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## Simulation of the Sensing Performance of a Plasmonic Biosensor Based on Birefringent Solid-Core Microstructured Optical Fiber

A finite element method is used to analyze the performance of a microstructured optical fiber based surface plasmon resonance sensors aimed for biomedical applications, such as the detection of blood carried species. Birefringence obtained by removing of a row of holes in a two-ring hexagonal lattice of holes in a gold covered silica fiber leads to relatively high sensitivity of the fiber optical response to a refractive index of the analyte surrounding the fiber. This fiber structure supports two types (I and II) of resonant modes. In these modes there is an opposite variation of some sensing parameters with the increase of the refractive index of the analyte between 1.36 and 1.39. Thus, for a smaller value (1.36) of the refractive index of the analyte  $n_a$ , the resonance spectral width  $\delta\lambda_{0.5}$  is large for the core mode I and small for the core mode II but for a larger value (1.39) of  $n_a$ ,  $\delta\lambda_{0.5}$  is small for the core mode I and large for the core mode II. Also, for  $n_a = 1.36$  the amplitude sensitivity  $S_A$  is small for the core mode I and large for the core mode II but for  $n_a = 1.39$ ,  $S_A$  is large for the core mode I and small for the core mode II. By adjusting the radius of the gold layer, the proposed sensor shows high spectral sensitivity  $S_\lambda$  and narrow  $\delta\lambda_{0.5}$  at the same resonance wavelength and  $n_a$  (1.39) where the figure of merit ( $FOM$ ) is very large in comparison with the most recently published values.

Keywords: Sensors, surface plasmon resonance, finite element method

V. A. Popescu, N. N. Puscas

Department of Physics, University Politehnica of Bucharest,  
Bucharest 060042 Romania

e-mail (corresponding author: V A Popescu): [vapopescu@yahoo.com](mailto:vapopescu@yahoo.com)

G. Perrone

Department of Electronics and Telecommunications, Politecnico di Torino,  
C.so Duca degli Abruzzi 24, I-10129 Torino

## Introduction

Microstructured optical fiber-based plasmonic devices have attracted a large interest [1-8] for their application in chemical and biochemical sensing because of their large sensitivity combined with the possibility to easily tailor their properties by varying the geometry of the photonic crystal fiber. For instance, by changing the hole number and position the phase matching [1] or the loss matching [2-3] conditions between the fundamental  $HE_{11}$  core mode and a plasmon mode can be achieved.

In search of new approaches to enhance the sensitivity, recently, quite a number of papers have proposed new photonic crystal structures that exploit asymmetries to induce birefringence. An example is in [4], which uses a two ring hexagonal lattice photonic crystal fiber arrangement and the gold layer and the analyte are not placed inside the air-holes but outside the fiber structure, allowing a simplification in the fabrication process [2-3]. The obtained spectral sensitivity  $S_\lambda$  is 4000 nm/RIU (RIU stands for Refractive Index Units) when the refractive index of the analyte  $n_a$  is varied from 1.33 to 1.34 and 2000 nm/RIU when  $n_a$  is varied from 1.36 to 1.37; the amplitude sensitivity  $S_A$  is 320 RIU<sup>-1</sup> for  $n_a = 1.36$ . In another recent paper [5], a D-shaped hollow core microstructured optical fiber-based surface plasmon resonance sensors is proposed: in this case  $S_\lambda$  and  $S_A$  values of 2900 nm/RIU and 120 RIU<sup>-1</sup>, respectively, when  $n_a$  is varied from 1.33 to 1.34 have been reported. In another recent paper [6], an alternative plasmon D-shaped microstructured biosensor with rectangular lattice has been presented: the largest value of figure of merit ( $FOM$ ) [13] is 478.3 RIU<sup>-1</sup> and the lowest value of the resonance spectral width  $\delta\lambda_{0.5}$  is 13.6 nm for the core guided mode; then for  $n_a > 1.398$ , a record value of  $S_\lambda > 7481$  nm RIU<sup>-1</sup> has been obtained, although multiple resonance peaks and large spectral width can deteriorate the signal-to-noise ratio.

In this paper a new microstructured birefringent fiber-based plasmonic sensor is introduced and its sensing characteristics are analyzed through a finite element method. The proposed structure is made of a two-ring hexagonal lattice with five of the central horizontal air holes suppressed and, as in [4], the gold layer and the analyte are outside the fiber structure [2], so to simplify its realization and use.

## The Microstructured Plasmonic Optical Fiber Geometry

The considered microstructured optical fiber (Fig.1) is made by a SiO<sub>2</sub> core with fourteen small air holes placed at the vertices of a two-ring hexagonal lattice in which five central horizontal holes are omitted to introduce a birefringent behavior. The silica core is then further surrounded by gold and analyte layers. The structure is similar to that described in [4], except that in the proposed case the central hole and two air-holes in the same row - second ring are omitted. At the resonance wavelength, where there is a phase matching or a loss matching condition between a core mode and a plasmonic mode, this makes the  $x$ -component of the electric field in the sensing layer stronger than the corresponding  $y$ -component. In this fiber structure, there are two types of resonant modes: type I, when the main electric fields are oriented in the same  $x$  direction on the left and right sides of the gold layer; type II when orientations of these electric fields are in opposite directions. This allows maximizing the sensor performance by properly choosing the resonance mode type depending on the analyte expected refractive index value.

A finite element method is used to compute the propagation constants of the core and plasmon modes (mode index  $\nu = 1$ ) in the structure and to analyze the power absorption

efficiency for these modes. The wavelength dependence of the refractive index of silica and gold, has been modeled by using, respectively, a Sellmeier formula for SiO<sub>2</sub> [9-11] and a Drude relation [12] for Au.

## Numerical Results and Discussion

The proposed sensing structure is intended for biochemical applications, such as measurement of blood carried species for which the typical refractive index values of the analyte is in the range 1.36-1.39. Therefore, the radii and thickness parameters will be chosen to optimize the performance in this working range. For the same reason, the analysis has been carried out mainly for said refractive index values. In the first part of this section we report the results obtained from the analysis of the proposed microstructured optical fiber probe (Fig.1) in which the fourteen small air holes have all the same radius ( $r = r_1 = r_2 = \dots = r_{14} = 0.5 \mu\text{m}$ ) and are placed at the vertices of a two-ring hexagonal lattice with vertice-to-vertice distance  $d = 2 \mu\text{m}$ . As already pointed out, five central horizontal holes are then omitted to introduce the asymmetry that in turns induces the strong birefringent behavior. The SiO<sub>2</sub> substrate has radius  $r_g = r_{15} = 5 \mu\text{m}$  and is surrounded by a gold layer, with thickness  $t_g = r_{16} - r_{15} = 40 \text{ nm}$ , followed by an analyte layer. These radii and thicknesses are the values giving the optimal sensor performance as it will be shown in the second part of this section, in which some results for slightly different values will be reported.

Table 1 shows the resonant wavelength  $\lambda$ , the effective indices  $\beta/k$  for the core and plasmon modes, the difference  $\Delta(\beta/k)_r$  between the real parts of the effective indices of core and plasmon modes and the difference  $\Delta(\beta/k)_i$  between the imaginary parts of the effective indices of the same modes. The values of the effective indices are given for the maximum value of the imaginary part of the core modes. Thus, when  $n_a$  is increased from 1.36 to 1.39 in the place of the phase matching point there is a loss matching point.

Fig.2 shows the contour plot of the z-component  $S_z(x,y)$  of the Poynting vector at the phase matching point ( $\lambda_{II} = 0.6575 \mu\text{m}$ ) between the core guided and the plasmon modes II for a photonic crystal fiber when the refractive index of the analyte is  $n_a = 1.36$ . Similarly, Fig.3 reports the contour plot of the z-component  $S_z(x,y)$  of the Poynting vector at the loss matching point ( $\lambda_I = 0.78135 \mu\text{m}$ ) between the core guided and the plasmon modes I for the same fiber structure when the refractive index of the analyte is  $n_a = 1.39$ . It is interesting to note that for  $n_a = 1.39$ , the value of the z-component  $S_z(x,y)$  of the Poynting vector of the type I core guided mode at  $x=0$  is smaller than that obtained in the case of  $n_a = 1.36$  (the power fraction transferred to the analyte layer is 0.022937 for  $n_a = 1.36$  and 0.227788 for  $n_a = 1.39$ ). At the resonance wavelength, the power fraction carried in the analyte layer increases with  $n_a$  for the core modes I and II (Table 2). Fig. 4 shows the real part of the effective index versus the wavelength for the core and plasmon modes near the loss matching point ( $\lambda_I = 0.78135 \mu\text{m}$  and  $\lambda_{II} = 0.7990 \mu\text{m}$ ) when the refractive index of the analyte is  $n_a = 1.39$ . It is interesting to note that for each of the two types of modes I and II, there are anti-crossing points between plasmonic mode and core-guided mode and then the modes of each other exchange after the anticrossing point as in [6]. Fig. 5 shows the loss spectra for the core and plasmon modes near the loss matching point ( $\lambda_I = 0.78135 \mu\text{m}$  and  $\lambda_{II} = 0.7990 \mu\text{m}$ ) for a photonic crystal fiber when the refractive index of the analyte is  $n_a = 1.39$ . Fig. 6 reports the imaginary part of the effective index versus the wavelength for the type I and II core modes near the resonance wavelength for two slightly different values of the analyte refractive index ( $n_a = 1.39$  and  $n_a = 1.391$ ). As expected, the core

guided mode and the plasmon mode are strongly coupled at the loss matching point in comparison with the case of phase matching point. This fact is responsible for the larger value of the power fraction carried in the analyte layer by the core mode (0.022937 for mode I and 0.152933 for mode II when  $n_a = 1.36$  and 0.227788 for mode I and 0.273888 for mode II when  $n_a = 1.39$ ). Also, in these modes there is an opposite variation of the resonance spectral width  $\delta\lambda_{0.5}$  with the increase of the refractive index of the analyte. Thus, for a smaller value (1.36) of the refractive index of the analyte  $n_a$ , the resonance spectral width  $\delta\lambda_{0.5}$  is large (30.9 nm) for the core mode I and small (14.6 nm) for the core mode II but for a larger value (1.39) of  $n_a$ ,  $\delta\lambda_{0.5}$  is small (12.2 nm) for the core mode I and large (54 nm) for the core mode II.

The maximum values of the amplitude sensitivity  $S_A$  and the corresponding resolutions (assuming that a 1 % change in the transmitted intensity can be detected) for the guided modes I and II are given in Table 2 for different values of the analyte refractive index, namely 1.36, 1.37, 1.38 and 1.39. Fig. 7 shows the amplitude sensitivity for the guided core modes (I and II) versus the wavelength near the resonance wavelength ( $\lambda_I = 0.6552 \mu\text{m}$  and  $\lambda_{II} = 0.6575 \mu\text{m}$  when  $n_a = 1.36$  and  $\lambda_I = 0.78135 \mu\text{m}$  and  $\lambda_{II} = 0.7990 \mu\text{m}$  when  $n_a = 1.39$ ). It is interesting to note that for  $n_a = 1.36$  the amplitude sensitivity  $S_A$  is small (192.6  $\text{RIU}^{-1}$ ) for the first core mode I and large (405.7  $\text{RIU}^{-1}$ ) for the second core mode II but for  $n_a = 1.39$ ,  $S_A$  is large (886.9  $\text{RIU}^{-1}$ ) for the first mode I and small (245.8  $\text{RIU}^{-1}$ ) for the second mode II. Fig. 8 shows the resonance spectral width  $\delta\lambda_{0.5}$  and the amplitude sensitivity  $S_A$  for the core modes (I,II) with the increase of the refractive index of the analyte from  $n_a = 1.35$  to  $n_a = 1.40$ . One observe that there is a dip of  $\delta\lambda_{0.5} = 14.6 \text{ nm}$  at  $n_a = 1.36$  for the core mode II and another dip of  $\delta\lambda_{0.5} = 12.2 \text{ nm}$  at  $n_a = 1.39$  for the core mode I. Also there is a peak of  $S_A = 405.7 \text{ RIU}^{-1}$  at  $n_a = 1.36$  for the core mode II and another peak of  $S_A = 886.9 \text{ RIU}^{-1}$  at  $n_a = 1.39$  for the core mode I.

Table 2 summarizes also all the relevant parameters of type I and II core modes to fully characterize the sensor performance: phase or the loss matching points, transmission loss  $\alpha$ , propagation length  $L$ , power fraction  $P_1$  in the analyte layer; power fraction  $P_2$  in the gold layer; shift  $\delta\lambda_{res}$  towards longer wavelengths of the phase matching point or loss matching point for an increase  $\Delta n_a$  of the analyte refractive index by 0.001 RIU; resonance spectral width  $\delta\lambda_{0.5}$  (computed at the full width at half maximum of the loss spectra); signal-to-noise ratio  $SNR$ ; spectral sensitivity  $S_\lambda$ ; spectral resolution  $SR_\lambda$  (detection limit in the wavelength interrogation mode, assuming a spectral resolution of 0.1 nm); maximum value of the amplitude sensitivity  $S_A$  and the corresponding resolution; difference  $\Delta\lambda$  between maximal amplitude sensitivity and resonant wavelengths; the figure of merit  $FOM$ , which is defined as the ratio between the spectral sensitivity  $S_\lambda$  and  $\delta\lambda_{0.5}$  [13].

Besides the refractive index of the analyte layer, the resonance condition, sensor sensitivity and the loss or the phase matching condition are determined by the radii of the gold layer and of the small air holes, the thickness of the gold layer. Thus, for an increase of the radius  $r_g$  of the gold layer by 1  $\mu\text{m}$  (that is for  $r = 0.5 \mu\text{m}$ ,  $r_g = 6 \mu\text{m}$ ,  $t_g = 40 \text{ nm}$  and  $d = 2 \mu\text{m}$ ), the phase matching point for the core modes I(II) shifts by 7.5 nm (0.3 nm) towards longer wavelengths when  $n_a = 1.36$ . Correspondingly, the shift  $\delta\lambda_{res}$  is 3.1 nm (3.4 nm), whereas the spectral resolution  $SR_\lambda$  is  $3.2 \times 10^{-5} \text{ RIU}$  ( $2.9 \times 10^{-5} \text{ RIU}$ ).

For a decrease of the radius  $r_g$  of the gold layer by 0.45  $\mu\text{m}$  (that is for  $r = 0.5 \mu\text{m}$ ,  $r_g = 4.55 \mu\text{m}$ ,  $t_g = 40 \text{ nm}$ ,  $d = 2 \mu\text{m}$ ), the phase matching point for the core modes I(II) shifts by 4.2 nm (3.0 nm) towards shorter wavelengths when  $n_a = 1.36$ . Correspondingly, the shift  $\delta\lambda_{res}$  is

2.5 nm (2.7 nm), whereas the spectral resolution  $SR_\lambda$  is  $4.0 \times 10^{-5}$  RIU ( $3.8 \times 10^{-5}$  RIU). On the other hand for the same modified structure but when  $n_a = 1.39$ , the parameters of the core modes I(II) become:  $\delta\lambda_{res} = 6.3$  nm (7.4 nm),  $\delta\lambda_{0.5} = 11.8$  nm (46.4 nm),  $SNR = 0.53$  (0.16),  $FOM = 532.3$  RIU<sup>-1</sup> (159.5 RIU<sup>-1</sup>),  $S_\lambda = 6254$  nmRIU<sup>-1</sup> (7400 nmRIU<sup>-1</sup>),  $SR_\lambda = 1.6 \times 10^{-5}$  RIU ( $1.4 \times 10^{-5}$  RIU),  $S_A = 943.3$  RIU<sup>-1</sup> (235.0 RIU<sup>-1</sup>),  $SR_A = 1.1 \times 10^{-5}$  RIU ( $4.3 \times 10^{-5}$  RIU),  $\alpha = 504.2$  dB/cm (532.9 dB/cm),  $L = 86.1$   $\mu$ m (81.5  $\mu$ m),  $P_1 = 0.242701$  (0.284722),  $P_2 = 0.001977$  (0.002058),  $\lambda = 0.768936$   $\mu$ m (0.7881  $\mu$ m) and  $\Delta\lambda = 6.3$  nm (13.9 nm). In this case, the effective indices  $\beta/k$  for the core and plasmon modes I at the loss wavelength ( $\lambda_I = 0.768936$   $\mu$ m) are  $1.448113 + 0.000784i$  and  $1.447656 + 0.000784i$ , respectively. The effective indices  $\beta/k$  for the core and plasmon modes II at the loss wavelength ( $\lambda_{II} = 0.7881$   $\mu$ m) are  $1.443474 + 0.000820i$  and  $1.446467 + 0.000821i$ , respectively. Thus,  $\delta\lambda_{0.5}$  is very small,  $FOM$  is high and  $S_A$  is very high for the core mode I.

For an increase of the radius  $r$  of the small air holes by 0.1  $\mu$ m (that is for  $r = 0.6$   $\mu$ m,  $r_g = 5$   $\mu$ m,  $t_g = 40$  nm and  $d = 2$   $\mu$ m), the phase matching point for the core modes I(II) shifts by 8.79 nm (11.1 nm) towards longer wavelengths when  $n_a = 1.39$ . Correspondingly, the shift  $\delta\lambda_{res}$  is 7.5 nm (8.9 nm), whereas the spectral resolution  $SR_\lambda$  is  $1.1 \times 10^{-5}$  RIU ( $4.2 \times 10^{-5}$  RIU). In this case,  $\delta\lambda_{res}$  is very large (8.9 nm),  $\delta\lambda_{0.5} = 61.6$  nm and the line shape of the wavelength-dependent loss is asymmetric for the core mode II.

For a decrease of the thickness of the gold layer by 10 nm (that is for  $r = 0.5$   $\mu$ m,  $r_g = 5$   $\mu$ m,  $t_g = 30$  nm and  $d = 2$   $\mu$ m), the loss matching point for the core modes I(II) shifts by 58.2 nm (56.5 nm) towards shorter wavelengths when  $n_a = 1.39$ . Correspondingly, the shift  $\delta\lambda_{res}$  is 5.9 nm (7.0 nm), whereas the spectral resolution  $SR_\lambda$  is  $1.7 \times 10^{-5}$  RIU ( $1.4 \times 10^{-5}$  RIU). Also, the transmission loss for the guided modes I(II) is decreased to 280.1 dB/cm (294.3 dB/cm) and the power fraction carried in the analyte layer by the core mode is only 0.127993 for mode I and 0.150925 for mode II. In this case, the larger value of  $\delta\lambda_{0.5}$  for higher  $n_a$  is due to a supplementary interaction between core mode II (mode index  $\nu = 1$ ) and a higher order plasmon mode (mode index  $\nu = 2$ ) at the wavelength 0.6928  $\mu$ m with a large loss (312.4 dB/cm) and with a large power fraction (0.130845) in the analyte layer.

## Conclusions

The proposed photonic fiber-based plasmonic sensor with a thin gold layer and fourteen small air holes supports two types of resonant modes with a strong interaction between the core and plasmon modes near the phase or the loss matching points. The two modes can be best exploited depending on the analyte refractive index value. Type II core guided mode resonances are most suited when  $n_a \approx 1.36$ ; it exhibits higher loss (889.8 dB/cm), smaller propagation length (48.8  $\mu$ m), smaller bandwidth value (14.6 nm) of bandwidth, large amplitude sensitivity (405.6 RIU<sup>-1</sup>), very small difference between the wavelength for maximal amplitude sensitivity and the resonant wavelength (3.5 nm) and a symmetric line shape of the wavelength-dependent loss. On the other hand, for higher analyte refractive index values, say  $n_a \approx 1.39$ , type I core guided mode exhibits better results: higher spectral sensitivity (7000.0 nmRIU<sup>-1</sup>), higher  $SNR$  ratio (0.57), very large  $FOM$  (573.8 RIU<sup>-1</sup>) in comparison with the most recently published values [6], higher amplitude sensitivity (886.9 RIU<sup>-1</sup>), better value of the detection limit of the amplitude-based sensor ( $1.1 \times 10^{-5}$  RIU), smaller value (12.2 nm) of

bandwidth and the wavelength dependence of the imaginary part of the effective index is also symmetric. For  $n_a \cong 1.38$  (refractive index for the whole human blood [14]) one can improve the information from our sensor by using both types of modes (Table 2). The basis structure that contains 14 holes where five central horizontal holes are omitted can be extended to a larger radius of the gold layer with a large number of rings in the lattice of the holes.

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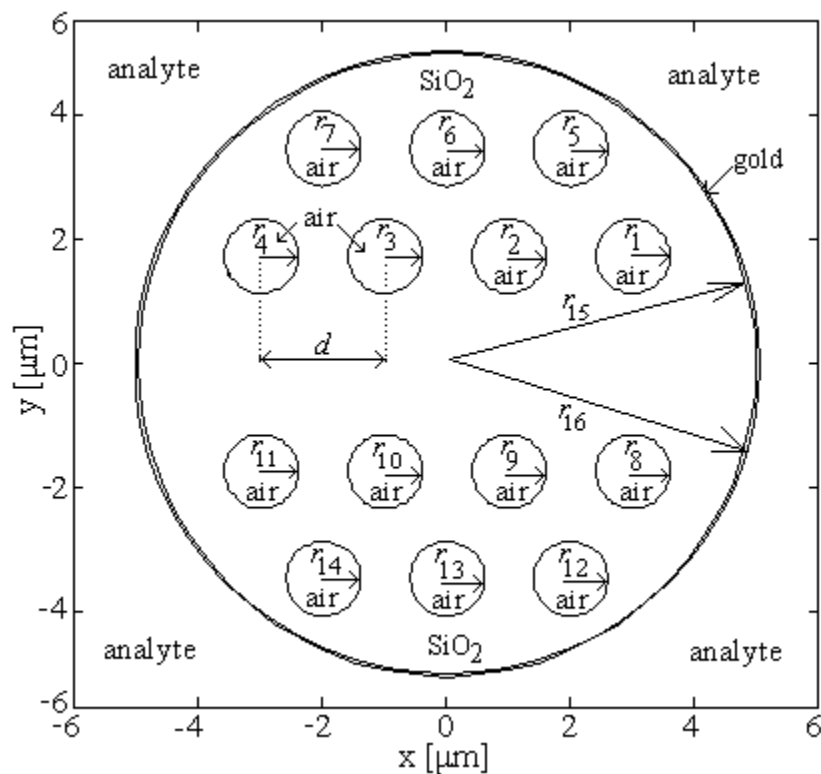


Fig.1. Cross section of a microstructured optical fiber made by fourteen small air holes (radius  $r_1 = r_2 = \dots = r_{14} = 0.5 \mu\text{m}$ ) which are placed at the vertices of a two-ring hexagonal lattice with vertex-to-vertex distance  $d = 2 \mu\text{m}$  (five central horizontal holes are omitted) that are inserted in a  $\text{SiO}_2$  substrate (radius  $r_{15} = 5 \mu\text{m}$ ) which is surrounded by a gold layer (thickness  $r_{16} - r_{15} = 40 \text{ nm}$ ) and by an analyte layer.

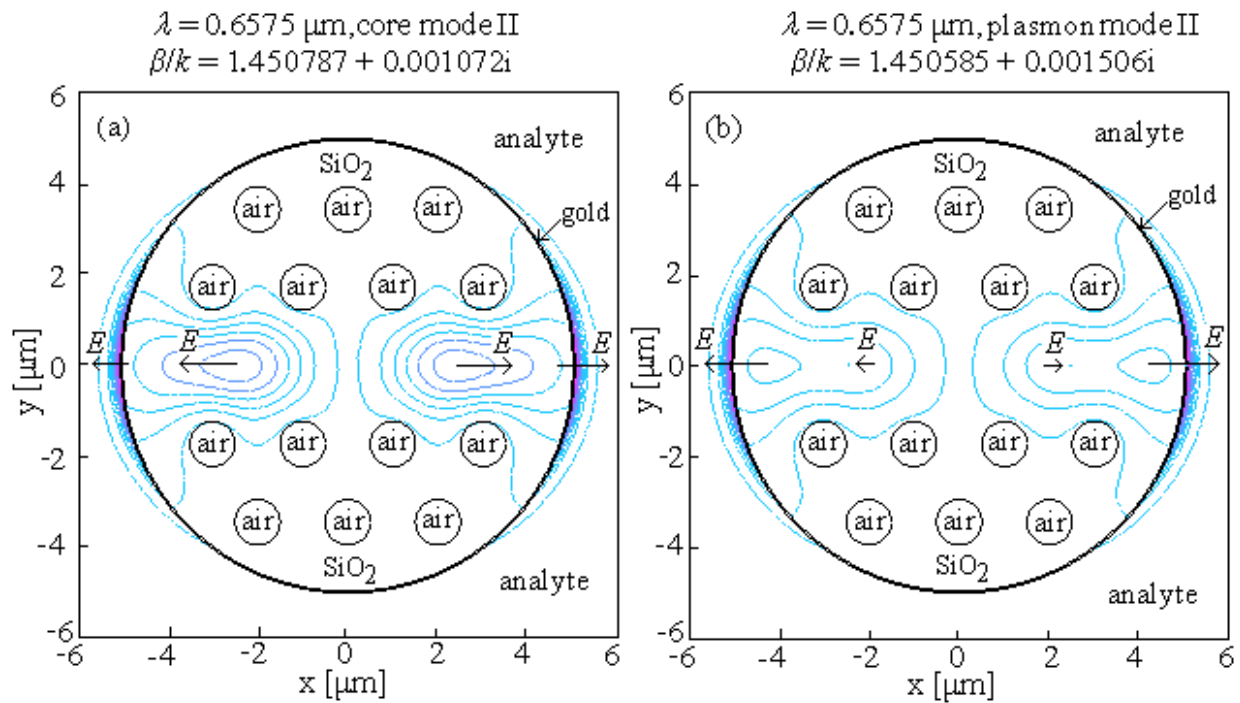


Fig.2. Contour plot of the z-component  $S_z(x, y)$  of the Poynting vector at the phase matching point ( $\lambda = 0.6575 \mu\text{m}$ ) between the core guided (a) and the plasmon (b) modes (II) for a photonic crystal fiber ( $r_1 = r_2 = \dots = r_{14} = 0.5 \mu\text{m}$ ,  $r_{15} = 5 \mu\text{m}$ ,  $r_{16} = 5.04 \mu\text{m}$  and  $d = 2 \mu\text{m}$ ) when the refractive index of the analyte is  $n_a = 1.36$ . The main electric fields are oriented in the opposite x direction on the left and right sides of the gold layer.

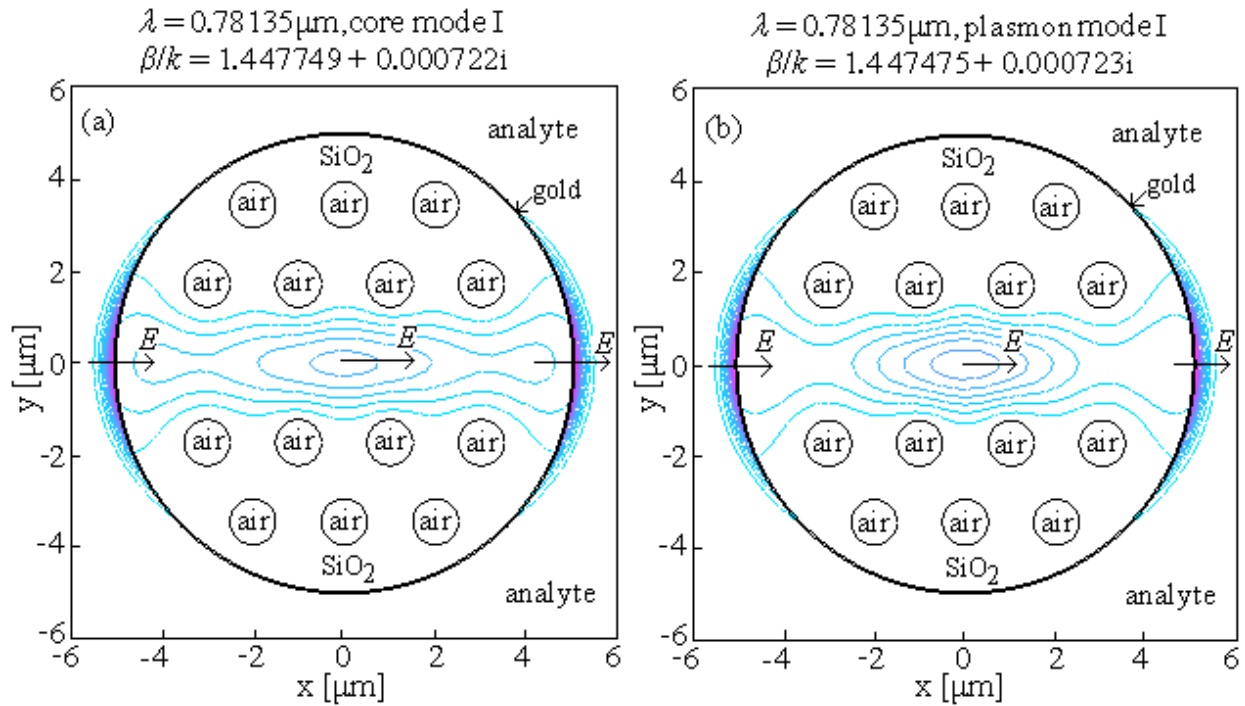


Fig.3. Contour plot of the z-component  $S_z(x, y)$  of the Poynting vector at the loss matching point ( $\lambda = 0.78135 \mu\text{m}$ ) between the core guided (a) and the plasmon (b) modes (I) for a photonic crystal fiber ( $r_1 = r_2 = \dots = r_{14} = 0.5 \mu\text{m}$ ,  $r_{15} = 5 \mu\text{m}$ ,  $r_{16} = 5.04 \mu\text{m}$  and  $d = 2 \mu\text{m}$ ) when the refractive index of the analyte is  $n_a = 1.39$ . The main electric fields are oriented in the same x direction on the left and right sides of the gold layer.

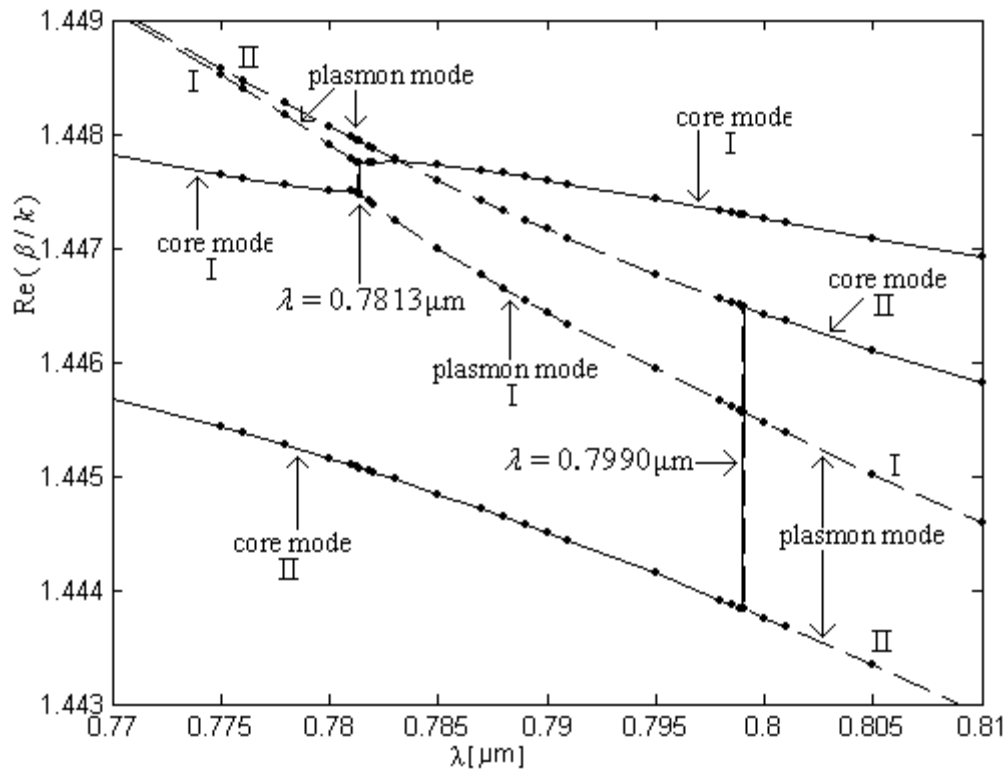


Fig. 4. The real part of the effective index versus the wavelength for the core and plasmon modes near the loss matching point ( $\lambda_I = 0.78135 \mu\text{m}$  and  $\lambda_{II} = 0.7990 \mu\text{m}$ ) for a photonic crystal fiber ( $r_1 = r_2 = \dots = r_{14} = 0.5 \mu\text{m}$ ,  $r_{15} = 5 \mu\text{m}$ ,  $r_{16} = 5.04 \mu\text{m}$  and  $d = 2 \mu\text{m}$ ) when the refractive index of the analyte is  $n_a = 1.39$ .

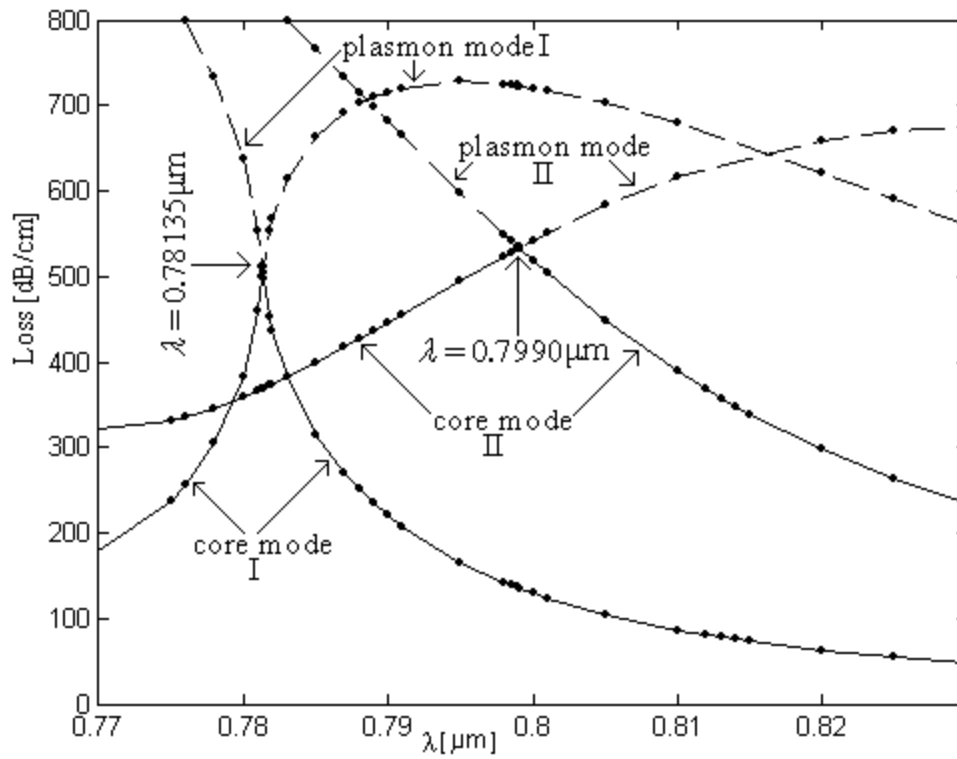


Fig. 5. The loss spectra for the core and plasmon modes near the loss matching point ( $\lambda_{\text{I}} = 0.78135 \mu\text{m}$  and  $\lambda_{\text{II}} = 0.7990 \mu\text{m}$ ) for a photonic crystal fiber ( $r_1 = r_2 = r_{14} = 0.5 \mu\text{m}$ ,  $r_{15} = 5 \mu\text{m}$ ,  $r_{16} = 5.04 \mu\text{m}$  and  $d = 2 \mu\text{m}$ ) when the refractive index of the analyte is  $n_a = 1.39$ .

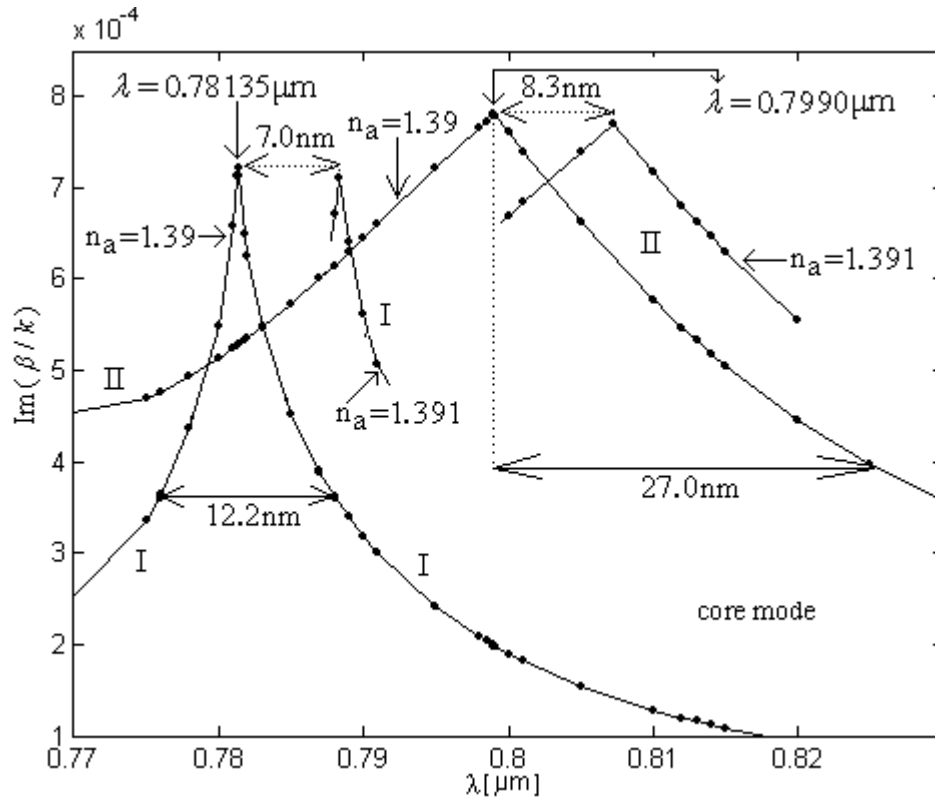


Fig. 6. The imaginary part of the effective index versus the wavelength for the core modes I and II near the resonance wavelength for a photonic crystal fiber ( $r_1 = r_2 = \dots = r_{14} = 0.5 \mu\text{m}$ ,  $r_{15} = 5 \mu\text{m}$ ,  $r_{16} = 5.04 \mu\text{m}$  and  $d = 2 \mu\text{m}$ ) by varying the refractive index of the analyte from  $n_a = 1.39$  to  $n_a = 1.391$ .

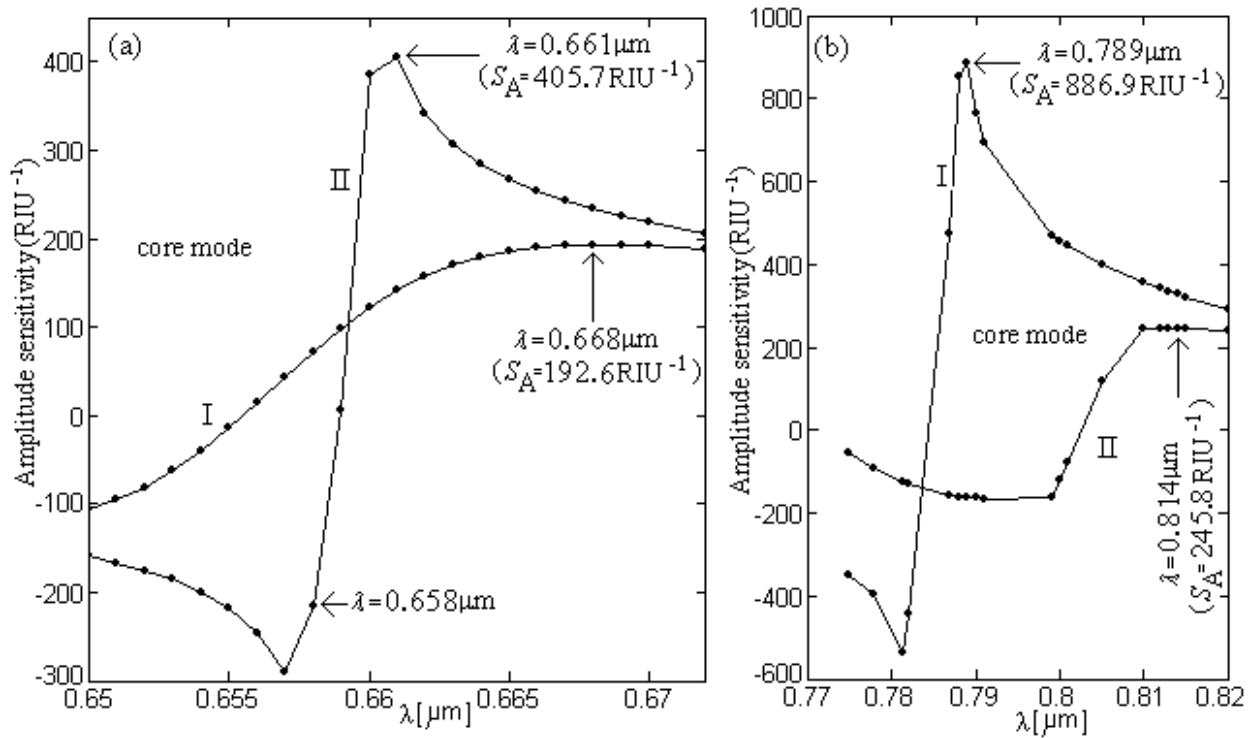


Fig. 7. The amplitude sensitivity for the guided modes (I and II) versus the wavelength near the resonance wavelength ( $\lambda_I = 0.6552 \mu\text{m}$  and  $\lambda_{II} = 0.6575 \mu\text{m}$  when  $n_a = 1.36$  (a) and  $\lambda_I = 0.78135 \mu\text{m}$  and  $\lambda_{II} = 0.7990 \mu\text{m}$  when  $n_a = 1.39$  (b)) for a photonic crystal fiber ( $r_1 = r_2 = \dots = r_{14} = 0.5 \mu\text{m}$ ,  $r_{15} = 5 \mu\text{m}$ ,  $r_{16} = 5.04 \mu\text{m}$  and  $d = 2 \mu\text{m}$ )

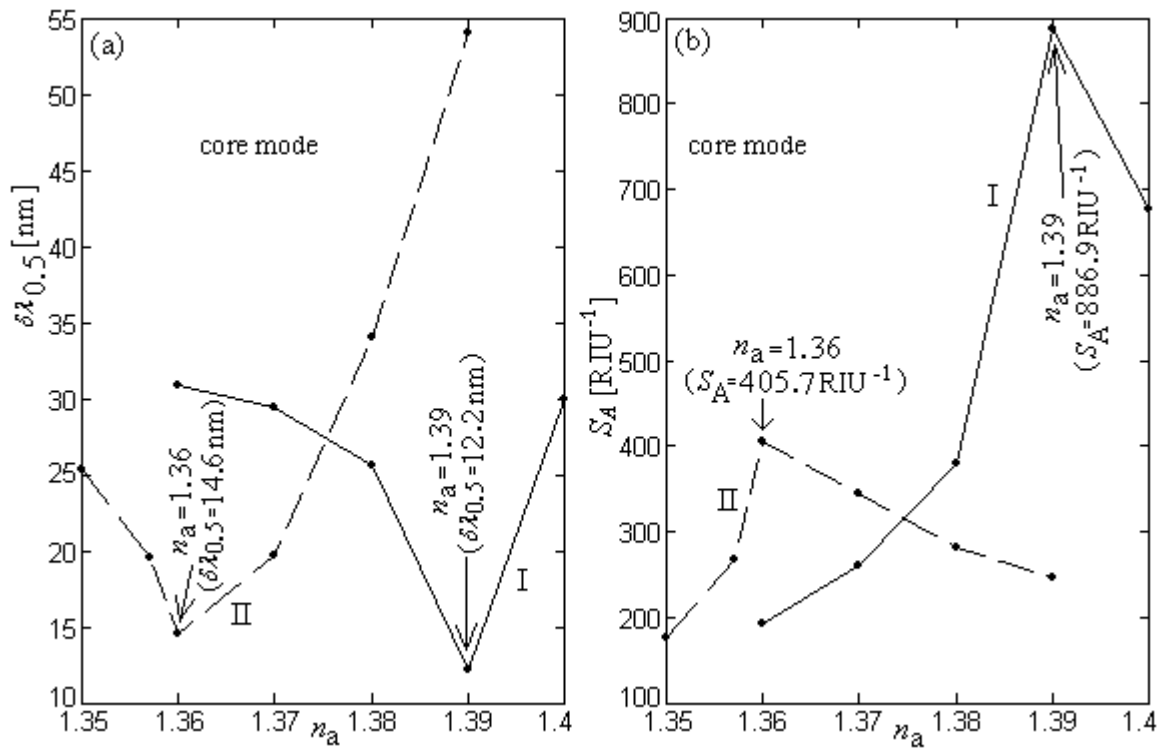


Fig. 8. The resonance spectral width  $\delta\lambda_{0.5}$  (a) and the amplitude sensitivity  $S_A$  (b) for the core modes (I,II) with the increase of the refractive index of the analyte from  $n_a = 1.35$  to  $n_a = 1.40$ .

Table 1. The resonant wavelength  $\lambda$  [ $\mu\text{m}$ ],  $\beta/k$  for the core and plasmon modes, the difference  $\Delta(\beta/k)_r$  between the real parts of the effective indices of core and plasmon modes and the difference  $\Delta(\beta/k)_i$  between the imaginary parts of the effective indices of the same modes.

Mode ( $r_g; r; n_a$ )	$\lambda$ [ $\mu\text{m}$ ]	$\beta/k$ (core) $\beta/k$ (plasmon)	$\Delta(\beta/k)_r$	$\Delta(\beta/k)_i$
I (5;0.5;1.36)	0.6552	1.452097 + 0.000165i 1.451403 + 0.002141i	0.000694	0.001976
II (5;0.5;1.36)	0.6575	1.450787 + 0.001072i 1.450585 + 0.001506i	0.000202	0.000434
I (5;0.5;1.37)	0.6855	1.450949 + 0.000229i 1.450557 + 0.001726i	0.000392	0.001497
II (5;0.5;1.37)	0.69059	1.448537 + 0.001064i 1.450130 + 0.001064i	0.001593	0.000000
I (5;0.5;1.38)	0.7255	1.449520 + 0.000339i 1.449323 + 0.001334i	0.000197	0.000995
II (5;0.5;1.38)	0.7349	1.446499 + 0.000901i 1.448674 + 0.000903i	0.002175	0.000002
I (5;0.5;1.39)	0.78135	1.447749 + 0.000722i 1.447475 + 0.000723i	0.000274	0.000001
II (5;0.5;1.39)	0.7990	1.443833 + 0.000780i 1.446487 + 0.000782i	0.002654	0.000002

Table 2. Values of  $\delta\lambda_{res}$ [nm],  $\delta\lambda_{0.5}$ [nm],  $SNR$ ,  $FOM$  [RIU<sup>-1</sup>],  $S_\lambda$ [nmRIU<sup>-1</sup>],  $SR_\lambda$ [RIU],  $S_A$  [RIU<sup>-1</sup>],  $SR_A$  [RIU],  $\alpha$  [dB/cm],  $L$  [ $\mu$ m],  $P_1$ ,  $P_2$ ,  $\lambda$  [ $\mu$ m] and  $\Delta\lambda$  [nm] with increase of the refractive index of the analyte from  $n_a = 1.36$  to  $n_a = 1.39$ .

Mode ( $r_g; r_c; n_a$ )	$\delta\lambda_{res}$ $\delta\lambda_{0.5}$	$SNR$ $FOM$	$S_\lambda$ $SR_\lambda$	$S_A$ $SR_A$	$\alpha$ $L$	$P_1$ $P_2$	$\lambda$ $\Delta\lambda$
I (5;0.5;1.36)	2.7 30.9	0.09 87.4	2700 $3.7 \times 10^{-5}$	192.6 $5.2 \times 10^{-5}$	137.7 315.3	0.022937 0.000460	0.6552 12.8
II (5;0.5;1.36)	2.7 14.6	0.18 184.9	2700 $3.7 \times 10^{-5}$	405.7 $2.5 \times 10^{-5}$	889.8 48.8	0.152933 0.003003	0.6575 3.5
I (5;0.5;1.37)	3.5 29.4	0.12 119.0	3500 $2.9 \times 10^{-5}$	259.1 $3.9 \times 10^{-5}$	182.0 238.6	0.041625 0.000635	0.6855 11.5
II (5;0.5;1.37)	3.9 19.7	0.20 196.4	3870 $2.6 \times 10^{-5}$	344.7 $2.9 \times 10^{-5}$	840.8 51.6	0.205089 <i>0.003017</i>	0.69059 4.6
I (5;0.5;1.38)	4.7 25.6	0.18 183.6	4700 $2.1 \times 10^{-5}$	379.4 $2.6 \times 10^{-5}$	255.3 170.1	0.081271 0.000898	0.7255 9.5
II (5;0.5;1.38)	5.3 34.0	0.16 155.9	5300 $1.9 \times 10^{-5}$	282.1 $3.5 \times 10^{-5}$	669.0 64.9	0.232833 0.002420	0.7349 7.1
I (5;0.5;1.39)	7.0 <i>12.2</i>	<i>0.57</i> <i>573.8</i>	7000 $1.4 \times 10^{-5}$	<i>886.9</i> <i>1.1 \times 10^{-5}</i>	504.2 86.1	0.227788 0.001685	0.78135 7.7
II (5;0.5;1.39)	8.3 54.0*	0.15 152.8	8250 $1.2 \times 10^{-5}$	245.8 $4.1 \times 10^{-5}$	532.9 81.5	<i>0.273888</i> 0.001838	0.7990 15.0

The optimized results are written with italicized characters. The symbol \* refers to an assumed symmetric line shape of the wavelength-dependent loss.