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# Mechanical characterization of glass-ceramic scaffolds at multiple characteristic lengths through nanoindentation

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# Abstract

The mechanical behaviour of implantable scaffolds is of relevant interest in all applications which require load-bearing capability. This study aims at establishing a quantitative relationship between the mechanical properties of glass-ceramic scaffolds for bone repair and the nano/micro-scale properties of their constituent materials. A nanoindentation study is carried out spanning different penetration depth on bulk (pore-free) glass-ceramc samples and on the walls of porous scaffolds. Micro-tomographical investigations allow assessing small-scale porosity of the scaffold walls. A simple homogenization model is used to establish the relationship between the elastic modulus of the bulk material and that of the micro-porous walls of the scaffolds. The elastic modulus of scaffold walls was found to be approximately 50% lower than that of the bulk glass-ceramic. The properties estimated experimentally on the walls of the scaffolds are quantitatively consistent with the analytical predictions provided by the homogenization model and the micro-porosity measured through tomographical analyses.

Keywords: Glass-ceramic, scaffold, Nanoindentation, micro-CT.

# 1. Introduction

The increase in average life expectancy is a great achievement of scientific findings; meanwhile, with aging population over the last decades, now bone re-

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pair is one of the major clinical needs which requires significant research efforts

- [1, 2]. Several studies have suggested the use of bioceramics, which include biocompatible glasses, glass-ceramics and (crystalline) ceramics, for bone defect healing and bone fracture treatment [3] in different regions of the body, i.e. in vertebrae, maxillofacial reconstruction [4], hearing restorations (ear prosthesis) [5], orthopedics, dental implants [6], [7], [8] etc. Bioactive ceramics and
- <sup>10</sup> **bioactive glasses** are able to create a stable interface with host tissue, and some of them can even stimulate new tissue growth, which is crucial to pursue clinical success in their applications [9]. In the early 1970s, Hench and coworkers showed bioactivity of 45S5 bioglass [10]; from then various formulation of bioglasses have attracted the interest of the researchers in different tissue
- repair applications [11], [12], [13], [14], and in the specific field of bone repair [15], [14], [16], [17], [18]. In this regard, the most important role played by the scaffolds in bone tissue repair is the recovery of natural bone functions [19], [20]. Specifically, major attention was devoted to optimizing the design, composition and mechanical behaviour of porous bioactive glass-based scaffolds for hard tissue recovery.
- Often a three-dimensional (3-D) porous scaffold structure is fabricated by using bioactive glasses in order to direct and support bone tissue growth and regeneration [21], [22]. Bioactive glasses are reported to stimulate more bone regeneration compared to other bioactive ceramics but they lag behind other bioactive
- <sup>25</sup> ceramics in terms of clinical success [15]. Hence, the number of research activities on bioactive glasses is growing due to their unreached potential in the market. In this work we deal with 3-D bioceramic sintered scaffolds fabricated from the  $SiO_2$ -based glass formulation CEL2 which was demonstrated to be highly bioactive in vitro [23] and biocompatible with osteoblasts that expressed
- the typical markers of osteogenesis [24], [25]. The method selected for scaffold fabrication, i.e. sponge replication, is able to produce highly-interconnected 3-D network of open macropores [26] and trabecular structures characterized by micro and nanopores. These peculiar features at different length scales substantially affect the mechanical properties of the scaffold. **It is therefore of great**
- <sup>35</sup> relevance to establish a characterization method that is able to determine the real mechanical properties of the glass-ceramic scaffold. This method must explicitly account the features of the material which are peculiar for the specific manufacturing approach: namely, micro-porosity of the scaffold walls originated by the sintering pro-
- <sup>40</sup> **cess.** The specific aim of this study is to establish a quantitative relationship between the mechanical properties of the glass-ceramic scaffold and the nano and micro-scale properties of the constituent material with specific reference to the material stiffness. This aim is achieved through an experimental and analytical approach to the mechanical characterization of the scaffolds carried
- <sup>45</sup> out at multiple characteristic lengths. A nanoindentation study carried out at multiple penetration depths (indentation loads) is integrated with analytical homogenization models and voxel-specific micro-CT data on 3-D porous scaffolds. Very few papers are available on the application of nanoindentation tests on ceramic scaffolds, among them Vivanco et al. [27] used

- <sup>50</sup> nanoindentation to characterize the mechanical properties of the scaffold walls with specific reference to the effect of the compliance of the micro-struts. More papers are available on micro-CT scan data used to assess the micro-porosity of the ceramic microstructures. Scheiner et al. [28] used micro-CT data to assess the microporosity of the
- <sup>55</sup> same glass-ceramic material investigated in this study. To the Authors' knowledge, the approach presented in this paper which puts together the micro-CT data and the nanoindentation data gathered at multiple characteristic lengths is novel. The mechanical characterization of the constituent glass-ceramic in a bulk form was the starting point of
- this study. Unlike its bulk form, sintered glass-ceramic scaffolds exhibit small scale porosity which may heavily affect the mechanical properties of the scaffold wall. Thereby, the nanoindentation study carried out on the microstructure of the sintered scaffold will determine in a quantitative fashion the effect of the sintering process on the mechanical properties of the scaffold structural fea-
- <sup>65</sup> tures. Well-established analytical homogenization models are used to correlate the mechanical properties of the sintered structures with their nano- and microporosity. The porous structure as estimated through the analytical approach will be validated by making use of the attenuation data of micro-CT scans carried out on the glass-ceramic scaffolds.

#### 70 2. Materials and Methods

#### 2.1. Preparation of CEL2 bulk samples and scaffolds

An experimental  $SiO_2$ -based glass formulation (CEL2; molar composition: 45%  $SiO_2$ , 3%  $P_2O_5$ , 26% CaO, 15%  $Na_2O$ , 7% MgO and 4%  $K_2O$ ) was selected to produce the samples investigated in the present work. The glass

- <sup>75</sup> was prepared by melting the required quantities of high-purity reagents (powders of  $SiO_2$ ,  $Ca_3(PO_4)_2$ ,  $CaCO_3$ ,  $Na_2CO_3$ ,  $(MgCO_3)_4Mg(OH)_2$  5H<sub>2</sub>O and  $K_2CO_3$  purchased from Sigma-Aldrich and used as received) in a platinum crucible in air (1500°C for 0.5 h to ensure homogeneity of the melt; heating rate 10°C/min). The melt was poured in stainless steel moulds (about
- <sup>80</sup> 50  $mm \times 10 \ mm \times 10 \ mm$ ) and an annealing treatment (500°C for 12 h) was applied for glass thermal stress relaxation. The obtained glass bars were cut into 2-mm thick slices by using a diamond wheel (Accutom 5, Struers); these slices will hereafter be referred to as bulk samples. The porous samples were obtained by means of the procedure described below. The melt
- was quenched into cold water to obtain a frit that was ground by ball milling (a six-ball zirconia milling machine was used), and the glass powders were eventually sieved through stainless steel sieves (Giuliani Technologies, Italy) to obtain a powder with a particle size below 32  $\mu m$ . The 3-D scaffolds were produced by the sponge replication method, which was shown to be very effective to obtain
- <sup>90</sup> porous ceramics with a highly-interconnected 3-D network of open macropores [26]. Small cubic blocks (10 mm × 10 mm × 10 mm) of a commercial open-cell polyurethane (PU) sponge (45 ppi; density of the porous PU  $\approx 20 kg/m^3$ ) were

coated with CEL2 powder by impregnation into a water-based glass slurry (glass : distilled water : poly(vinyl alcohol) (PVA) = 30 : 64 : 6 wt.%). After PVA hydrolysis under continuous magnetic stirring at  $80^{\circ}C$ , CEL2 powder was added to the solution; the water evaporated during PVA dissolution was re-added to the slurry to restore the correct weight ratios among the slurry components. After further stirring for 15 min at room temperature to ensure slurry homo-

- geneity, the sponge blocks were immersed in the slurry. The slurry infiltrated the porous network of the PU template, that after 1 min was extracted from the batch and subsequently compressed ( $\approx 50 \ kPa$  for 1 s) up to 60% in thickness along three orthogonal spatial directions, in order to homogeneously remove the excess slurry; this infiltration/compression cycle was repeated for three times and a final cycle of impregnation alone was performed. The glass-coated sponges
- were dried at room temperature overnight and afterwards thermally treated at 950°C for 3 h (heating and cooling rates set at 5 and  $10^{\circ}Cmin^{-1}$ , respectively) in order to burn-off the polymeric template and to sinter the inorganic particles. A glass-derived replica of the starting PU template was finally obtained. As reported elsewhere [26], two crystalline silicate phases develop during the above-mentioned heat treatment; however, for the sake of simplicity, the expressions CEL2 scaffold or CEL2 sample will be hereafter adopted, without further specifying the glass-ceramic nature of the sintered materials.
- Consistently, the bulk samples were heat-treated according to the same conditions used to produce the scaffolds in order to obtain a material with the same <sup>115</sup> crystalline phases.

#### 2.2. Embedding and polishing

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Bulk and CEL2 samples were embedded in epoxy resin (Epofix, Struers) in order to facilitate the polishing procedure. Subsequently, a metallographic polishing wheel (Buehler) was used to perform 7 consecutive steps of polishing: 4 steps were performed using SiC sandpapers (grit sizes 600, 1200, 2500 and 4000) 120 and 3 steps using adhesive papers (Alulap and Polilap) with alumina  $(Al_2O_3)$ suspensions (particle sizes  $1 \ \mu m, 0.05 \ \mu m$  and  $20 \ nm$ ). Each step was performed at 100 rpm speed for 4 minutes in clockwise direction and 4 minutes in counterclockwise direction. After polishing, samples were immersed in ultrasonication bath (SONIC A) with deionized water for 7 times, 5 minutes each, in order to 125 remove polishing debris. A contact profilometry procedure was used to assess the average roughness over a  $20\mu m \times 20\mu m$  square area of the polished surface. This was performed by using the Nanotest Platform described below and a thiny contact load (0.05 mN); an average roghness of approximately 100 nm was achieved. The heterogeneous nature 130 of the sample surface did not allow us to obtain smoother surfaces. Due to this specific nature of the sample surface, indentation sites were selected manually on the basis of the microscopic imaging of the surface.

#### 2.3. Nanoindentation tests

<sup>135</sup> Three bulk samples and four porous samples underwent nanoindentation tests. Nanoindentation tests were performed on Nanotest Platform 3 (MicroMaterials) at controlled temperature of  $28^{\circ}C$  using a Berkovich diamond indenter. Load-controlled indentation tests were performed at 1, 50, 100 and 200 mN maximum load. For each load between 45 and 73 indentations were performed on the bulk samples, while between 11 and 33 tests were performed on

- the scaffolds. Loading and unloading rates were selected based on the maximum load, as shown in table 1. The peak load was held constant for a defined holding time depending on the maximum load (table 1). At the end of the test the load was held constant for 30 s at 10% of the maximum load; the measured displacement drift was used for the thermal drift compensation during post-processing. Diamond Area Functions (DAFs) and compliance values were calibrated on standard samples (fused silica) with standard procedures. Three different polynomial DAFs were used based on maximum penetration of the tip in the sample: a first DAF was calibrated for penetrations smaller than 200
- nm, a second DAF for penetrations between 200 nm and 1400 nm, the ideal DAF was used for higher penetration depths. Analysis of the experimental curves was performed using the MicroMaterials software, which implements the Oliver-Pharr theory. Unloading curves were interpolated between 95% and 50% of maximum load for slope calculation. Nanoindentation modulus and hardness
  were obtained from each indentation curve. The nanoindentation modulus E\*

is defined by:

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$$\frac{1}{E^*} = \frac{1 - \nu_i^2}{E_i} + \frac{1 - \nu_s^2}{E_s} \tag{1}$$

Mechanical properties of the indenter (i) are known ( $E_i = 1141 \ GPa, \nu_i = 0.07$ ), therefore Young's modulus of the sample (s) can be calculated for a given Poisson's ratio ( $\nu_s$ ). The mechanical properties of the samples are identified by the reduced modulus M defined by:

$$\frac{1}{M} = \frac{1 - \nu_s^2}{E_s} \tag{2}$$

# 2.4. Morphological investigation

The morphology of scaffold at the macro- and micro-scale was investigated through Scanning Electron Microscopy at two different magnification levels: 100X and 2500X. The 100X images allowed us to identify the typical macro-pore size, while the 25000X images allowed us to assess the micro- or nano-porosity

of the walls of the scaffold. The inner porous network of CEL2 scaffolds was also non-destructively investigated by micro-computed tomography (Micro-CT; SkyScan 1174, Micro Photonics Inc.) to quantitatively assess the pore and strut features. Scanning pa-

- <sup>170</sup> rameters were selected as follows: source voltage 50 kV, current 800  $\mu A$ , voxel size 13.73  $\mu m \times 13.73 \ \mu m \times 13.73 \ \mu m$ , exposure time per projection 8500 ms, rotation step 0.3°. The attenuation factors were converted in grey scale values and analysed to assess macro-porosity and nano-/micro-porosity of the material by means of a MATLAB code as described below.
- <sup>175</sup> Cubic Volume Of Interests (VOI) were identified in the whole analysed sample having different size and position within the sample. The edge size of the VOIs

ranged between 50  $\mu m$  to 500  $\mu m$ . A built-in thresholding algorithm based on the Otsu's method was used to determine a global threshold with the purpose to identify pixels representing voids and pixels representing solid material (the latter being porous, i.e. micro/nano-pores had size smaller than the pixel size). Macro-porosity  $\Phi^M$  is than obtained as follows:

$$\Phi^M = 1 - \frac{N_{solid}}{N_{tot}} \tag{3}$$

in which  $N_{solid}$  is the number of solid pixels and  $N_{tot}$  is the total number of pixels in the VOI.

The micro-porosity  $\phi^{\mu}$  is obtained by analysing the histograms of grey level distributions af all VOIs and by means of the following relationship:

$$\phi^{\mu} = \frac{X - X_s}{X_{air} - X_s} \tag{4}$$

in which  $X_s = 255$  is the grey level for the solid pixels at the peak of the histogram, while  $X_{air}$  is the grey level which corresponds to the peak of void pixels as obtained by identifying the peak in the hitograms of each VOI.

A material is considered macro-homogeneous in continuum micromechanics

# 2.5. Analytical model for porosity-mechanical properties relationship

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- if a micro-heterogeneous portion of it can form a representative volume element (RVE) [29]. The characteristic length 1 of a RVE should be such that l >> d, where d is the characteristic length of the inhomogeneity within the RVE, and l << L, where L is the characteristic length of geometry/loading of the structure made by the material of the RVE. The microstructure within one RVE is not described in complete detail. In order to estimate the mechanical properties of the scaffold walls, the so-called Mori-Tanaka scheme [30] was applied, which has been previously used for similar scaffolds [28]. The Mori-Tanaka scheme was developed for composite materials with spherical inclusions and utilizes the bulk phases properties to estimate the homogenized modulus of the composite. For this application, a quasi-homogeneous portion of microporous material was selected within the scaffold walls as the RVE in order to apply the scheme. It was modelled as a composite where the solid phase is the
  - bulk glass-ceramic material and inclusion material is air  $(K_{air} = 0, G_{air} = 0)$ . Young's modulus for the dense material was obtained by nanoindentation on the bulk glass-ceramic samples, while Poisson's ratio was assumed 0.2766 [28]. By applying the Mori-Tanaka scheme, the homogenized bulk modulus  $K_{sk}^{(hom)}$ and shear modulus  $G_{sk}^{(hom)}$  can be estimated as a function of the scaffold wall micro-porosity  $\phi^{\mu}$  as:

$$K_{sk}^{(hom)} = \frac{(1-\phi) K_{dg}}{(1-\phi) + \frac{\phi}{1-\alpha_{dg}}}; \quad G_{sk}^{(hom)} = \frac{(1-\phi) G_{dg}}{(1-\phi) + \frac{\phi}{1-\beta_{dg}}}$$
(5)

where  $K_{dg}$  and  $G_{dg}$  are the bulk and shear moduli of the solid phase, while  $\alpha_{dg}$  and  $\beta_{dg}$  are the volumetric and deviatoric part of the Eshelby tensor [31], respectively:

$$\alpha_{dg} = \frac{3K_{dg}}{3K_{dg} + 4G_{dg}}; \quad \beta_{dg} = \frac{6(K_{dg} + 2G_{dg})}{5(3K_{dg} + 4G_{dg})} \tag{6}$$

The homogenized Young's modulus is obtained by applying the classical relations of isotropic linear elasticity:

$$E_{sk}^{\text{hom}} = \frac{9K_{sk}^{hom}G_{sk}^{hom}}{3K_{sk}^{hom} + G_{sk}^{hom}} \tag{7}$$

<sup>215</sup> The reduced modulus of the microporous material is therefore:

$$M_{sk}^{hom} = \frac{E_{sk}^{hom}}{1 - \nu_{sk}^{hom2}}; \quad \nu_{sk}^{hom} = \frac{3K_{sk}^{hom} - 2G_{sk}^{hom}}{6K_{sk}^{hom} + 2G_{sk}^{hom}}$$
(8)

In equations (5,6,7,8) the following relationships are used  $K_{dg} = \frac{E_{dg}}{3(1-2\nu_{dg})}, G_{dg} = \frac{E_{dg}}{2(1+\nu_{dg})}$ .

### 3. Results

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#### 3.1. Nanoindentation tests

Results from nanoindentation experiments on the bulk material are reported first. The nanoindentation moduli  $(E^*)$  and hardness are shown in figure 1. In all box plots the symbols represent the average measure at each load level, while the top and bottom bounds of the boxes represent the 95 percentile and 5 percentile of all experimental measures. Top and bottom whiskers represent the extreme measured values. Outliers are reported with cross symbols.

The penetration depths ranged between 82 nm and 1300 nm, approximately; this indicates that the nanoindentation experiments spanned the characteristic lengths which covered one order of magnitude. No statistically significant difference was found between **measures at different loads for both indentation moduli and hardness**; this indicates that mechanical properties of the bulk

sample did not show dependence on the characteristic length of the experiments. The average nanoindentation modulus was 105.98 GPa, which corresponds to a reduced modulus of 116.77 GPa and to an elastic modulus of 108.27 GPa, assuming a Poisson's ratio of 0.2766 [28]. This result was found to be consistent with the one obtained using the impulse excitation technique (99.8 GPa).

Nanoindentation moduli and hardness obtained on the scaffold walls are reported in figure 2.

The penetration depth ranged between 43 nm and 1700 nm, approximately. A decreasing trend of the nanoindentation modulus with peak load was observed. Significant differences were found between the distributions of nanoindentation

modulus obtained at different peak loads (Wilcoxon test, p < 0.05). No significant differences were found for hardness.

This size-dependence can be interpreted by inspection of the SEM images of the scaffold surface at high magnification (figure 3).

As reported before, the image acquired at low magnification (figure 4) showed that the pore size of the macropores is larger than  $100 \ \mu m$ . Whereas, the image acquired at higher magnification showed that the scaffold walls are characterized by micro- and nano-porosity the typical size of which is smaller than  $1 \ \mu m$ . In figure 3 the size of the

- areas involved in indentations at different peak loads was schematically represented. It can be noticed that micro-porosity is not involved when applying 1 mN peak load, while indentations at higher loads involve a larger area affected by micro-porosity. The dependency of nanoindentation modulus on the applied load is then attributed to the porosity of the walls. In fact, the nanoindentation
- <sup>255</sup> modulus obtained at 1 mN peak load  $(109.43 \pm 17.86 \ GPa)$  is comparable with those obtained on the bulk material, which does not exhibit porosity; while at 200 mN nanoindentation modulus decreased  $(58.32 \pm 12.21 \ GPa)$  because the area involved in the test is porous.
- 260 3.2. Porosity and microstructure

As reported elsewhere [26], the development of two crystalline phases  $(Na_4Ca_4(Si_6O_{18})$ and  $Ca_2Mg(Si_2O_7))$  occurs upon sintering of CEL2 scaffolds, that are actually constituted by a glass-ceramic material.

The porosity of the starting PU template, assessed by micro-CT measurements,

- was 90 vol.%; the mean strut thickness and the mean pore size were about 85  $\mu m$  and 580  $\mu m$ , respectively. During the sponge replication process, the PU foam was coated with a thin and continuous layer of CEL2 particles in order to obtain, after the heat treatment, a glass-ceramic replica of the template. The total porosity of the scaffolds was estimated to range betwen 55 and 60 vol.%
- <sup>270</sup> by micro-CT analysis, that also revealed an excellent 3-D interconnectivity of the macropores (the open porosity was estimated to be above 95% of the overall porosity). The mean strut thickness and mean pore size were about 100  $\mu m$ and 450  $\mu m$ , respectively. Macro-porosity was also observed by SEM (figure 4). In more details, figure 5 shows the values of macro-porosity as obtained from
- eq. (3) for all considered sizes of the VOI. It is worth noting that for small VOIs a high dispersion of macro-porosity values was found at each VOI size. This means that macro-porosity is strongly dependent on the location of the VOI within the whole sample. Conversely, larger VOIs (larger than 400  $\mu$ m) showed less dispersed values of macro-porosity. This is an expected result as large por-
- tions of the VOIs overlap for size larger than 400  $\mu m$ . Figure 6 shows the value of micro-porosity as obtained from eq. (4) for all considered sizes of VOI. Also micro-porosity values exhibited high dispersion for small size VOIs; on the contrary, less dispersed values were obtained for VOI larger than 350  $\mu m$ . As discussed above, this is also an expected result. An average micro-porosity value of 200% is found for the larger VOIs. Therefore electric methods and reduced
- <sup>285</sup> of 28% is found for the largest VOIs. Therefore elastic modulus and reduced

modulus of the glass-ceramic walls was obtained as a function of micro-porosity by applying equations 5,6,7. The normalized reduced modulus  $M/M_{dg}$  with  $M_{dg} = 116.77 \ GPa$  is shown in figure 7. Both the reduced modulus obtained through the shallow indentations and that obtained through

- the deep indentations at 200 mN maximum load were used in the Mori Tanaka scheme to estimate the micro-porosity of the walls. Reduced moduli obtained at 200 mN ranged from about 48.0 GPa to 75.0 GPa (average 61.4 GPa), which correspond to normalized reduced moduli ranging between 0.41 and 0.64 (average 0.54); therefore porosity was estimated to range from 0.21 to 0.38 (average 0.27). This micro-porosity range is consistent with that found through gray values of micro-CT scans; in particular, the average estimated estimates of the set of the
  - timated micro-porosity (0.29) is consistent with the micro-porosity estimated through CT-scans and the Mori Tanaka homogenization approach.

#### 4. Discussion

- The aim of this paper was to assess the mechanical properties of glass-300 ceramic scaffolds allowing for micro- or nano-porosity at the microarchitecural level. The porous material was obtained by means of a sponge replica process. The characterization study was carried out by means of the nanoindentation tests performed at multiple characteristic lengths and analyses of micro-CT scans. Shallow penetration indentations on the walls of the porous structures 305 showed elastic properties which were consistent with those found on the bulk glass-ceramic sample (i.e. without macro- and micro-porosity). Deep penetration indentations on the walls of the porous scaffold showed nanoindentation moduli which were lower than those found both at shallow penetrations on the scaffold and on bulk material. The shallow penetration depth was in the order 310 of 50 nm which resulted in a contact diameter lower than the typical microporosity; on the contrary, the deep penetration depth was in the order of 1500 nm which is much larger than the typical nano- and micro-pores in the scaffold wall. This size comparison indicates that the mechanical properties determined
- at deep penetrations are affected by the porosity of the wall structure of the scaffold. This hypothesis has been confirmed by the estimation of the micronano-porosity of the walls obtained through the analyses of the micro-CT data. Indeed, a simple homogenization scheme for a micro- or nano-porous structure, the Mori Tanaka method, allowed us to estimate the porosity of the scaffold
- walls by comparing the reduced moduli found at shallow and deep indentations. The porosity of the walls assessed by micromechanical modelling (Eq.(5,6,7)) was consistent with that found through the micro-CT data analysis. Although it might be argued that the decrease of the indentation moduli with the penetration depth might be owed to damage or nano-fracture phenomena occurring
- <sup>325</sup> locally under the indenter, the consistency between the micro-CT analysis and the nano-indentation results would actually exclude fracture phenomena. The surface roughness is, in general, a limiting factor for the reliability of indentation measures. In this study, average roughness was in the order of 100 nm (quadratic roughness estimate). This value was estimated over surface area

- <sup>330</sup> much larger  $(20 \ \mu m \times 20 \ \mu m)$  than the typical micro-pore size (about  $1 \ \mu m$ ), which greatly affected the roughness measure. Indentation tests with loads higher than 50 mN involved penetration depth higher than 500 nm; therefore surface roughness was assumed to be suitable for indentations at these load levels. Shallow indentations involved smaller contact area, therefore they were less affected by the micro-pores.
- Pore size and trabecular thickness are comparable to those reported by other authors for human healthy cancellous bone (radius and tibia) [32]. This opens the route to new potential applications of these scaffolds as discussed in detail by Baino et al. [33]. The mechanical
- <sup>340</sup> properties of the scaffold walls are higher than that exhibited by the bone tissue at the trabecular level [34]; therefore further research is needed. This study have shown that the micro-porosity of the scaffold walls can be a morphological parameter which may be tuned with the purpose to match the target mechanical properties.
- <sup>345</sup> The assessment of the macroscopic stiffness and macroscopic strength of the glass-ceramic porous scaffolds is also a relevant issue for a comprehensive mechanical characterization of such materials. This will be achieved in a future study by means of CT-based finite element modelling in the linear and in the non-linear range, along with the suitably designed macroscopic laboratory tests.

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## 5. Conclusions

Bone-like glass-ceramic scaffolds with multiscale porosity have been produced by the sponge replication method. Mechanical properties of the scaffolds at the scale of the single strut have been assessed in this work by means of a <sup>355</sup> nanoindentation study. The experiments have proven that the elastic modulus of the scaffold walls is lower than that of the bulk material. Micro-porosity resulting from SEM and micro-CT investigation on the porous scaffolds explains the elastic mismatch with the bulk material which does not exhibit micro- or nano-porosity. The approach reported in this work allows quantifying the effect of the fabrication route (foam replica followed by sintering) on the mechanical properties of scaffold struts.

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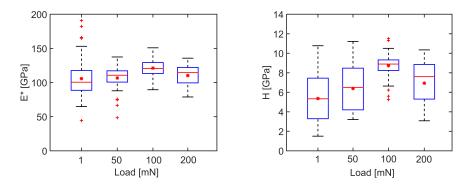


Figure 1: Nanoindentation modulus (left) and hardness (right) obtained from nanoindentation tests on the bulk material  $% \left( {{\left[ {{{\rm{T}}_{\rm{T}}} \right]}_{\rm{T}}} \right)$ 

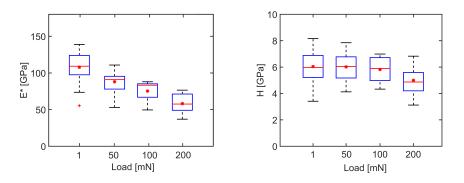


Figure 2: Nanoindentation modulus (left) and hardness (right) obtained from nanoindentation tests on the scaffold

Load [mN]	Loading rate $(mN/s)$	holding time [s]	unloading rate $(mN/s)$
1	0.5	30	0.5
50	2.5	3	5
100	2.5	3	5
200	2.5	30	5

Table 1: Parameters for nanoindentation tests

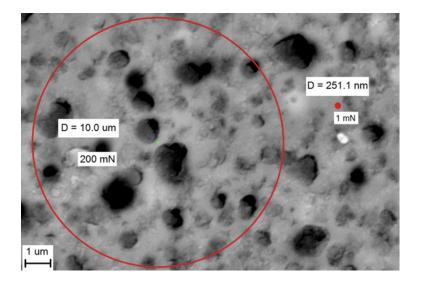


Figure 3: SEM image of the scaffold surface (magnification 25000x)

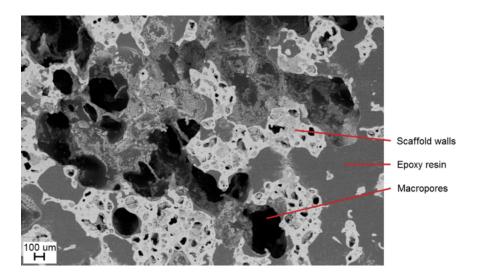


Figure 4: SEM image of the scaffold surface (magnification  $100 \mathrm{x})$ 

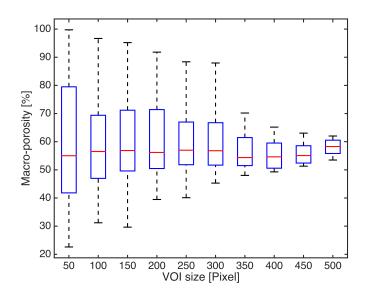


Figure 5: Macro-porosity estimated through the micro-CT data

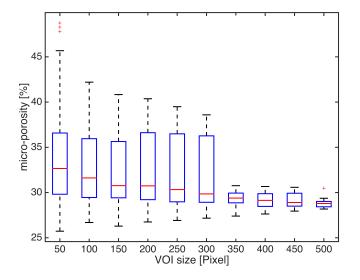


Figure 6: Micro-porosity estimated through the micro-CT data

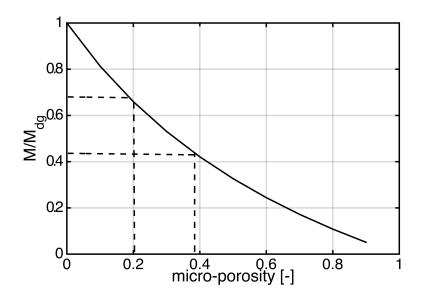


Figure 7: Mori-Tanaka estimate of the normalized reduced modulus vs micro-porosity