

ELECTROSPUN MEMBRANES WITH ENHANCED BIOACTIVITY FOR PERIODONTAL TISSUE ENGINEERING APPLICATIONS

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Introduction

Periodontal disease affects the tooth supporting structures, namely alveolar bone, cementum and periodontal ligament. Current regenerative treatments show limited and unpredictable results, and fail to effectively promote a complete regeneration of the periodontal tissues damaged or lost due to the disease [1]. Therefore, new alternative strategies are needed to improve clinical outcomes. Decellularized cell-derived extracellular matrix (dECM) offers the opportunity to enhance the bioactivity of the scaffolds, and has been explored for tissue engineering (TE) applications since it can mimic the *in vivo* microenvironment [2].

In this work, electrospun polycaprolactone/chitosan (PCL/CTS) nanofibrous membranes loaded with dECM were developed using lyophilized dECM powders derived from human Periodontal Ligament Stem Cells (PDLSCs) incorporated in the electrospinning polymeric solutions.

Methods

Following a previously established protocol, PDLSCs were cultured for 10 days and decellularized to obtain dECM, which was then lyophilized [3]. PCL, PCL-CTS and PCL-CTS-ECM membranes were fabricated by electrospinning using the following parameters, needle gauge: 21G; flow rate: 0.5 mL/h; voltage: 24 kV; needle to collector distance: 22 cm; temperature: 23-24 °C; relative humidity: 30-40%. The morphology of the electrospun fibers was characterized by scanning electron microscopy (SEM). The mechanical properties of the membranes were assessed through uniaxial tensile testing using a mechanical tester (UniVert Model UV-200-01, CellScale). PDLSCs were seeded on PCL, PCL-CTS and PCL-CTS-ECM membranes and cultured in osteogenic medium for 21 days. Alkaline phosphatase (ALP) and collagen I (COL I) gene expression was determined by quantitative real-time Polymerase Chain Reaction (qRT-PCR) analysis.

Results

The electrospun membranes were composed of beadless and homogeneous nanofibers, showing high porosity and interconnectivity (Figure 1A-C). PCL-CTS and PCL-CTS-ECM membranes showed similar mechanical properties, which were decreased compared to PCL (Figure 1D). PCL-CTS-ECM membranes significantly promoted cell proliferation in comparison to the other membranes (Figure 1E). *ALP*

and *COL I* gene expression exhibited a statistically significant increase in PCL-CTS-ECM membranes (Figure 1F).

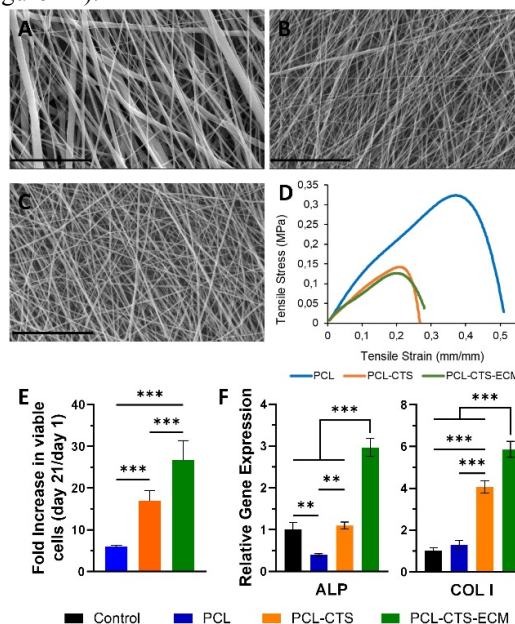


Figure 1: SEM images of PCL (A), PCL-CTS (B), and PCL-CTS-ECM (C) nanofibers. Scale bar: 8 μ m. Representative stress-strain curves (D). Fold increase (E) in the number of viable cells on day 21 (in relation to day 1). F: *ALP* and *COL I* gene expression by PDLSCs after 21 days of osteogenic differentiation on the electrospun membranes. Values are expressed as mean \pm SD ($N = 3$). ** $p < 0.01$ and *** $p < 0.001$.

Discussion

Our results show that dECM incorporation did not affect the membrane's properties, as loaded membranes maintained similar fiber morphology and mechanical properties of PCL-CTS membranes. PCL-CTS-ECM membranes promoted cell proliferation and enhanced the osteogenic differentiation of PDLSCs, confirmed by increased *ALP* and *COL I* gene expression, in comparison to PCL and PCL-CTS membranes, due to the presence of dECM. This work describes the use of lyophilized dECM to yield electrospun membranes with enhanced bioactivity for periodontal (TE) applications.

References

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