_i} (\mathcal{N}\phi|_{\partial\Omega_i})(\mathbf{r}) + (\mathcal{K}d|_{\partial\Omega_{i-1}})(\mathbf{r}) - (\mathcal{K}d|_{\partial\Omega_i})(\mathbf{r}) \\ = \begin{cases} -\sigma_1 v_s(\mathbf{r}) + \sigma_1 \sum_{k=1}^{N_f} \mathcal{W} \mathbb{J}_{\Lambda_k}(\mathbf{r}) & \mathbf{r} \in \partial\Omega_i, i = 1, \\ 0 & \mathbf{r} \in \partial\Omega_i, i = 2 \dots N. \end{cases} \end{aligned} \quad (34)$$

For the third equation, the gradient operator of eq. (20) is applied to the innermost layer, which leads to the current equation

$$\nabla v_{\text{dip}}(\mathbf{r}) - \nabla \sum_{k=1}^{N_f} \mathcal{V} \mathbb{J}_{\Lambda_k}(\mathbf{r}) = \underline{\sigma}_{\Lambda_n}^{-1} \mathbb{J}_{\Lambda_n}(\mathbf{r}) - \nabla (\mathcal{D}\phi|_{\Gamma_1})(\mathbf{r}) + \sigma_1^{-1} \nabla (Sd|_{\Gamma_1})(\mathbf{r}), \quad \mathbf{r} \in \Lambda, n = 1 \dots N_f. \quad (35)$$

Note that the quantities restricted to non-existing surfaces i.e. Γ_0 and Γ_{N+1} are set to zero and that on the outermost layer $d|_{\Gamma_N}$ is identically Zero. This formulation requires the solution of two surface equations out of which the surface unknowns interact with only their immediate neighbors. This will give rise to a block diagonal matrix, thus reducing the apparently higher computational cost.

4. Discretization

The numerical solution of the presented equations is achieved following a Galerkin approach. In this respect, the different head surfaces Γ_i are tessellated into triangular meshes and the fibers Λ_j into cylindrical segments. On these finite elements, each unknown $S(\mathbf{r})$ is approximated by a linear combination of the N_x basis functions $\{x_i\}$

$$S(\mathbf{r}) \approx \sum_{i=1}^{N_x} a_i x_i(\mathbf{r}), \quad (36)$$

where a_i is the coefficient of the i th basis function. In order to obtain a square linear system, the discretized equations are then tested with an appropriate set of functions of same cardinality as the set of basis functions. The choice of these finite elements is not arbitrary and must be in accordance with the operators' mapping properties i.e. the basis functions should span the domain of the operator and the testing functions should span the dual of its range [11,34]. The functions used to discretize the different unknowns must be capable of satisfying their different physical properties, for instance the

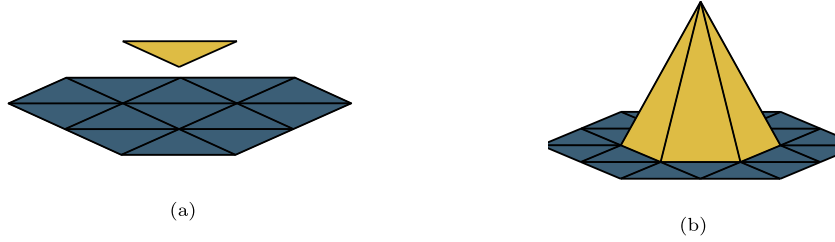


Fig. 2. Illustration of (a) the patch (b) the pyramid basis functions respectively defined in eq. (37) and eq. (38).

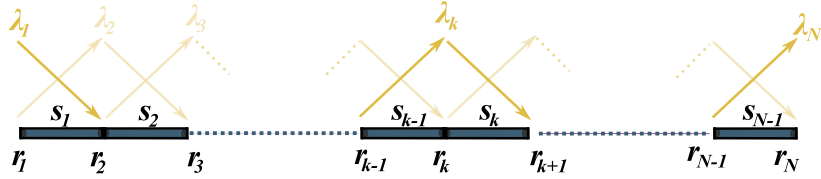


Fig. 3. Illustration of the hat basis functions, as defined in section 4.

discretization of the current density should not permit the existence of jumps. In this paper we considered patch $\{\varphi_n(\mathbf{r})\}$ and pyramid $\{\psi_n(\mathbf{r})\}$ functions to expand the surface unknowns ϕ , q and d depending of the formulation and hat basis functions $\{\lambda_n(\mathbf{r})\}$ to expand the current density $\mathbb{J}(\mathbf{r})$. The pyramid and patch basis functions $\psi_n(\mathbf{r})$ are respectively expressed as

$$\varphi_n(\mathbf{r}) = \begin{cases} 1 & \text{if } \mathbf{r} \in Tr_n, \\ 0 & \text{otherwise,} \end{cases} \quad (37)$$

and,

$$\psi_n(\mathbf{r}) = \begin{cases} \frac{|(\mathbf{r}_j - \mathbf{r}_i) \times (\mathbf{r} - \mathbf{r}_i)|}{|(\mathbf{r}_j - \mathbf{r}_i) \times (\mathbf{r}_n - \mathbf{r}_i)|} & n \neq i \neq j \text{ if } \mathbf{r} \in Tr_n, \\ 0 & \text{otherwise.} \end{cases} \quad (38)$$

where $\mathbf{r}_n, \mathbf{r}_i, \mathbf{r}_j$ are the position vectors of the vertices constituting the triangle Tr_n . Figs. 2(a) and 2(b) present the schematic definitions of these basis functions.

The current density is expanded with oriented hat functions whose support is made of two straight segments $s_k = (\mathbf{r}_k; \mathbf{r}_{k+1})$ and $s_{k+1} = (\mathbf{r}_{k+1}; \mathbf{r}_{k+2})$ (Fig. 3) and defined as

$$\lambda_k(\mathbf{r}) = \begin{cases} \frac{\mathbf{r} - \mathbf{r}_{k-1}}{|\mathbf{r}_k - \mathbf{r}_{k-1}|} & \text{if } \mathbf{r} \in s_{k-1}, \\ \frac{\mathbf{r}_{k+1} - \mathbf{r}}{|\mathbf{r}_k - \mathbf{r}_{k+1}|} & \text{if } \mathbf{r} \in s_k, \\ 0 & \text{otherwise.} \end{cases} \quad (39)$$

It should be noted that the hat basis functions are continuous and thus automatically enforce the jump condition of the current density.

4.1. Discretization of the double layer-wire formulation

In eqs. (24) and (25), the surface potential ϕ is discretized with pyramid basis functions and the current density \mathbb{J} is discretized with hat basis functions. Equations (24) and (25) are then tested with pyramid and hat functions respectively. This gives rise to the following matrix system

$$\begin{bmatrix} \mathbf{G}_{\Lambda_m}^v + \mathbf{V}_{\Lambda_m \Lambda_n}^v & \mathbf{D}_{\Gamma_n \Lambda_m}^v \\ \mathbf{V}_{\Lambda_m \Gamma_n}^s & \mathbf{G}_{\Gamma_n}^s + \mathbf{D}_{\Gamma_n \Gamma_m}^s \end{bmatrix} \begin{bmatrix} \mathbf{J} \\ \phi \end{bmatrix} = \begin{bmatrix} \mathbf{w}_\Lambda \\ c \end{bmatrix}, \quad (40)$$

where the matrix entries are

$$\begin{aligned}
(\mathbf{V}_{\Lambda_i \Lambda_j}^v)_{mn} &= \left\langle \lambda_m^{\Lambda_j}(\mathbf{r}), \nabla \mathcal{V} \lambda_n^{\Lambda_i}(\mathbf{r}) \right\rangle_{\Lambda}, \\
(\mathbf{G}_{\Lambda_i}^v)_{mn} &= \left\langle \lambda_m^{\Lambda_i}(\mathbf{r}), (\underline{I} - \underline{\kappa}) \lambda_n^{\Lambda_i}(\mathbf{r}) \right\rangle_{\Lambda}, \\
(\mathbf{D}_{\Gamma_i \Lambda_j}^v)_{mn} &= (\sigma_{i+1} - \sigma_i) \left\langle \lambda_m^{\Lambda_j}(\mathbf{r}), \nabla \mathcal{D} \psi_n^{\Gamma_i}(\mathbf{r}) \right\rangle_{\Lambda}, \\
(\mathbf{V}_{\Lambda_i \Gamma_j}^s)_{mn} &= \left\langle \psi_m^{\Gamma_j}(\mathbf{r}), \mathcal{V} \lambda_n^{\Lambda_i}(\mathbf{r}) \right\rangle_{\Gamma}, \\
(\mathbf{D}_{\Gamma_i \Gamma_j}^s)_{mn} &= (\sigma_{i+1} - \sigma_i) \left\langle \psi_m^{\Gamma_j}(\mathbf{r}), \mathcal{D} \psi_n^{\Gamma_i}(\mathbf{r}) \right\rangle_{\Gamma}, \\
(\mathbf{G}_{\Gamma_i}^s)_{mn} &= \frac{(\sigma_{i+1} + \sigma_i)}{2} \left\langle \psi_m^{\Gamma_i}(\mathbf{r}), \psi_n^{\Gamma_i}(\mathbf{r}) \right\rangle_{\Gamma},
\end{aligned}$$

and, $\langle f, g \rangle_x = \int_x f \cdot g \, dx$ denotes the duality product. The entries of the right-hand side are

$$\begin{aligned}
(\mathbf{w}_{\Lambda})_m &= \left\langle \lambda_m(\mathbf{r}), \nabla \mathcal{V} \text{dip}(\mathbf{r}) \right\rangle_{\Lambda}, \\
(\mathbf{v}_{d\Gamma})_m &= \left\langle \psi_m(\mathbf{r}), \mathcal{V} \text{dip}(\mathbf{r}) \right\rangle_{\Gamma}.
\end{aligned}$$

One of the attractive features pertaining to integral operators is that by specifying their data at the boundaries and on the fibers, it is possible to get the potential everywhere in the head domain. By solving the (DLW) equation system formulation, the potential is recovered at the vertices of the mesh. It follows that this potential can be easily computed at random position on the boundaries by a simple interpolation. If however the potential is desired at location that does not belong to the boundaries, we can use the following equation

$$\phi(\mathbf{r}) = \frac{1}{\sigma_j} * \left[\sigma_1 \mathcal{V} \text{dip}(\mathbf{r}) - \sigma_1 \sum_{k=1}^{N_f} \mathcal{V} \mathbb{J}_{\Lambda_k}(\mathbf{r}) + \sum_{i=1}^N (\sigma_{i+1} - \sigma_i) (\mathcal{D} \phi|_{\Gamma_i})(\mathbf{r}) \right] \quad (41)$$

where σ_j is the local conductivity of the evaluation point.

4.2. Discretization of the single layer-wire formulation

Similarly to the previous approach, the surface unknown q in eqs. (29) and (31) is discretized with pyramid basis functions and the current density \mathbb{J} is discretized with hat basis functions. Equations (29) and (31) are then tested with pyramid and hat functions respectively. This gives rise to the system

$$\begin{bmatrix} \mathbf{G}_{\Lambda_i}^v + \mathbf{V}_{\Lambda_i \Lambda_j}^v & | & \mathbf{K}_{\Gamma_i \Lambda_j}^v \\ \mathbf{W}_{\Lambda_i \Gamma_j}^s & | & \mathbf{G}_{\Gamma_i}^s + \mathbf{K}_{\Gamma_i \Gamma_j}^s \end{bmatrix} \begin{bmatrix} \mathbf{J} \\ \mathbf{q} \end{bmatrix} = \begin{bmatrix} \mathbf{w}_{\Lambda} \\ \mathbf{v}_{s\Gamma} \end{bmatrix} \quad (42)$$

where the matrix entries are

$$\begin{aligned}
(\mathbf{V}_{\Lambda_i \Lambda_j}^v)_{mn} &= \left\langle \lambda_m^{\Lambda_j}(\mathbf{r}), \nabla \mathcal{V} \lambda_n^{\Lambda_i}(\mathbf{r}) \right\rangle_{\Lambda}, \\
(\mathbf{G}_{\Lambda_i}^v)_{mn} &= \left\langle \lambda_m^{\Lambda_i}(\mathbf{r}), (\underline{I} - \underline{\kappa}) \lambda_n^{\Lambda_i}(\mathbf{r}) \right\rangle_{\Lambda}, \\
(\mathbf{K}_{\Gamma_i \Lambda_j}^v)_{mn} &= \left\langle \lambda_m^{\Lambda_j}(\mathbf{r}), \mathcal{K} \psi_n^{\Gamma_i}(\mathbf{r}) \right\rangle_{\Lambda}, \\
(\mathbf{W}_{\Lambda_i \Gamma_j}^s)_{mn} &= \left\langle \psi_m^{\Gamma_j}(\mathbf{r}), \mathcal{V} \lambda_n^{\Lambda_i}(\mathbf{r}) \right\rangle_{\Gamma}, \\
(\mathbf{G}_{\Gamma_i}^s)_{mn} &= \frac{(\sigma_{i+1} + \sigma_i)}{2(\sigma_{i+1} - \sigma_i)} \left\langle \psi_m^{\Gamma_i}(\mathbf{r}), \psi_n^{\Gamma_i}(\mathbf{r}) \right\rangle_{\Gamma}, \\
(\mathbf{K}_{\Gamma_i \Gamma_j}^s)_{mn} &= \left\langle \psi_m^{\Gamma_j}(\mathbf{r}), \mathcal{K} \psi_n^{\Gamma_i}(\mathbf{r}) \right\rangle_{\Gamma},
\end{aligned}$$

and where the entries of the right-hand side are

$$\begin{aligned}
(\mathbf{w}_{\Lambda})_m &= \left\langle \lambda_m(\mathbf{r}), \nabla \mathcal{V} \text{dip}(\mathbf{r}) \right\rangle_{\Lambda}, \\
(\mathbf{v}_{s\Gamma})_m &= \left\langle \psi_m(\mathbf{r}), \mathcal{V}_s(\mathbf{r}) \right\rangle_{\Gamma}.
\end{aligned}$$

After solving this system of equations, the electric potential in the head can be computed via eq. (30).

Table 1

Definition of the different coefficients associated with the discretization of the symmetric formulation.

Condition	α_{ij}	β_{ij}	γ_{ij}	θ_j
$j = 1$	—	—	—	1
$j = i$	$\sigma_i + \sigma_j$	-2	$\sigma_i^{-1} + \sigma_j^{-1}$	—
$j = i - 1$	$-\sigma_i$	1	$-\sigma_i^{-1}$	—
$j = i + 1$	$-\sigma_j$	1	$-\sigma_j^{-1}$	—
otherwise	0	0	0	0

4.3. Discretization of the symmetric-wire formulation

In contrast with the two previous approaches, the symmetric formulation (eqs. (33) to (35)) has two surface unknowns: the potential ϕ that we discretize with pyramid basis functions, the current flux with patch basis functions and the current density \mathbb{J} with hat basis functions. Equations (33) to (35) are tested with patch, pyramid and hat basis functions respectively, resulting in the following system of equations

$$\begin{bmatrix} \mathbf{G}_{\Lambda_i}^v - \mathbf{V}_{\Lambda_i \Lambda_j} & \mathbf{D}_{\Gamma_n \Lambda_m}^v & \mathbf{S}_{\Gamma_n \Lambda_m}^v \\ \mathbf{W}_{\Lambda_i \Gamma_j}^s & \mathbf{N}_{\Gamma_i \Gamma_j}^s & \mathbf{K}_{\Gamma_i \Gamma_j}^s \\ \mathbf{V}_{\Lambda_m \Gamma_n}^s & \mathbf{D}_{\Gamma_i \Gamma_j}^s & \mathbf{S}_{\Gamma_i \Gamma_j}^s \end{bmatrix} \begin{bmatrix} \mathbf{J} \\ \phi \\ \mathbf{d} \end{bmatrix} = \begin{bmatrix} \mathbf{w}_\Lambda \\ \mathbf{V}_{s\Gamma} \\ \mathbf{V}_{d\Gamma} \end{bmatrix} \quad (43)$$

in which the system entries are defined as

$$\begin{aligned} (\mathbf{V}_{\Lambda_i \Lambda_j}^v)_{mn} &= \left\langle \lambda_m^{\Lambda_j}(\mathbf{r}), \nabla \mathcal{V} \lambda_n^{\Lambda_i}(\mathbf{r}) \right\rangle_\Lambda, \\ (\mathbf{G}_{\Lambda_i}^v)_{mn} &= \left\langle \lambda_m^{\Lambda_i}(\mathbf{r}), (\underline{1} - \underline{\kappa}) \lambda_n^{\Lambda_i}(\mathbf{r}) \right\rangle_\Lambda, \\ (\mathbf{D}_{\Gamma_i \Lambda_j}^v)_{mn} &= \left\langle \lambda_m^{\Lambda_j}(\mathbf{r}), \theta_i \mathcal{D} \psi_n^{\Gamma_i}(\mathbf{r}) \right\rangle_\Lambda, \\ (\mathbf{S}_{\Gamma_i \Lambda_j}^v)_{mn} &= \left\langle \lambda_m^{\Lambda_j}(\mathbf{r}), \theta_i \mathcal{S} \psi_n^{\Gamma_i}(\mathbf{r}) \right\rangle_\Lambda, \\ (\mathbf{W}_{\Lambda_i \Gamma_j}^s)_{mn} &= \left\langle \psi_m^{\Gamma_j}(\mathbf{r}), \theta_j \mathcal{W} \lambda_n^{\Lambda_i}(\mathbf{r}) \right\rangle_\Gamma, \\ (\mathbf{V}_{\Lambda_i \Gamma_j}^s)_{mn} &= \left\langle \psi_m^{\Gamma_j}(\mathbf{r}), \theta_j \mathcal{V} \lambda_n^{\Lambda_i}(\mathbf{r}) \right\rangle_\Gamma, \\ (\mathbf{N}_{\Gamma_i \Gamma_j}^s)_{mn} &= \left\langle \psi_m^{\Gamma_j}(\mathbf{r}), \alpha_{ij} \mathcal{N} \psi_n^{\Gamma_i}(\mathbf{r}) \right\rangle_\Gamma, \\ (\mathbf{K}_{\Gamma_i \Gamma_j}^s)_{mn} &= \left\langle \psi_m^{\Gamma_j}(\mathbf{r}), \beta_{ij} \mathcal{K} \varphi_n^{\Gamma_i}(\mathbf{r}) \right\rangle_\Gamma, \\ (\mathbf{D}_{\Gamma_i \Gamma_j}^s)_{mn} &= \left\langle \varphi_m^{\Gamma_j}(\mathbf{r}), \beta_{ij} \mathcal{D} \psi_n^{\Gamma_i}(\mathbf{r}) \right\rangle_\Gamma, \\ (\mathbf{S}_{\Gamma_i \Gamma_j}^s)_{mn} &= \left\langle \varphi_m^{\Gamma_j}(\mathbf{r}), \gamma_{ij} \mathcal{S} \varphi_n^{\Gamma_i}(\mathbf{r}) \right\rangle_\Gamma, \end{aligned}$$

the entries of the right-hand side are

$$\begin{aligned} (\mathbf{w}_{\Lambda_j})_m &= \left\langle \lambda_m^{\Lambda_j}(\mathbf{r}), \nabla \mathcal{V} \text{dip}(\mathbf{r}) \right\rangle_\Lambda, \\ (\mathbf{v}_{d\Gamma_j})_m &= \left\langle \psi_m^{\Gamma_j}(\mathbf{r}), \theta_j \mathcal{V} \text{dip}(\mathbf{r}) \right\rangle_\Gamma, \\ (\mathbf{V}_{s\Gamma_j})_m &= \left\langle \psi_m^{\Gamma_j}(\mathbf{r}), \theta_j \mathcal{V} s(\mathbf{r}) \right\rangle_\Gamma, \end{aligned}$$

and the coefficients α , β , γ and θ are defined in Table 1.

By solving this system, we obtain the potential at all the nodes of the interface's mesh. If the points of interest are on the mesh, the potential can be recovered by interpolation. If the points of interest are not located on the mesh, one can use either eq. (41) or eq. (18).



Fig. 4. Anisotropic cube inside a three layered sphere: (a) reference model and (b) simulated model.

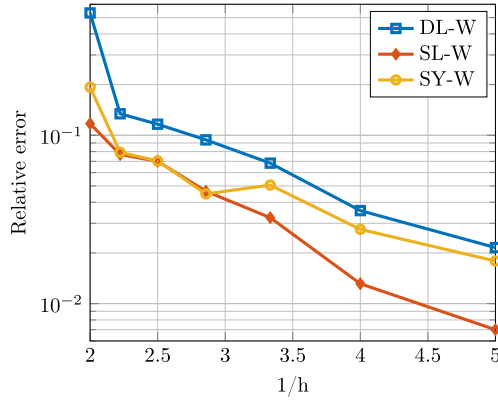


Fig. 5. The relative error of the DLW, SLW and SYW formulations as a function of the average edge length which shows the convergence of the solutions to the reference solution obtained with FEM. The simulated geometry is illustrated in Fig. 4.

5. Numerical results

In this section the newly developed integral formulations are validated and their performances are studied through several numerical examples. The parameters of the simulations are given in normalized units and the systems of equations are solved with direct inversion via LU factorization and backward substitution.

5.1. Convergence of the solution

In order to demonstrate that the proposed formulations are capable of capturing the anisotropic conductivity and do converge to the exact solution, we have simulated a cubic block whose anisotropic conductivity is 10 along the z axis and 1 in the (x, y) plane, residing inside a three layered sphere (Fig. 4(a)). The radii of the spheres are 0.87, 0.92 and 1 respectively. The cube, whose side length is equal to 0.7, is placed at their center. The conductivities of the different spheres are 1, 1/15 and 1 respectively. A current source with a dipolar moment equal to $[1, 1, 1]$ is set at $[0.4, 0, 0]$. In order to account for the anisotropic effect of the cube with our formulations, we have created a grid of 64 equally spaced fiber, as illustrated in Fig. 4(b). The wires have a radius of 0.05 and their conductivity is set to be 10 along the wires and 1 in their transverse direction. A convergence analysis has been carried out in which the model is discretized with increasingly refined mesh (the number of wires has been kept constant). Note that we could have solved and used as reference the scenario shown in Fig. 4(b) using a highly refined mesh, but we opted to use the structure of Fig. 4(a) with FEM. We made this choice to validate and illustrate the merits of our new schemes by selecting a different modelization (wire elements) of the underlying physics (volume).

Fig. 5 reports the obtained relative error as a function of the mesh edge length; a FEM solution corresponding to highly refined mesh (1 443 230 nodes) is used as reference. The relative error is defined as the following dimensionless quantity

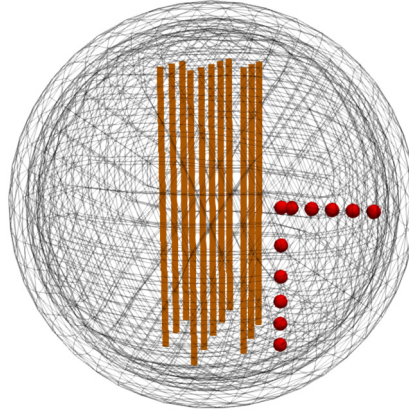
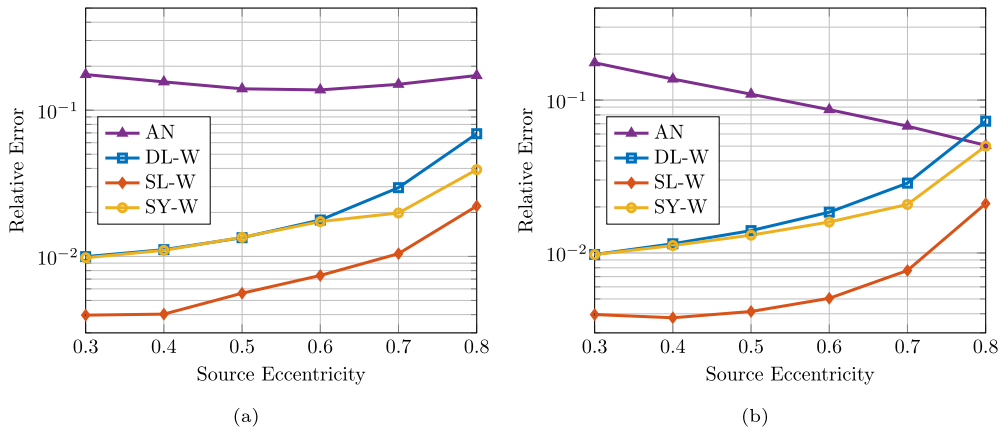
$$RE = \frac{|\mathbf{y}_{ref} - \mathbf{y}|}{|\mathbf{y}_{ref}|} \quad (44)$$

in which \mathbf{y}_{ref} and \mathbf{y} denote the solution and the reference solution in that order. From Fig. 5, we can see that the three formulations converge to the reference solution with a convergence order of approximately $O(h^2)$ and can indeed account for the anisotropy of the medium.

Table 2

Coordinates of the wires in the xy plane corresponding to Fig. 6.

x	-0.4	-0.2	0	0.2	0.4	-0.2	0	0.2	-0.2	0	0.2
y	0	0	0	0	0	-0.2	-0.2	-0.2	0.2	0.2	0.2

**Fig. 6.** Geometry of the simulated model; the red dots indicate the position of the current sources.**Fig. 7.** Relative error of the different formulations as a function of dipole eccentricity: (a) along the fibers and (b) away from the fibers. The simulated geometry as well as the dipole sources are shown in Fig. 6 where a refined FEM solution was used as a reference. In the legend, AN refers to the analytical solution of the corresponding spherical geometry in the absence of the fibers.

5.2. Accuracy for different dipole eccentricities

In the second test, we have studied the effect of source eccentricity on the computed potential. Three concentric spheres of radius 0.87, 0.92 and 1 have been considered. Eleven vertical fibers of radius 0.05 were set at the coordinates summarized in Table 2. The conductivities of the different layers of the sphere were set to 1, 1/15 and 1 and the fibers to 10 along the z direction and 1 in the transversal direction. The model was discretized with 642 nodes per surface and 15 segments per fiber. The forward problem was then solved for a varying dipole position: along and away from the fibers as shown in Fig. 6 with red dots. The computed relative error, where a high resolution FEM was used as a reference, is shown in Figs. 7(a) and 7(b) for the two cases. In order to illustrate the error introduced when neglecting the anisotropic conductivity of the fibers, we have also included the relative error produced by the analytic solution of the same spherical model in the absence of the fibers.

In general the accuracy of the three numerical solutions decreases for shallow sources. This behavior is due to the singularity of the source and is in agreement with what has been reported in the literature [12,35,36]. It is also observed that not accounting for the anisotropic conductivity of the fibers leads to higher errors, especially in vicinity of the fibers. As expected, these errors decrease when the source is moved away from the fibers (Fig. 7(b)) and remains stable when moving in their vicinity (Fig. 7(a)).

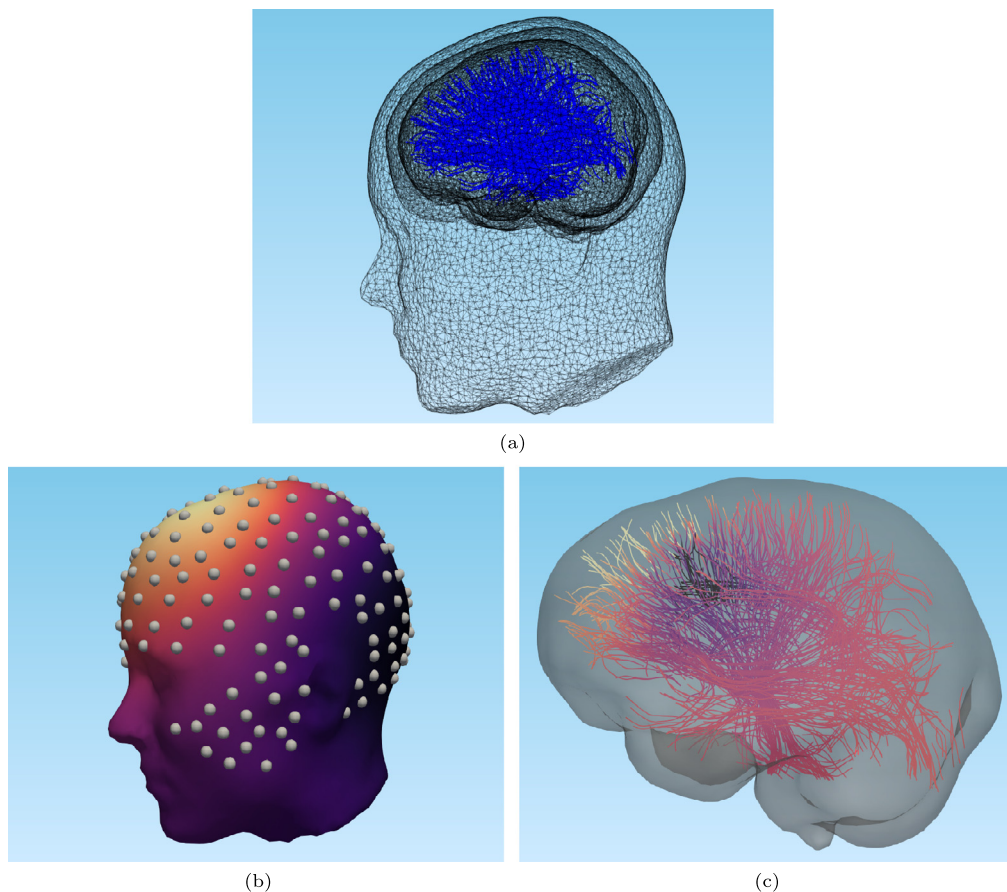


Fig. 8. MRI-based head model: (a) the simulated head model composed of white matter fibers, brain, skull and scalp surfaces; (b) computed distribution of the electric potential on the scalp, the dots indicate the position of electrodes of a high density EEG device; (c) magnitude of the calculated current density along the fibers.

5.3. Application to a realistic head mesh

As a last numerical test, a realistic head model obtained from MRI images is considered (Fig. 8(a)). Using standard procedures (see for example [37]), we have constructed a 3 layered mesh in which each domain represents the brain, the skull and the scalp, each of which is made of 6248, 8328 and 9346 triangles, respectively. Furthermore, the white matter fibers, made of 23888 segments, are recovered using DTI-based tractography implemented in [38]. The conductivity of the different tissues is set to 0.33, 0.022 and 0.33 for the scalp, skull and brain respectively [39]. The conductivity of the fibers is set to be 0.33 in their local transverse direction and 10 times greater in their longitudinal direction. Following the EGI system [40], a set of 256 electrodes has been placed on the scalp as shown in Fig. 8(b). At these positions, the electric potential was computed using the newly introduced schemes. For the sake of comparison, we have also computed the solution with FEM, on a volume mesh of 10 million tetrahedrons. We show the results obtained in Fig. 9, where we observe that the four formulations are in agreement with a relative error less than 0.8%. In Fig. 8(c), we plot the magnitude of the current density along the fibers.

6. Conclusion

The correct modeling of the electric properties of the head is crucial for an accurate forward solution and, consequently, for brain source reconstruction. This includes the anisotropic behavior of the white matter, given its impact on the scalp potential. In this paper, we have presented new integral techniques that can handle the anisotropic conductivity profile of the head and thus extend the application of conventional BEM approaches. The one dimensional nature of the wire basis functions ensures the computational efficiency of the schemes. It has been shown throughout several numerical tests that the computed potential exhibit high accuracy and stability making it a competitive alternative to differential equations based methods. Given that the different approaches that we have presented share the same surface equation with standard BEM techniques (double layer, adjoint double layer and symmetric formulation), they inherit some of their properties, merits and disadvantages: (i) the accuracy of the different formulations matches, in general, the ones observed with purely surfacic

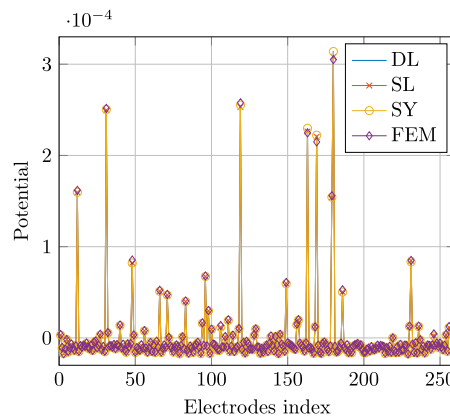


Fig. 9. Electric potential computed at electrodes position shown in Fig. 8(b).

counterparts [11,12]; in particular their precision is higher for deep sources and degrades gradually for shallower sources. Several strategies, that equally apply to our equations, have been proposed in the literature such as adaptive discretization or opting for less singular source; (ii) similarly, the number of unknowns in discretizing a particular mesh is higher in the symmetric formulation (because it entails two surface equations), though the system is band diagonal. (iii) the accuracy also depends on the conductivity ratio, for which the symmetric formulation was shown to handle better the high contrast. Recently, several techniques have been introduced to make the DL and SL cope better with the high contrast [9,11]. Those techniques are compatible with our equations; (iv) lastly, the DL-W and SL-W are integral equations of the second kind, which translate into well-conditioned systems with h-refinement, the SY-W, however has two surface integral equations of the first kind; this suggests an ill-conditioning for an increasing mesh density. A preconditioner based on Calderón identities has been recently proposed [41] that effectively stabilizes the condition number and can be easily adapted to the proposed scheme.

Declaration of competing interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

Acknowledgement

This work has been funded in part by the European Research Council (ERC) under the European Union's Horizon 2020 research and innovation program (ERC project 321, grant No. 724846).

References

- [1] G. Thut, C. Miniussi, New insights into rhythmic brain activity from tms-*eeg* studies, *Trends Cogn. Sci.* 13 (4) (2009) 182–189.
- [2] A. Van Cott, R.P. Brenner, Technical advantages of digital *eeg*, *J. Clin. Neurophysiol.* 15 (6) (1998) 464–475.
- [3] P. Nemtsas, G. Birot, F. Pittau, C.M. Michel, K. Schaller, S. Vulliemoz, V.K. Kimiskidis, M. Seeck, Source localization of ictal epileptic activity based on high-density scalp *eeg* data, *Epilepsia* 58 (6) (2017) 1027–1036.
- [4] R.D. Pascual-Marqui, Review of methods for solving the *eeg* inverse problem, *Int. J. Bioelectromagn.* 1 (1) (1999) 75–86.
- [5] T. Hedrich, G. Pellegrino, E. Kobayashi, J. Lina, C. Grova, Comparison of the spatial resolution of source imaging techniques in high-density *eeg* and *meg*, *NeuroImage* 157 (2017) 531–544.
- [6] P. Khosropanah, A.R. Ramli, K.S. Lim, M.H. Marhaban, A. Ahmedov, Fused multivariate empirical mode decomposition (memd) and inverse solution method for *eeg* source localization, *Biomed. Eng./Biomed. Tech.* 63 (4) (2018) 467–479.
- [7] L. Greengard, S. Wandzura, Fast multipole methods, *IEEE Comput. Sci. Eng.* 5 (3) (1998) 16–18.
- [8] J. Ostrowski, Z. Andjelic, M. Bebendorf, B. Cranganu-Cretu, J. Smajic, Fast bem-solution of Laplace problems with h-matrices and aca, *IEEE Trans. Magn.* 42 (4) (2006) 627–630.
- [9] M. Stenroos, J. Sarvas, Bioelectromagnetic forward problem: isolated source approach revis (it) ed, *Phys. Med. Biol.* 57 (11) (2012) 3517.
- [10] G. Adde, M. Clerc, O. Faugeras, R. Keriven, J. Kybic, T. Papadopoulos, Symmetric bem formulation for the *m/eeg* forward problem, in: *Information Processing in Medical Imaging*, Springer, 2003, pp. 524–535.
- [11] L. Rahmouni, S.B. Adrian, K. Cools, F.P. Andriulli, Conforming discretizations of boundary element solutions to the electroencephalography forward problem, *C. R. Phys.* 19 (1–2) (2018) 7–25.
- [12] J. Kybic, M. Clerc, T. Abboud, O. Faugeras, R. Keriven, T. Papadopoulos, A common formalism for the integral formulations of the forward *eeg* problem, *IEEE Trans. Med. Imaging* 24 (1) (2005) 12–28.
- [13] A. Pillain, L. Rahmouni, F.P. Andriulli, On the handling of brain tissue anisotropy in the forward *eeg* problem with a conformingly discretized surface integral method, in: *Biomedical Imaging (ISBI), 2016 IEEE 13th International Symposium on*, IEEE, 2016, pp. 233–236.
- [14] Carsten Hermann Wolters, Alfred Anwander, X. Tricoche, D. Weinstein, Martin A. Koch, R.S. MacLeod, Influence of tissue conductivity anisotropy on *eeg/meg* field and return current computation in a realistic head model: a simulation and visualization study using high-resolution finite element modeling, *NeuroImage* 30 (3) (2006) 813–826.

- [15] J. Hauelsen, D.S. Tuch, C. Ramon, P. Schimpf, V. Wedeen, J. George, J. Belliveau, The influence of brain tissue anisotropy on human eeg and meg, *NeuroImage* 15 (1) (2002) 159–166.
- [16] L. Rahmouni, R. Mitharwal, F.P. Andriulli, Two volume integral equations for the inhomogeneous and anisotropic forward problem in electroencephalography, *J. Comput. Phys.* 348 (2017) 732–743.
- [17] O. Friman, G. Farneback, C.-F. Westin, A Bayesian approach for stochastic white matter tractography, *IEEE Trans. Med. Imaging* 25 (8) (2006) 965–978.
- [18] M. Lazar, D.M. Weinstein, J.S. Tsuruda, K.M. Hasan, K. Arfanakis, M.E. Meyerand, B. Badie, H.A. Rowley, V. Haughton, A. Field, et al., White matter tractography using diffusion tensor deflection, *Hum. Brain Mapp.* 18 (4) (2003) 306–321.
- [19] E. Olivi, T. Papadopoulou, M. Clerc, Handling white-matter anisotropy in BEM for the EEG forward problem, in: *Proceedings of the 8th IEEE International Symposium on Biomedical Imaging: From Nano to Macro, ISBI 2011, IEEE, 2011*, pp. 799–802, <https://hal.inria.fr/inria-00578876/document>.
- [20] S.N. Makarov, A. Pascual-Leone, A. Nummenmaa, Modeling fiber-like conductivity structures via the boundary element method using thin-wire approximation. I construction of basis functions, in: *2016 38th Annual International Conference of the IEEE Engineering in Medicine and Biology Society (EMBC), IEEE, 2016*, pp. 6473–6476.
- [21] A. Pillain, Line, surface, and volume integral equations for the electromagnetic modelling of the electroencephalography forward problem, Ph.D. thesis, Ecole Nationale Supérieure des Télécommunications de Bretagne-ENSTB, 2016.
- [22] R.B. Mars, S. Jbabdi, J. Sallet, J.X. O'Reilly, P.L. Croxson, E. Olivier, M.P. Noonan, C. Bergmann, A.S. Mitchell, M.G. Baxter, et al., Diffusion-weighted imaging tractography-based parcellation of the human parietal cortex and comparison with human and macaque resting-state functional connectivity, *J. Neurosci.* 31 (11) (2011) 4087–4100.
- [23] D.K. Hammond, B. Scherrer, S.K. Warfield, Cortical graph smoothing: a novel method for exploiting dwi-derived anatomical brain connectivity to improve eeg source estimation, *IEEE Trans. Med. Imaging* 32 (10) (2013) 1952–1963.
- [24] D.K. Hammond, B. Scherrer, A. Malony, Incorporating anatomical connectivity into eeg source estimation via sparse approximation with cortical graph wavelets, in: *Acoustics, Speech and Signal Processing (ICASSP), 2012 IEEE International Conference on, IEEE, 2012*, pp. 573–576.
- [25] L. Rahmouni, A. Pillain, A. Merlini, F.P. Andriulli, Integral equation modelling of brain fibers for handling white matter anisotropies in the eeg forward problem, in: *Electromagnetics in Advanced Applications (ICEAA), 2017 International Conference on, IEEE, 2017*, pp. 1809–1812.
- [26] P.J. Papakanellos, P. Paschalidis, G. Fikioris, On the extended thin-wire kernel, *IEEE Trans. Antennas Propag.* 64 (7) (2016) 3180–3184.
- [27] A. Mohan, D.S. Weile, Accurate modeling of the cylindrical wire kernel, *Microw. Opt. Technol. Lett.* 48 (4) (2006) 740–744.
- [28] D.R. Wilton, N.J. Champagne, Evaluation and integration of the thin wire kernel, *IEEE Trans. Antennas Propag.* 54 (4) (2006) 1200–1206.
- [29] D. Werring, C. Clark, G. Barker, A. Thompson, D. Miller, Diffusion tensor imaging of lesions and normal-appearing white matter in multiple sclerosis, *Neurology* 52 (8) (1999) 1626.
- [30] W.C. Chen, S. Foxley, K.L. Miller, Detecting microstructural properties of white matter based on compartmentalization of magnetic susceptibility, *NeuroImage* 70 (2013) 1–9.
- [31] C.H. Wolters, Influence of tissue conductivity inhomogeneity and anisotropy on eeg/meg based source localization in the human brain, Ph.D. thesis, Max Planck Institute of Cognitive Neuroscience Leipzig, 2003.
- [32] J. De Munck, B. Van Dijk, H. Spekreijse, Mathematical dipoles are adequate to describe realistic generators of human brain activity, *IEEE Trans. Biomed. Eng.* 35 (11) (1988) 960–966.
- [33] J. Sarvas, Basic mathematical and electromagnetic concepts of the biomagnetic inverse problem, *Phys. Med. Biol.* 32 (1) (1987) 11.
- [34] O. Steinbach, *Numerical Approximation Methods for Elliptic Boundary Value Problems: Finite and Boundary Elements*, Springer Science & Business Media, 2007.
- [35] J. Vorwerk, C. Engwer, S. Pursiainen, C.H. Wolters, A mixed finite element method to solve the eeg forward problem, *IEEE Trans. Med. Imaging* 36 (4) (2017) 930–941.
- [36] L. Rahmouni, S.B. Adrian, K. Cools, F.P. Andriulli, A mixed discretized adjoint double layer formulation for the electroencephalography forward problem with high brain-skull contrast ratios, in: *Electromagnetics in Advanced Applications (ICEAA), 2017 International Conference on, IEEE, 2017*, pp. 1817–1820.
- [37] M. Windhoff, A. Opitz, A. Thielscher, Electric field calculations in brain stimulation based on finite elements: an optimized processing pipeline for the generation and usage of accurate individual head models, *Hum. Brain Mapp.* 34 (4) (2013) 923–935.
- [38] N. Toussaint, J.-C. Souplet, P. Fillard, et al., Medinria: medical image navigation and research tool by inria, in: *Proc. of MICCAI*, vol. 7, 2007, p. 280.
- [39] T.F. Oostendorp, J. Delbeke, D.F. Stegeman, The conductivity of the human skull: results of in vivo and in vitro measurements, *IEEE Trans. Biomed. Eng.* 47 (11) (2000) 1487–1492.
- [40] P. Luu, T. Ferree, Determination of the hydrocel geodesic sensor nets' average electrode positions and their 10–10 international equivalents, Inc, *Technical Note*.
- [41] A. Pillain, L. Rahmouni, F.P. Andriulli, et al., A Calderon regularized symmetric formulation for the electroencephalography forward problem, *J. Comput. Phys.* 375 (2018) 291–306.