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# Dynamic modeling and experimental validation of a haptic finger based on a McKibben muscle

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**Abstract** The paper deals with the implementation of a McKibben pneumatic muscle in a tele-operation robotic system provided with haptic feedback, aimed to the generation of the perception force at the operator's fingertip. The architecture of the device is presented and a dynamic model of the system is proposed. A prototype of the device has been tested in dynamic conditions, and the outcomes have been compared with the numerical results, highlighting that the use of a pneumatic muscle is suitable for the actuation of a haptic finger device.

**Keywords:** Pneumatic artificial muscle, McKibben muscle, Haptics, Teleoperation, Force reflection, Hand exoskeleton, Human-machine interaction

## 1. Introduction

Teleoperation deals with the remote control of a device (slave). The teleoperation interface (master) is called *haptic* if able to transmit a force feedback to the operator's hand. In this case, the perception force must be generated by controlled actuators, whose mechanical impedance is relevant to allow the correct human-machine interaction.

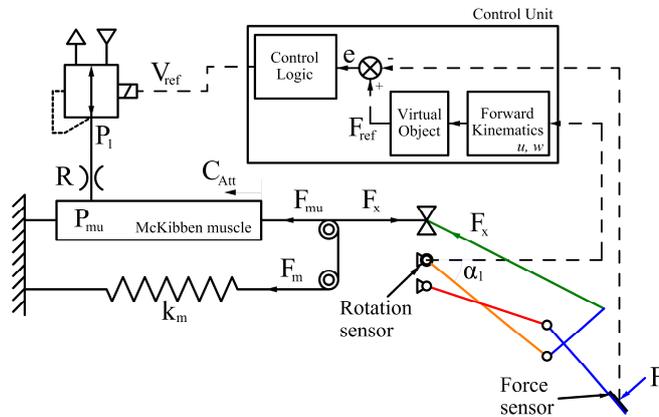
Due to their intrinsic self-adaptability to the compliance of the biological tissues, non-conventional deformable actuators, as shape memory alloy actuators [1] or pneumatic deformable actuators [2], may be employed for this purpose. Among the latter, the McKibben pneumatic artificial muscle has been integrated in several haptic manipulators and gloves [3-6].

The aim of this work is to study the feasibility of a haptic device whose architecture is based on a single degree-of-freedom mechanism driven by a McKibben muscle actuator. In the paper, the structure of the device is outlined, and a dynamic mathematical model of the system is described. The performance of the real system has been tested in a virtual environment, evaluating the force exerted on

the operator's finger during a manipulation task. Then, the results of the simulation have been compared to the experimental data in order to validate the model.

## 2. The device

The device, whose scheme is shown in Figure 1, consists of: a four-bar linkage able to generate a desired path of the index fingertip support; a rotary encoder (Baumer electric, BDK series), used to measure the rotation of one of the links, so as to perform the forward kinematic analysis of the mechanism and calculate the position of the fingertip; a planar beam force sensor (FUTEK Advanced Sensor Technology, Inc., FR1020, maximum load 89N) for the measurement of the force applied to the fingertip, providing the required feedback signal to the perception force control loop; a control unit, that, considering the geometrical and mechanical characteristic of the selected virtual object, generates the force reference signal and the command for the actuator; an actuation system, composed by a McKibben pneumatic muscle (Shadow Robot Company Ltd., London), preloaded with a parallel spring (SPEC<sup>®</sup> T41660) and supplied by a pressure control proportional valve (FESTO<sup>®</sup> MPPE-3-1/4-10-010B), driving the coupler of the four-bar mechanism through the application of a tensile force to a polyethylene fiber tendon. The device architecture has been detailed in [7]. The control logic has been developed in MATLAB-Simulink<sup>®</sup> and implemented by means of dSpace<sup>®</sup> boards and a user interface designed in ControlDesk<sup>®</sup>.



**Fig. 1.** Scheme of the haptic device.

In Figure 2 the prototype of the device is depicted. The operator rests his hand on the fixed frame of the device, while his fingertip is held by a specially designed support integral with the force sensor mounted on the coupler of the four-bar mechanism.

The operator moves the finger between the position of maximum extension and that of maximum flexion to perform the tele-manipulation of the remote device, and therefore imposes the rotation  $\alpha_l$  of the rocker, measured by the encoder.

Through the forward kinematics evaluation of the mechanism, the control unit calculates the position of the finger in the sagittal plane ( $u$ ,  $w$ ) and then, by definition of the shape and the mechanical characteristic of the virtual object, generates the reference force signal  $F_{ref}$ . The control unit calculates the error  $e$  between the force reference  $F_{ref}$  and the measured force  $F$ , and provides the command signal for the pressure control proportional valve  $V_{ref}$ , used to regulate the upstream pressure of the fluidic resistance  $p_l$ . Therefore, the muscle is supplied and consequently pulls the tendon that actuates the coupler of the four-bar mechanism.

As described in [8], the synthesis of the four-bar mechanism was carried out by ensuring that the trajectory of the point P (fingertip holder) should be included into the natural workspace of a finger, calculated by taking into account the dependency among the rotations of each joint (Figure 3a). The lengths of the proximal, middle and distal phalanxes selected are respectively 4 cm, 2.5 cm and 2 cm, while the rotation of the DIP joint has been considered equal to 2/3 of the PIP joint rotation.

The dimensions of the four-bar linkage (Figure 3b) are reported in Table 1. The operator's fingertip is positioned at point P, while the MCP joint is coincident with the fixed hinge O. The tendon 5 is connected to the coupler 2 in  $X_1$ , passes through the low-friction support point X, and is pulled by the McKibben muscle.

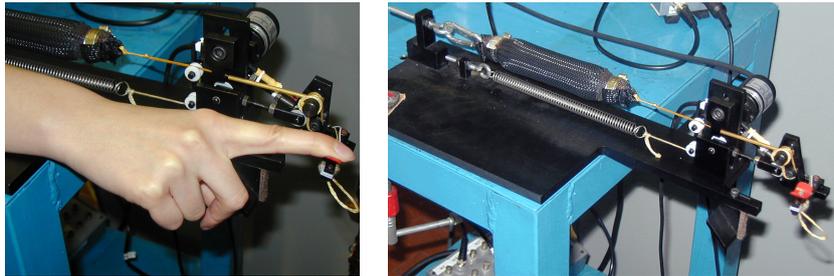


Fig. 2. The prototype of the device.

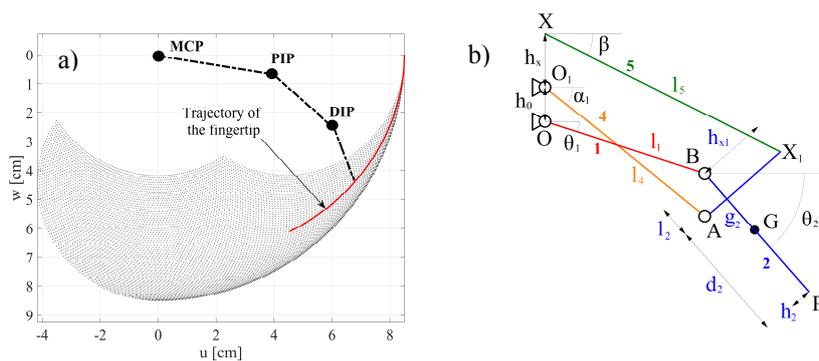


Fig. 3. a): workspace of a human index finger. b): sketch of the mechanism (metacarpophalangeal joint, MCP, proximal inter-phalangeal joint, PIP, and distal inter-phalangeal joint, DIP).

### 3. The dynamic mathematical model

The block diagram of the dynamic model of the device is presented in Figure 4:

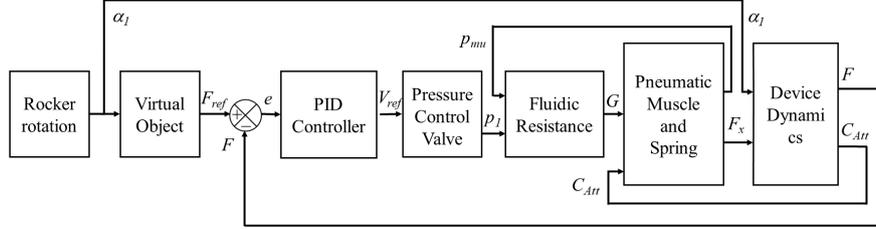


Fig. 4. Block diagram of the device model.

The *Device Dynamics* block calculates the feedback force  $F$  applied to the fingertip and the stroke of the McKibben muscle  $C_{Act}$ , starting from the rotation of the rocker  $\alpha_1$ , imposed by the operator, and the force  $F_x$  generated by the combination of the pneumatic muscle and the spring.

The positioning in the sagittal plane  $(u, w)$  of each link of the mechanism can be calculated solving the non-linear system of Eq. (1-3):

$$l_4 \cos \alpha_1 + h_2 \sin \vartheta_2 - l_2 \cos \vartheta_2 = l_1 \cos \vartheta_1 \quad (1)$$

$$l_4 \sin \alpha_1 - h_2 \cos \vartheta_2 - l_2 \sin \vartheta_2 - h_0 = l_1 \sin \vartheta_1 \quad (2)$$

$$\beta = \tan^{-1} \left( \frac{h_x + h_0 + l_1 \sin \vartheta_1 + l_2 \sin \vartheta_2 - h_{x1} \cos \vartheta_2}{l_1 \cos \vartheta_1 + l_2 \cos \vartheta_2 + h_{x1} \sin \vartheta_2} \right) \quad (3)$$

The stroke of the actuator  $C_{Act}$  depends on the length of the tendon  $l_5$  and the preload stroke of the spring,  $C_{Act1}$ , and is calculated by solving Eq. (4):

$$C_{Act} = l_{5\max} - l_5 + C_{Act1}, \quad l_5 = \frac{l_4 \cos \alpha_1 + (h_2 + h_{x1}) \sin \vartheta_2}{\cos \beta} \quad (4)$$

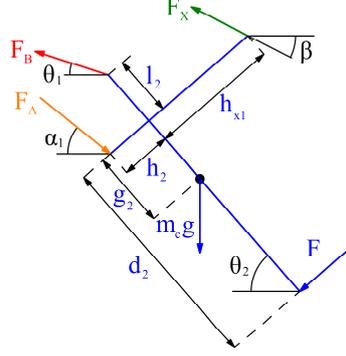
The value of  $l_{5\max}$  corresponds to the maximum length  $XX_1$  of the tendon (Figure 3b), that is at the maximum flexion of the finger. The trajectory of the fingertip in the  $(u, w)$  plane (Figure 3a) is then calculated.

The force  $F$  applied to the fingertip is evaluated for each value of  $\alpha_1$  considering the equilibrium of link 2 (Figure 5). The direction of  $F$  is considered as perpendicular to the link 2 in point P due to sliding between the fingertip and the support. The equivalent mass of the system  $m_c$  has been considered as centered at point G belonging to the link 2. The static analysis yields the following Eq. (5-7):

$$-F_B \cdot \cos \vartheta_1 + F_A \cdot \cos \alpha_1 - F_x \cdot \cos \beta = F \cdot \sin \vartheta_2 \quad (5)$$

$$F_B \cdot \sin \vartheta_1 - F_A \cdot \sin \alpha_1 + F_x \cdot \sin \beta = F \cdot \cos \vartheta_2 + m_c \cdot g \quad (6)$$

$$\begin{aligned}
& F_A \cdot [\cos \alpha_1 \cdot (l_2 \cdot \sin \vartheta_2 + h_2 \cdot \cos \vartheta_2) - \sin \alpha_1 \cdot (l_2 \cdot \cos \vartheta_2 + h_2 \cdot \sin \vartheta_2)] \\
& + F_x \cdot [\cos \beta \cdot (h_{x1} \cdot \cos \vartheta_2 - l_2 \cdot \sin \vartheta_2) + \sin \beta \cdot (h_{x1} \cdot \sin \vartheta_2 + l_2 \cdot \cos \vartheta_2)] \\
& = F \cdot (l_2 + d_2) + m_c \cdot g \cdot \cos \vartheta_2 \cdot (g_2 + l_2)
\end{aligned} \tag{7}$$



**Fig. 5.** The free body diagram of the coupler of the linkage.

Given the feedback force  $F$ , it is possible to calculate the force error  $e$ , being the force reference  $F_{ref}$  a function of the position of the fingertip, i.e. of the rocker  $\alpha_1$ :

$$e = F_{ref} - F \quad F_{ref} = F_{ref}(\alpha_1) \tag{8}$$

Due to its simplicity, a proportional-integral-derivative (PID) controller has been used:

$$V_{ref} = K_p e + K_I \int_0^t e dt + K_D \frac{de}{dt} \tag{9}$$

where  $K_p$ ,  $K_I$  and  $K_D$  are, respectively, the proportional, integral and derivative gains. An iterative approach has been used for the definition of the control logic parameters: finally, a simple proportional control came out to be sufficiently accurate and stable for the application.

A second order system transfer function has been used to simulate the dynamic behavior of the pressure control proportional valve (*Pressure Control Valve* block):

$$p_1 = \frac{K_V \sigma_n^2}{s^2 + 2\zeta \sigma_n s + \sigma_n^2} V_{ref} \tag{10}$$

where  $K_V$  is the static gain,  $\sigma_n$  the natural frequency and  $\zeta$  the damping factor of the valve.

The pneumatic resistance (*Fluidic Resistance* block) has been modeled according to the ISO 6358 [9]. The mass air flow passing through the resistance can be

calculated in sonic or subsonic condition depending on the ratio between the downstream and upstream pressures, as presented in Eq. (4):

$$G = \rho_0 P_1 C \text{ for } 0 < \frac{P_{mu}}{P_1} \leq b, \quad G = \rho_0 P_1 C \sqrt{1 - \left( \frac{P_{mu}/P_1 - b}{1-b} \right)^2} \text{ for } b < \frac{P_{mu}}{P_1} \leq 1 \quad (11)$$

where  $P_1$  is the upstream absolute pressure,  $P_{mu}$  is the downstream absolute pressure,  $C$  is the sonic conductance,  $b$  is the critical ratio and  $\rho_0=1.18 \text{ kg/m}^3$  is the air density in normal conditions. The  $C$  and  $b$  parameters are reported in Table 1.

Being  $R=287.2 \text{ J/(kgK)}$  the air constant,  $T$  the absolute air temperature, assuming the variation of the internal volume  $V$  of the pneumatic muscle as negligible, the time derivative of the absolute internal pressure of the muscle for an isothermal transformation can be expressed as:

$$\frac{dP_{mu}}{dt} = \frac{RT}{V} G = \frac{RT}{\pi r^2 l} G \quad (12)$$

with the actual  $l$  length and the radius  $r$  of the actuator given by [d]:

$$l = l_0 - C_{Att}, \quad r = \frac{\sqrt{h^2 - l^2}}{2\pi n_i} \quad (13)$$

where  $C_{Att}$  is the stroke of the pneumatic muscle whose initial pre-loaded length is  $l_0$ ,  $n_i$  is the number of turns of the fibers, whose length  $h$  is 178 mm for the employed McKibben muscle with 20 mm diameter.

The internal relative pressure of the muscle  $p_{mu}$  can be calculated integrating Eq. (12). Therefore, the force exerted by the muscle is given by Eq. (14) as a function of the internal pressure of the actuator [10]:

$$F_{mu} = -p_{mu} \frac{h^2 - l^2}{4\pi r_i^2} + E \frac{l - l_i}{l_i} 2r_i \pi s_i + \left[ p_{mu} l \frac{\sqrt{h^2 - l^2}}{2\pi r_i} - \frac{E s_i l}{r_i} \left( \frac{\sqrt{h^2 - l^2}}{2\pi r_i} - r_i \right) \right] \frac{l}{n_i \sqrt{h^2 - l^2}} \quad (14)$$

where  $r_i$  and  $l_i$  are respectively the initial radius and length of the muscle at rest,  $s_i$  is the initial thickness of the inner chamber,  $E$  is the Young modulus of the chamber.

Finally, the force  $F_x$  is directly connected to the force exerted by the muscle  $F_{mu}$  and the spring  $F_m$  by the following relations:

$$F_x = F_{mu} - F_m, \quad F_m = k_m \cdot C_{Att} + F_{m0} \quad (15)$$

where  $k_m$  is the spring constant, and  $F_{m0}$  its preload.

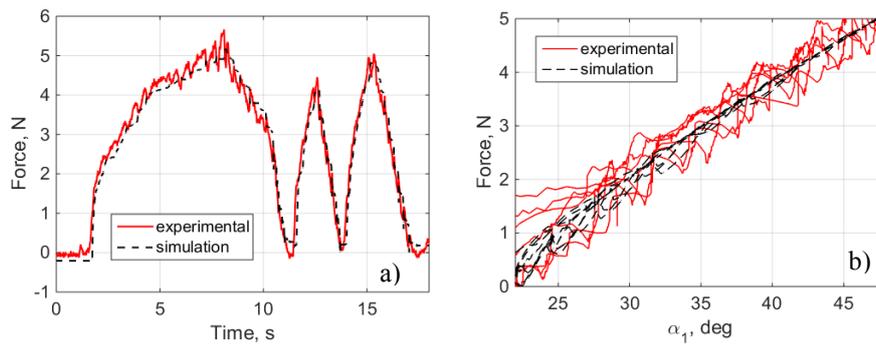
**Table 1.** Parameters of the model.

Parameter	Value	Parameter	Value	Parameter	Value
$l_1$	55 mm	$h_{x1}$	18 mm	$n_i$	1,52
$l_2$	5 mm	$k_m$	140 N/m	$E$	0.95 MPa
$d_2$	25 mm	$F_{m0}$	13.934 N	$K_p$	0.28 V/N
$g_2$	13 mm	$C_{Att1}$	20 mm	$K_f$	1e5 Pa/V
$h_2$	7 mm	$m_c$	55 g	$\zeta$	1.8
$l_4$	63.9 mm	$l_0$	162 mm	$\sigma_n$	140 rad/s
$l_{5max}$	81.4 mm	$l_i$	110 mm	$C$	5.25e-9 m <sup>3</sup> Pa <sup>-1</sup> s <sup>-1</sup>
$h_0$	15 mm	$r_i$	10 mm	$b$	0.39
$h_x$	0 mm	$s_i$	0.8 mm	$K_{obj}$	8 N/rad

#### 4. Simulation and experimental validation

In order to evaluate the ability of the device to generate a haptic feedback in dynamic condition, corresponding to the interaction between the remote unit and the environment (whether a real or virtual one), some experimental tests were carried out on the prototype. The outcomes of the trials have been also used to validate the model described in the previous paragraph.

The results presented in Figure 6 refer to the case in which the operator, freely moving his finger, handles a virtual object whose crushing force is proportional to the rotation of rocker  $\alpha_1$ , i.e. to the reference feedback force  $F_{ref} = K_{obj} \Delta\alpha_1$ , with the stiffness constant  $K_{obj}$  set to 8 N/rad. Figure 6a shows the force signal acquired experimentally, compared to the one provided by the simulation, and obtained considering the same rotation pattern  $\alpha_1(t)$ . This comparison highlights the ability of the model to predict the trend of the force generated by the device in dynamic condition with good precision. The Figure 6b shows the relationship between the force generated on the fingertip  $F$  and the rotation angle  $\alpha_1$  of the rocker, in both experimental and simulated conditions.

**Fig. 6.** Comparison between experimental and simulation results ( $K_{obj} = 8$  N/rad).

The relationship between the force  $F$  and the angle of rotation  $\alpha_l$  of the rocker depends on the mechanical characteristics of the virtual object and it is influenced by the performance of the system. In fact, any oscillation in the contact force  $F$  affects negatively the ability of the device to provide the correct haptic feedback to the operator. Probably they are due to the behavior of the control logic and eased by the elasticity of both the mechanism and the actuation group. The entity of such oscillations could be relevant for some applications. To overcome this issue, a different design of the control logic and the use of a damper may be necessary.

## 5. Conclusion

This work demonstrated that the proposed haptic system, based on a four-bar mechanism, and actuated by a McKibben pneumatic artificial muscle, is able to generate the required perception force at the operator's fingertip, with good performance both in static and dynamic conditions. Therefore, it could be used as a base for the development of hand haptic exoskeletons. In addition, the proposed model proved to be able to predict with good accuracy the behavior of the system, and may be used for the design and optimization of such devices.

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