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# Unified plate finite elements for the large strain analysis of hyperelastic material structures

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**Abstract:** *This paper proposes a high-order two-dimensional (2D) finite element model for the analysis of isotropic, nearly incompressible hyperelastic material structures based on a decoupled neo-Hookean strain energy function. The model is based on the Carrera Unified Formulation (CUF), which allows to automatically implement different kinematics by using an opportune recursive notation. The principle of virtual work and a finite element approximation are exploited to obtain the nonlinear governing equations. Considering the three-dimensional full Green–Lagrange strain components and given the material Jacobian tensor, the explicit forms of tangent stiffness matrices of unified plate elements are presented in terms of the fundamental nuclei, which are independent of the theory approximation order. Several problems of soft material plates under uniform pressure are investigated, including a silicone rubber clamped plate and a simply supported plate made of biological material. The proposed model is compared with literature results including those coming from experiments and numerical solutions. The numerical investigation demonstrated the validity and accuracy of the proposed methodology for the analysis of hyperelastic plates.*

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## 1 Introduction

Structures made of hyperelastic soft materials are widely used in different engineering fields, from aerospace to biomedical. Some examples are represented by neurosurgery in the biomedical field [1], in the diagnosis of breast cancer by differentiating healthy tissues from diseased ones [2], and in the description of the behaviour of the arteries [3] [4]. In the mechanical and aerospace fields, hyperelastic materials are exploited to produce devices characterized by unique elastic properties, such as pressure sensors [5], optical composites used for optical transmittance [6], devices that exploit Soft Electroactive Materials (SEAM) for conversion of mechanical energy into electrical energy such as Wave Energy Converter (WEC) able to convert wave energy into electrical energy through a membrane of dielectric material [7] [8]. From a physical point of view, structures can undergo large deformations where the elastic constitutive equations lose validity. In addition, some structures have a very small linear region of the constitutive model, thus they have nonlinear behaviour.

In these years, researchers developed different strain energy function models to describe the strong nonlinear behaviour that this type of structures usually show during services. The

most used model is the Neo-Hookean one. It derives from the molecular theory that the measured material is modelled as a network of a long chain of molecules that are bound at a few points. Therefore, the elastic energy of the network will be the sum of the energies of the individual chains [9]. Another polynomial strain energy function is the Mooney-Rivlin model, described by Mooney and Rivlin expressed in terms of the Cauchy-Green deformation tensor invariants [10]. This model was used for describing the behaviour of biological porcine material like brain tissue [11]. The Ogden model was developed in 1972 [12] and it is mainly used today to fit brain tissue test data as described by Kaster [1]. The models previously described have polynomial forms of the strain energy functions. They are mainly used for biological tissue because of their simplicity. Instead, the Gent model has a logarithmic form and was proposed by Gent in 1996 [13]. This model reproduces accurately the behaviour of many new elastomeric and biological materials as studied by Horgan [14]. More details and other material models are described by Khaniki et al. [15]. In this work, considered problems refer to a Neo-Hookean model. The reference solution of Breslavsky is also obtained using a Neo-Hookean model [16] [17]. Instead, the reference solution of a silicone rubber plate by Amabili refers to a Mooney-Rivlin model [18]. It is important to employ an appropriate strain energy function to model the structures. In the work of Khaniki et al. [19] structures related to biological materials of the human body such as the brain, arteries, skeletal muscles, skin, adipose tissue, and problems related to polymeric structures in different mechanical conditions are investigated.

The nonlinear analysis of nearly incompressible hyperelastic materials presents some difficulties because the bulk modulus has orders of magnitude larger than the shear modulus. Among the main issues, there are instabilities and phenomena of locking. Many researchers have tried to overcome these shortcomings. For example, in the work of Sussman and Bathe [20] a finite element formulation was presented for the analysis with both geometrical and physical nonlinearities of compressible and incompressible solids. Babuška and Suri investigated Poisson locking using the standard formulation, also called the displacement formulation [21]. In Ref.[22], they also investigated shear and membrane locking when the thickness of the plate or shell is very small. Other works, however, considered mixed formulations such as that of Caylak and Mahnken [23]. Düster et al. [24] applied p-FEM to finite isotropic hyperelastic bodies. These last two works are mainly based on the method  $\bar{\mathbf{F}}$ , in which the deformation gradient is divided into two parts, isochoric and dilatational.

After discussing the issues related to the nonlinear analysis structures in hyperelastic material, it is important to develop simple and accurate models for 1D and 2D cases. Many works proposed these models. For example, Chen and Wang [25] developed a model where the Yeoh governing equations of a hyperelastic beam are shown using the principle of the minimum energy potential. In 2D case, both Chen [26] and Breslavsky [16] [17] analyzed the static behaviour of thin plates of Neo-Hookean and Mooney-Rivlin material. In addition, Amabili [18] studied the behaviour of a silicone plate and compared the solution with experimental data. The equations of motion have been obtained by a unified energy approach, and geometrical nonlinearities are modelled according to the Novozhilov nonlinear shell theory. Amabili et al [27] also developed a geometrically nonlinear theory for circular cylindrical shells made of incompressible hyperelastic materials using a 9-parameter higher-order theory. Verhelst et al [28] presented formulations of stretch-based material models for isogeometric Kirchhoff-Love shells. They verified formulations on invariant-based Neo-Hookean and Mooney-Rivlin models using several numerical benchmarks. A numerical solution technique, named as variational differential quadrature (VDQ), was adopted for the compressible nonlinear elasticity problems by Hassani et al. [29].

The present work aims at introducing a unified 2D element able to deal with the nonlinear analysis of hyperelastic materials. The model is built in the framework of the Carrera Unified Formulation (CUF) which allows for the development of a plate finite element (FE) with different kinematics, from low- to higher-order. The FE arrays are written in terms of fundamental nuclei, which are invariant of the theory approximation order, and therefore the equations can be written in the compact form [30] [31] [32]. Recently, CUF was introduced to deal with a one-dimensional finite element for the analysis of hyperelastic soft materials [33]. Here, the formulation is further extended to deal with hyperelastic plates. This paper is structured as follows: a description of hyperelastic materials models and strain energy function considered in Section 2; CUF and finite element method for 2D models in Section 3; governing equations in the unified form and Newton-Raphson method are described in Section 4; then, numerical results are discussed in Section 5; finally, the main conclusions are drawn.

## 2 Nearly incompressible isotropic hyperelastic materials

### 2.1 Strain energy function

In this paper, homogeneous materials are considered, thus  $\Psi$  only depends on  $\mathbf{F}$ . For isotropic hyperelastic materials, the strain energy function  $\Psi$  can be expressed in terms of principal stretches  $(\lambda_1, \lambda_2, \lambda_3)$ , which are the eigenvalues of the strain gradient tensor  $\mathbf{F}$ . Energy function  $\Psi$  can also be defined as a function of the invariants  $(I_1, I_2, I_3)$  of the right Cauchy-Green strain tensor, defined as follows:

$$\mathbf{C} = \mathbf{F}^T \mathbf{F}. \quad (1)$$

It is possible to write:

$$\Psi = \Psi(I_1, I_2, I_3) \quad (2)$$

where

$$\begin{aligned} I_1 &= \text{tr}(\mathbf{C}) \\ I_2 &= \frac{1}{2}(I_1^2 - \text{tr}(\mathbf{C}^2)) \\ I_3 &= \det(\mathbf{C}) \end{aligned} \quad (3)$$

and  $\text{tr}(\bullet)$  and  $\det(\bullet)$  represent the trace and determinant of a tensor, respectively.

In the case of a nearly incompressible model, the Jacobian determinant  $J = \det(\mathbf{F})$  represents the volume ratio, and hence the value of  $I_3$  is approximately equal to the unit.

With a thermodynamic similarity, as described by Flory [34], the tensor  $\mathbf{F}$  can be written by dividing it into two parts:  $\mathbf{F}_{\text{vol}} = J^{\frac{1}{3}} \mathbf{1}$  and  $\bar{\mathbf{F}} = J^{-\frac{1}{3}} \mathbf{F}$  representing the volumetric part, related to deformation, and the isochoric part, respectively. Introducing Eq.(1), it is possible to write  $\mathbf{C}_{\text{vol}} = J^{\frac{2}{3}} \mathbf{1}$  and  $\bar{\mathbf{C}} = J^{-\frac{2}{3}} \mathbf{C}$ , and to obtain  $\mathbf{C} = \mathbf{C}_{\text{vol}} \bar{\mathbf{C}}$ . Now, the strain energy function can be decoupled into its volumetric ( $U$ ) and isochoric ( $\bar{\Psi}$ ) part):

$$\Psi = U(J) + \bar{\Psi}(\bar{I}_1, \bar{I}_2) \quad (4)$$

The function  $U(J)$  acts as a penalty of incompressibility, and it must be strictly convex, twice differentiable and continuous [35]. In the literature, several formulas [36] exist to express such

a function, and in this work, we use the one proposed by Sussman and Bathe [20], where:

$$U(J) = \frac{1}{D_1}(J - 1)^2 \quad (5)$$

where  $D_1 = 2/k$  is the incompressibility material parameter and  $k$  is the bulk modulus.

In the literature, there are many definitions of the isochoric part of the strain energy function  $\bar{\Psi}$  [14] [37]. The most commonly used, often for biological materials, are classified with respect to the form of the equation, the number of strain invariants used and the ability to fit experimental data [9]. Polynomial forms of strain energy functions are the most used due to their simplicity and efficiency. In this paper, a Neo-Hookean model is used and the strain energy function is related only to the first invariant such that  $\bar{\Psi} = \bar{\Psi}(\bar{I}_1)$ . In particular, it assumes the following form:

$$\bar{\Psi}(\bar{I}_1) = \frac{\mu}{2} (\bar{I}_1 - 3) \quad (6)$$

where  $\mu$  is the shear modulus for infinitesimal deformations.

## 2.2 The Jacobian Tensor

The constitutive relation in its general form is represented by the second stress tensor Piola–Kirchhoff (PK-2) defined as:

$$\mathbf{S} = 2 \frac{\partial \Psi}{\partial \mathbf{C}} \quad (7)$$

Introducing Eq.(4) into Eq.(7), the PK-2 stress tensor can be written as the sum of a volumetric and an isochoric part:

$$\begin{aligned} \mathbf{S} &= \mathbf{S}^{\text{vol}} + \mathbf{S}^{\text{iso}} \\ \mathbf{S}^{\text{vol}} &= J p \mathbf{C}^{-1} \\ \mathbf{S}^{\text{iso}} &= 2 J^{-\frac{2}{3}} \frac{\partial \bar{\Psi}}{\partial \bar{I}_1} \left( \mathbf{1} - \frac{1}{3} \bar{I}_1 \mathbf{C}^{-1} \right) \end{aligned} \quad (8)$$

Where  $\mathbf{1}$  represents the unit matrix,  $\mathbf{C}^{-1}$  is the inverse of the Cauchy-Green tensor, and  $p = \frac{U}{J}$  is the hydrostatic pressure. The isochoric contribution  $\mathbf{S}_{iso}$  refers to hyperelastic models correlated to the first invariant.

Consider PK-2  $\mathbf{S}$  of one point at some time  $t$ . According to Holzapfel [38],  $\mathbf{S}$  can be evaluated as a function of a variable which can be assumed as  $\mathbf{C}$ . It is possible to write a linear relationship between the increments of  $\mathbf{S}$  and  $\mathbf{C}$ :

$$\Delta \mathbf{S} = \mathbf{c} \cdot \frac{1}{2} \Delta \mathbf{C} \quad (9)$$

where  $\mathbf{c}$  is the gradient of the function  $\mathbf{S}$ . This quantity is the fourth-order elasticity tensor (*Jacobian tensor*) and measures the change in stresses starting from the change in strain and is defined as:

$$\mathbf{c} = \frac{\partial \mathbf{S}}{\partial \mathbf{E}} = 2 \frac{\partial \mathbf{S}}{\partial \mathbf{C}} = 4 \frac{\partial^2 \Psi}{\partial \mathbf{C} \partial \mathbf{C}} \quad (10)$$

where  $\mathbf{E} = \frac{1}{2}(\mathbf{C} - \mathbf{1})$  is the Green–Lagrange strain tensor. Considering  $U = U(J)$  and  $\bar{\Psi} = \bar{\Psi}(\bar{I}_1)$  and introducing the Eqs.(8) and (10) it is possible to get the expression of the material Jacobian tensor:

$$\mathbf{c} = \mathbf{c}^{\text{vol}} + \mathbf{c}^{\text{iso}} \quad (11)$$

A detailed description is shown in [33] and [38].

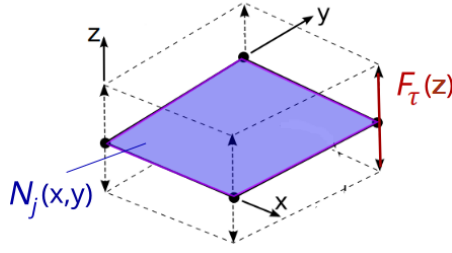


Figure 1: CUF-FEM configuration for plate model.

### 3 Two-dimensional finite elements

The two-dimensional (2D) model adopted in this work is based on the Carrera Unified Formulation (CUF)[30] [31]. CUF allows writing the equations of any refined theory 1D, 2D, or 3D in terms of a few fundamental nuclei FNs, whose shape does not depend on the assumptions used, such as type and order of the function, to describe the field of displacements.

Referring to Fig. 1, the three-dimensional (3D) displacement field  $\mathbf{U}(x, y, z)$  can be expressed as a product between a 2D in-plane shape function  $N_i(x, y)$  and 1D expansion function  $F_\tau(z)$ .

$$\mathbf{U}(x, y, z) = F_\tau(z)N_i(x, y)\mathbf{q}_{\tau i}, \quad \tau = 1, \dots, M \quad i = 1, \dots, p + 1 \quad (12)$$

where  $F_\tau(z)$  is the function of expansion along the thickness, with  $M$  equal to the number of terms of the expansion,  $q_{\tau i}$  are the discrete nodal displacements,  $N_i(x, y)$  are the 2D shape functions to use for the finite element method in the plane  $xy$  of the mean surface,  $p$  denotes the order of the shape functions and the repeated index  $i$  indicates summation. Note that the choice of the function  $F_\tau$  is made a priori and is completely arbitrary but its choice characterizes the model adopted. According to Pagani e Carrera [39], it is possible to write the Green-Lagrange strain vector as:

$$\mathbf{E} = (\mathbf{b}_l + \mathbf{b}_{nl})\mathbf{U} = (\mathbf{b}_l + \mathbf{b}_{nl})F_\tau(z)N_i(x, y)\mathbf{q}_{\tau i} = (\mathbf{B}_l^{\tau i} + \mathbf{B}_{nl}^{\tau i})\mathbf{q}_{\tau i} \quad (13)$$

where  $\mathbf{B}_l^{\tau j}$  and  $\mathbf{B}_{nl}^{\tau j}$  are the matrices of derivative operators applied to the form functions in the linear and nonlinear case, respectively. In this paper, Lagrange Expansion (LE) models are used as expansion functions  $F_\tau(z)$ . For simplicity, the considered plate theories are indicated by the acronym LDN, which represents the Layer-wise Displacement-based theory with the order of expansion  $N$  [32]. Specifically, the two-node linear (LD1) and three-node quadratic (LD2) have been developed along the thickness of plates. For 2D in-plane shape functions  $N_i(x, y)$ , four-node bilinear (Q4) and nine-node quadratic (Q9) have been adopted. Note that the choice of discretization along the thickness is independent of the choice of discretization in the  $xy$  plane.

## 4 Governing equations

### 4.1 Tangent stiffness matrix

In this section, the tangent stiffness matrix is defined. It is used in the iterations of Newton-Raphson method. Starting from the CUF-FEM formulation and considering a generic expansion for a 2D element, it is possible to define the tangent stiffness matrix for hyperelastic

materials. As already described, the strain vector can be written in terms of the unknowns generalized nodal displacements. In this case,  $\mathbf{E}$  is the strain vector derived from the Green-Lagrange strain tensor and  $\mathbf{U}_{\tau i}$  is the nodal virtual displacements. Therefore, it is possible to write:

$$\mathbf{E} = (\mathbf{b}_l + \mathbf{b}_{nl})\mathbf{u} = (\mathbf{b}_l + \mathbf{b}_{nl})F_\tau(x, z)N_i(y)\mathbf{U}_{\tau i} = (\mathbf{B}_l^{\tau i} + \mathbf{B}_{nl}^{\tau i})\mathbf{U}_{\tau i} \quad (14)$$

Then the virtual variation is:

$$\delta\mathbf{E} = \delta((\mathbf{B}_l^{\tau i} + \mathbf{B}_{nl}^{\tau i})\mathbf{U}_{s j}) = (\mathbf{B}_l^{s j} + 2\mathbf{B}_{nl}^{s j})\delta\mathbf{U}_{s j} \quad (15)$$

where indexes  $\tau$  and  $i$  have been respectively substituted with  $s$  and  $j$  for sake of convenience. The equilibrium equation must be linearized to obtain the expression of the fundamental nuclei of the tangent stiffness matrix.

$$\delta(\delta L_{int}) = \int_{\Omega} \delta(\delta\mathbf{E}^T \mathbf{S})dV = \int_{\Omega} \delta\mathbf{E}^T \delta\mathbf{S}dV + \int_{\Omega} \delta(\delta\mathbf{E}^T) \mathbf{S}dV \quad (16)$$

The first right-hand side term corresponds to the linearization of the constitutive equation of hyperelastic materials. Holzapfel [38] adopted the formulation with first invariant:

$$\delta\mathbf{S} = \mathbf{C} \frac{1}{2} \delta\mathbf{C} = \mathbf{C} \delta\mathbf{E} = \mathbf{C}(\mathbf{B}_l^{s j} + 2\mathbf{B}_{nl}^{s j})\delta\mathbf{U}_{\tau i} \quad (17)$$

where  $\mathbf{C}$  represents the tangent fourth-order elasticity tensor described in previous section. It is possible to write the linearization of the constitutive law in a weak form:

$$\begin{aligned} \int_{\Omega} \delta\mathbf{E}^T \delta\mathbf{S}dV &= \int_{\Omega} \delta\mathbf{U}_{s j}^T (\mathbf{B}_l^{s j} + 2\mathbf{B}_{nl}^{s j})^T \mathbf{C} ((\mathbf{B}_l^{\tau i} + 2\mathbf{B}_{nl}^{\tau i})\delta\mathbf{U}_{\tau i})dV \\ &= \delta\mathbf{U}_{s j}^T \left[ \int_{\Omega} \mathbf{B}_l^{s j T} \mathbf{C} \mathbf{B}_l^{\tau i} dV \right] \delta\mathbf{U}_{\tau i} + \delta\mathbf{U}_{s j}^T \left[ 2 \int_{\Omega} \mathbf{B}_l^{s j T} \mathbf{C} \mathbf{B}_{nl}^{\tau i} dV \right] \delta\mathbf{U}_{\tau i} + \\ &+ \delta\mathbf{U}_{s j}^T \left[ 2 \int_{\Omega} \mathbf{B}_{nl}^{s j T} \mathbf{C} \mathbf{B}_l^{\tau i} dV \right] \delta\mathbf{U}_{\tau i} + \delta\mathbf{U}_{s j}^T \left[ \int_{\Omega} 2\mathbf{B}_l^{s j T} \mathbf{C} 2\mathbf{B}_l^{\tau i} dV \right] \delta\mathbf{U}_{\tau i} \end{aligned} \quad (18)$$

Four contributions of 3x3 matrices are defined:

$$\begin{aligned} \mathbf{K}_{ll}^{ij\tau s} &= \int_{\Omega} \mathbf{B}_l^{s j T} \mathbf{C} \mathbf{B}_l^{\tau i} dV \\ \mathbf{K}_{lnl}^{ij\tau s} &= \int_{\Omega} \mathbf{B}_l^{s j T} \mathbf{C} \mathbf{B}_{nl}^{\tau i} dV \\ \mathbf{K}_{nll}^{ij\tau s} &= \int_{\Omega} 2\mathbf{B}_{nl}^{s j T} \mathbf{C} \mathbf{B}_l^{\tau i} dV \\ \mathbf{K}_{nlnl}^{ij\tau s} &= \int_{\Omega} 2\mathbf{B}_l^{s j T} \mathbf{C} 2\mathbf{B}_l^{\tau i} dV \end{aligned} \quad (19)$$

where  $\mathbf{K}_{T_1}^{ij\tau s} = 2\mathbf{K}_{lnl}^{ij\tau s} + \mathbf{K}_{nll}^{ij\tau s} + 2\mathbf{K}_{nlnl}^{ij\tau s}$  is the nonlinear contribution of the tangent stiffness matrix. It is possible to rewrite the linearized constitutive equation as:

$$\int_{\Omega} \delta\mathbf{E}^T \delta\mathbf{S}dV = \delta\mathbf{U}_{s j}^T \mathbf{K}_{ll}^{ij\tau s} \delta\mathbf{U}_{\tau i} + \delta\mathbf{U}_{s j}^T \mathbf{K}_{T_1}^{ij\tau s} \delta\mathbf{U}_{\tau i} \quad (20)$$

The second right-hand side term of the equation (16) corresponds to the linearization of geometric equations. Once the matrix of differential operators  $\mathbf{B}_{nl}^*$  and the virtual variation of the deformations have been defined:

$$\delta(\delta\mathbf{E}) = \mathbf{B}_{nl}^* \left\{ \begin{array}{c} \delta U_{x_{\tau i}} \delta U_{x_{sj}} \\ \delta U_{y_{\tau i}} \delta U_{y_{sj}} \\ \delta U_{z_{\tau i}} \delta U_{z_{sj}} \end{array} \right\} \quad (21)$$

The second term becomes:

$$\begin{aligned} \int_{\Omega} \delta(\delta\mathbf{E}^T) \mathbf{S} dV &= \int_{\Omega} \left\{ \begin{array}{c} \delta U_{x_{\tau i}} \delta U_{x_{sj}} \\ \delta U_{y_{\tau i}} \delta U_{y_{sj}} \\ \delta U_{z_{\tau i}} \delta U_{z_{sj}} \end{array} \right\} (\mathbf{B}_{nl}^*)^T \mathbf{S} dV \\ &= \int_{\Omega} \delta \mathbf{U}_{sj}^T \text{diag}((\mathbf{B}_{nl}^*)^T \mathbf{S}) \delta \mathbf{U}_{\tau i} dV \\ &= \delta \mathbf{U}_{sj}^T \mathbf{K}_{\sigma}^{ij\tau s} \delta \mathbf{U}_{\tau i} \end{aligned} \quad (22)$$

where  $\mathbf{K}_{\sigma}^{ij\tau s}$  is the geometric stiffness matrix and derives from the linearization of the non-linear displacement-strain relationship.

Then, substituting the different quantities in the Eq. (16), it is possible to obtain the fundamental nuclei of the tangent stiffness matrix as the sum of the linear, nonlinear and geometric contribution:

$$\delta(\delta L_{int}) = \delta \mathbf{U}_{sj}^T \mathbf{K}_{ll}^{ij\tau s} \delta \mathbf{U}_{\tau i} + \delta \mathbf{U}_{sj}^T \mathbf{K}_{T_1}^{ij\tau s} \delta \mathbf{U}_{\tau i} + \delta \mathbf{U}_{sj}^T \mathbf{K}_{\sigma}^{ij\tau s} \delta \mathbf{U}_{\tau i} = \delta \mathbf{U}_{sj}^T \mathbf{K}_T^{ij\tau s} \delta \mathbf{U}_{\tau i} \quad (23)$$

## 4.2 Internal force vector

Starting from the Eq. (15), the principle of virtual works establishes that:

$$\delta L_{int} - \delta L_{est} = 0 \quad (24)$$

Considering the Green-Lagrange strain  $\mathbf{E}$  and stress tensors PK2  $\mathbf{S}$ , the virtual variation of the work of the internal forces can be expressed as:

$$\delta L_{int} = \int_{\Omega} \delta \mathbf{E}^T \mathbf{S} dV \quad (25)$$

Now, adopting the same definition of generalized deformations and its virtual variation:

$$\delta \mathbf{E} = \delta((\mathbf{B}_l^{\tau i} + \mathbf{B}_{nl}^{\tau i}) \mathbf{U}_{\tau i}) \mathbf{U}_{sj} = (\mathbf{B}_l^{sj} + 2\mathbf{B}_{nl}^{sj}) \delta \mathbf{U}_{sj} \quad (26)$$

Substituting it in Eq. (25), it is possible to write:

$$\delta L_{int} = \int_{\Omega} \delta \mathbf{E}^T \mathbf{S} dV = \int_{\Omega} \delta \mathbf{U}_{sj}^T (\mathbf{B}_l^{sj} + 2\mathbf{B}_{nl}^{sj}) \mathbf{S} dV = \delta \mathbf{U}_{sj}^T \mathbf{F}_{int}^{sj} \quad (27)$$

The fundamental nuclei of the internal forces vector are obtained:

$$\mathbf{F}_{int}^{sj} = \int_{\Omega} (\mathbf{B}_l^{sj} + 2\mathbf{B}_{nl}^{sj}) \mathbf{S} dV \quad (28)$$



The FN of the external load vector is derived from the definition of 2D CUF-FEM. Considering  $p$  the vector of conservative loads, it is possible to write the virtual variation of the work done by external forces as:

$$\delta L_{\text{est}} = \int_{\Omega} \delta \mathbf{U}^T \mathbf{p} dV = \int_{\Omega} \mathbf{q}_{sj}^T F_s(z) N_j(x, y) \mathbf{p} dV = \mathbf{q}_{sj}^T \mathbf{p}_{sj} \quad (29)$$

Substituting in Eq. (24) and assembling the final structure, nonlinear algebraic equations are rewritten as:

$$\delta \mathbf{U} : \quad \mathbf{F}_{\text{int}} - \mathbf{F}_{\text{ext}} = 0 \quad (30)$$

Nonlinear equations are solved using the Newton-Raphson linearization. The vector of residual nodal forces  $\boldsymbol{\varphi}_{\text{res}}$  can be linearized by Taylor series expansion introducing the tangent stiffness matrix  $\mathbf{K}_T$ . It is necessary to introduce a constraint relation to solve the equations. Different incremental schemes can be implemented using different constraint equation. A more detailed description of Newton-Raphson method is provided in Ref. [39]. In particular, the *arc-length* method provides a solution for nonlinear problems when critical points are present. This method is accurately described by Crisfield [40].

## 5 Numerical results

In this paper, three study cases taken from literature are analyzed with the proposed 2D unified models:

- the first case refers to a simply supported square plate analyzed with general Neo-Hookean material model and biological material model;
- the second case deals with a simply supported rectangular plate considering at first geometrical nonlinearities and then geometrical and physical nonlinearities;
- the last case refers to a clamped silicone rubber plate under uniform pressure.

All the cases consider to plates under pressure. A Neo-Hookean nearly incompressible material has been adopted.

### 5.1 Thin hyperelastic plate under pressure

The first case was considered by Breslavsky et al. in [17] using a incompressible model ( $\nu = 0.5$ ). The same problem was analyzed by Ansari et al. in [41] considering a nearly incompressible model. A simply supported plate is considered with  $a = b = 0.1 \text{ m}$ ,  $h = 5 \times 10^{-4} \text{ m}$  and it is subjected to uniform pressure with the following boundary conditions, Fig. 2:

$$w|_{\delta S} = M|_{\delta S} = u|_{\delta S} = v|_{\delta S} = 0 \quad (31)$$

where  $\delta S$  is the boundary plate.

In this work, we considered the nearly incompressible Neo-Hookean model with material parameters present in Table 1. In the  $xy$  plane, we used a number of elements of  $8 \times 8$ ,  $10 \times 10$  with four-nodes (Q4) and  $10 \times 10$ ,  $16 \times 16$  with nine-nodes (Q9). Along the thickness, however, it was sufficient to use a three-node quadratic Lagrangian expansion function (LD2) to obtain the accuracy of the solution. As shown in Fig. 3, for a few elements (in this case  $8 \times 8$  Q4) the solution is not very accurate. Increasing the number of elements, however, the

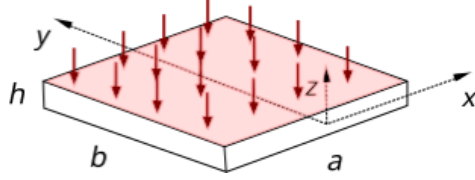


Figure 2: Thin hyperelastic plate geometry under pressure.

$E$	1247060.2 Pa
$\nu$	0.4999
$\mu$	415714.45 Pa
$D_1 = 2/k$	$9.6226 \times 10^{-10} \text{ Pa}^{-1}$

Table 1: Material parameters of thin hyperelastic plate. Neo-Hookean model adopted.

solution tends to coincide with the 27 degrees of freedom (DOF) Breslavsky solution obtained by the local model method, where the total number of degree of freedom DOF is given by  $N = N_W + N_U + N_V$  [17]. Table 2 shows the centre point deformation values for the different discretization models used and for different load steps. As it is possible to see from the graph, the convergence is achieved for a  $10 \times 10$  Q9 mesh. Using the nearly incompressible model with  $\nu = 0.4999$ , it is possible to notice that it is almost coincident with the incompressible case. They are practically coincident for small deformations.

## 5.2 Hyperelastic plate made of biological material

This case is also discussed by Breslavsky in [17]. The plate has the same dimensions and boundary conditions as in the previous example. The properties of the material are in [4]. A Neo-Hookean material model is considered with Young modulus  $E = 59383.2 \text{ Pa}$  and it is considered the nearly incompressible material condition with  $\nu = 0.4999$ .

For convergence analysis, 4-node Q4 elements were used in the  $xy$  plane and a 3-node quadratic Lagrangian expansion (LD2) along the thickness. Various discretizations have been tested. From Fig. 4 it is possible to see that a small number of elements is already sufficient to obtain an accurate solution. Moreover, even if it was used a nearly incompressibility condition, the solution obtained is close to the solution of incompressible material (for small

$p[kPa]$	$w/h$			Ref [17]
	$8 \times 8Q4$	$10 \times 10Q4$	$10 \times 10Q9$	
0.029	6.848	9.030	9.043	10.109
0.285	17.741	19.318	19.226	20.132
1.917	37.642	38.912	39.192	39.980
4.292	54.337	55.052	56.075	57.020
8.019	76.571	76.935	78.601	80.032
10.476	91.047	91.854	93.243	94.984

Table 2: Deflection measured at the center of the thin hyperelastic plate for different FEM models. Comparison with 27 DOF solution in [17].

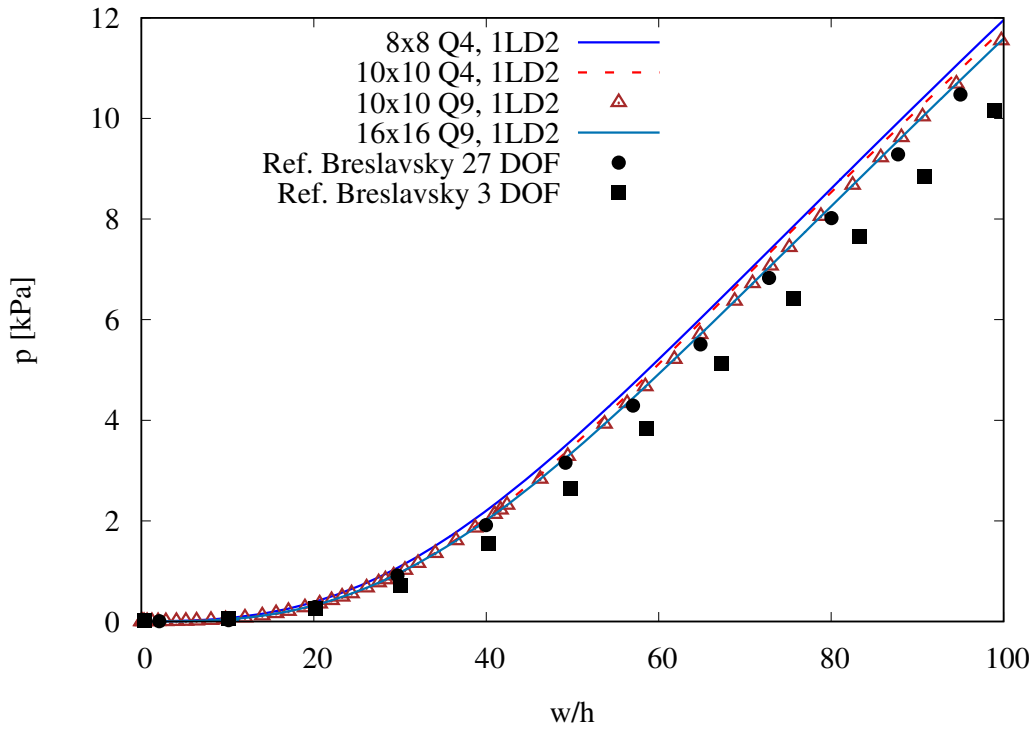


Figure 3: Neo-Hookean plate pressure–deflection response. Deflection measured at the centre of the plate and normalized with respect to the plate thickness  $h$ . Comparison between different FEM models and solution with 27 DOF and 3 DOF of Breslavsky [17].

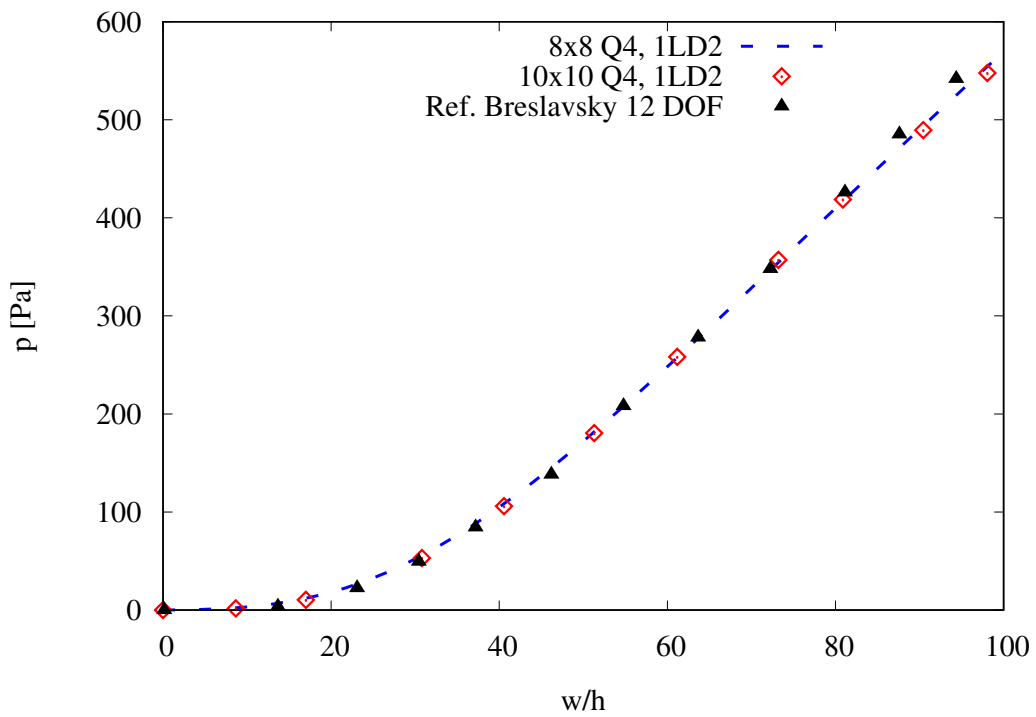


Figure 4: Pressure load–middle point deflection response of the biological material plate. Comparison between two different numbers of element and solution with 12 DOF of Breslavsky [17].

$p[Pa]$	$w/h$		
	$8 \times 8 Q4$	$10 \times 10 Q4$	Ref. [17]
3.83	11.21	12.09	13.67
84.64	36.41	36.93	37.21
208.51	54.83	54.83	54.83
426.39	81.66	82.03	81.20
542.14	96.46	97.11	94.27
568.45	99.69	100.50	98.33

Table 3: Middle point deflection of the biological material plate with mesh  $8 \times 8 Q4$ ,  $10 \times 10 Q4$  and Breslavsky’s solution with 12 DOF [17] for various load levels.

deformations it is nearly coincident) as shown in Table 3.

### 5.3 Rectangular plate: comparison between geometrical nonlinearities and geometrical and physical nonlinearities

The second example analyzed is a simply supported rectangular plate, always subject to uniform pressure. In this case, the plate has the following dimensions:  $a = 0.1 m$ ,  $b = 0.12 m$  and  $h = 5 \times 10^{-4} mm$ . The material properties considered are  $E = 10^7 Pa$  and  $\nu = 0.4999$ . The nearly incompressible material is considered. The analyzed case is taken from Breslavsky et al. [16], where the incompressible model ( $\nu = 0.5$ ) is used. For convergence analysis, a discretized model in the  $xy$  plane with  $12 \times 10$  elements both Q4 and Q9 is investigated. From Fig. 5, the discretized model with nine-node elements presents a more accurate solution than four-nodes elements solution. In Fig. 6, another convergence analysis is investigated. The solutions with nine-nodes element Q9 and a different number of elements ( $6 \times 5$  and  $12 \times 10$ ) are compared considering  $\nu = 0.4999$ . Note that a  $6 \times 5 Q9$  mesh is already accurate enough to describe the behaviour of the plate made from material with almost incompressible Neo-Hookean condition. Finally, the model with  $12 \times 10 Q9$  is assessed. The solution obtained considering only geometrical nonlinearities is compared with the solution obtained with both geometrical and physical ones. In Fig. 7, the solutions are similar to Breslavsky’s solutions. In Fig. 8, undeformed configuration and deformed configuration with  $p = 1.715, 8.694, 30.407 kPa$  are shown. In addition, it is possible to see that a 3-node (quadratic) discretization model along the thickness is sufficient to obtain the accuracy of the results. Note that the solutions of the nearly incompressible are similar to the incompressible case and they coincide for small deformations.

### 5.4 Silicone rubber plate

The last case under examination is taken from Amabili et al. [18]. In Fig. 9, a clamped plate with  $a = b = 0.26 m$  and thickness  $h = 1.5 \times 10^{-3} m$  is shown. The silicone rubber plate is under aerostatic pressure and it has been investigated analytically, numerically, and experimentally, as shown in Fig. 10. The plate has the following boundary conditions:

$$w|_{\partial\Omega} = \frac{\partial w}{\partial \mathbf{n}}|_{\partial\Omega} = u|_{\partial\Omega} = v|_{\partial\Omega} = 0 \quad (32)$$

where  $\partial\Omega$  is the plate’s middle surface boundary and  $\mathbf{n}$  is the normal to  $\partial\Omega$  lying on the plate surface. In order to compare the experimental data with the numerical solution, the material

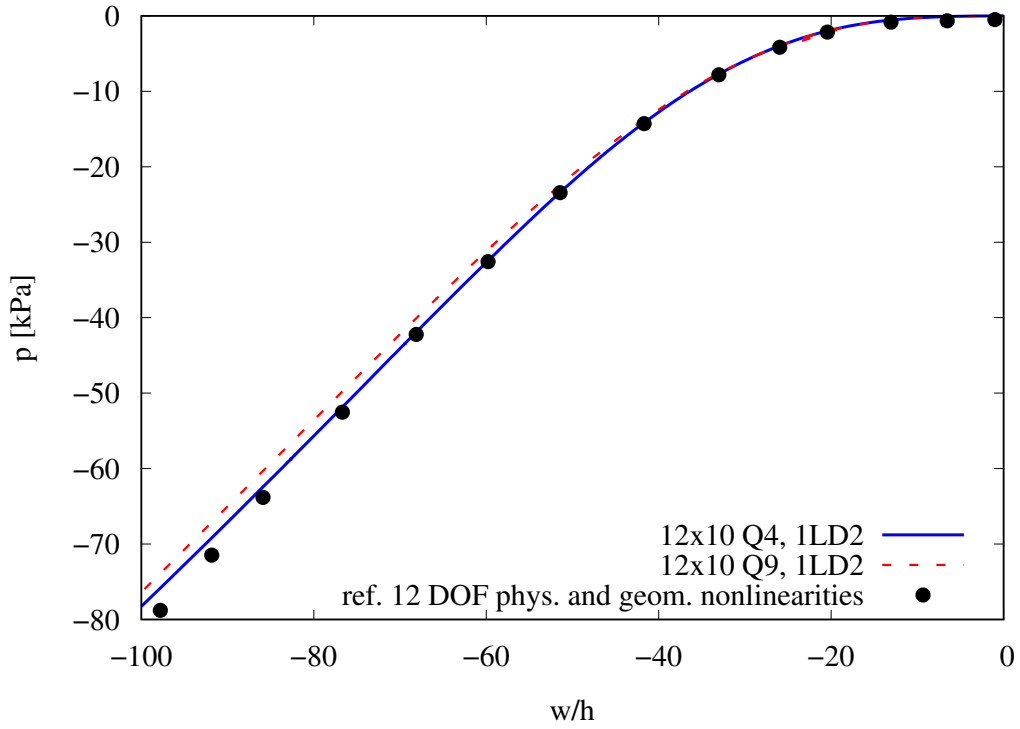


Figure 5: Middle point deflection-pressure curves for models with geometrical and physical nonlinearities . Comparison between two different models  $12 \times 10$  Q4,  $12 \times 10$  Q9 and solution with 12 DOF of Breslavsky [16].

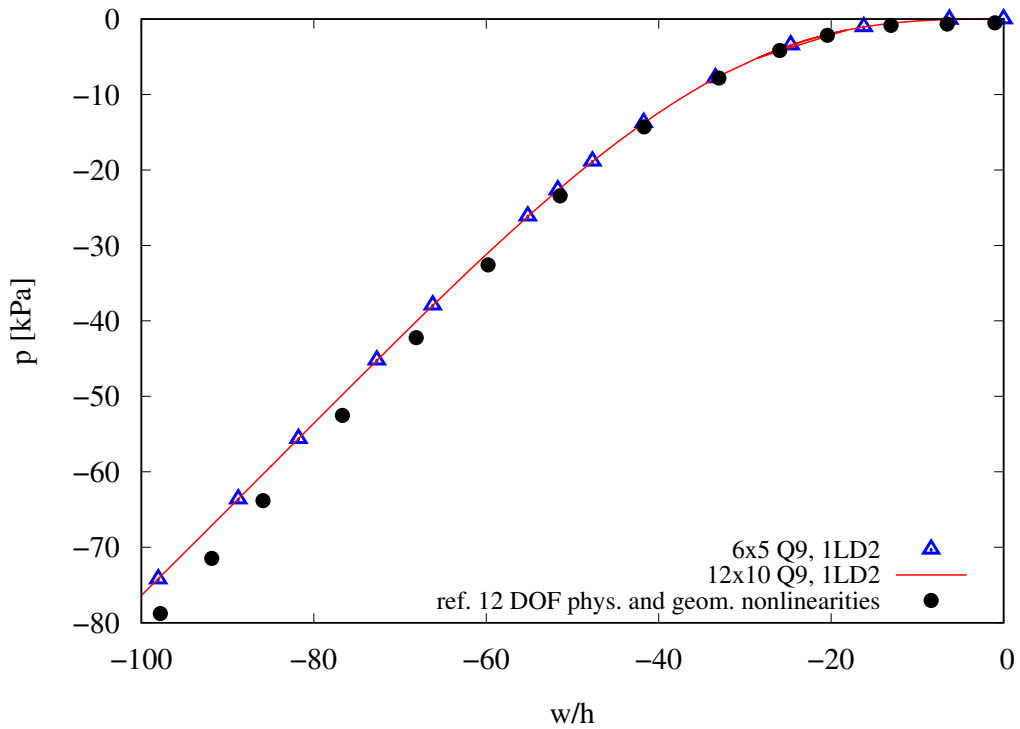


Figure 6: Middle point deflection-pressure curves for models with geometrical and physical nonlinearity . Comparison between  $6 \times 5$  Q9,  $12 \times 10$  Q9 and solution with 12 DOF of Breslavsky [16].

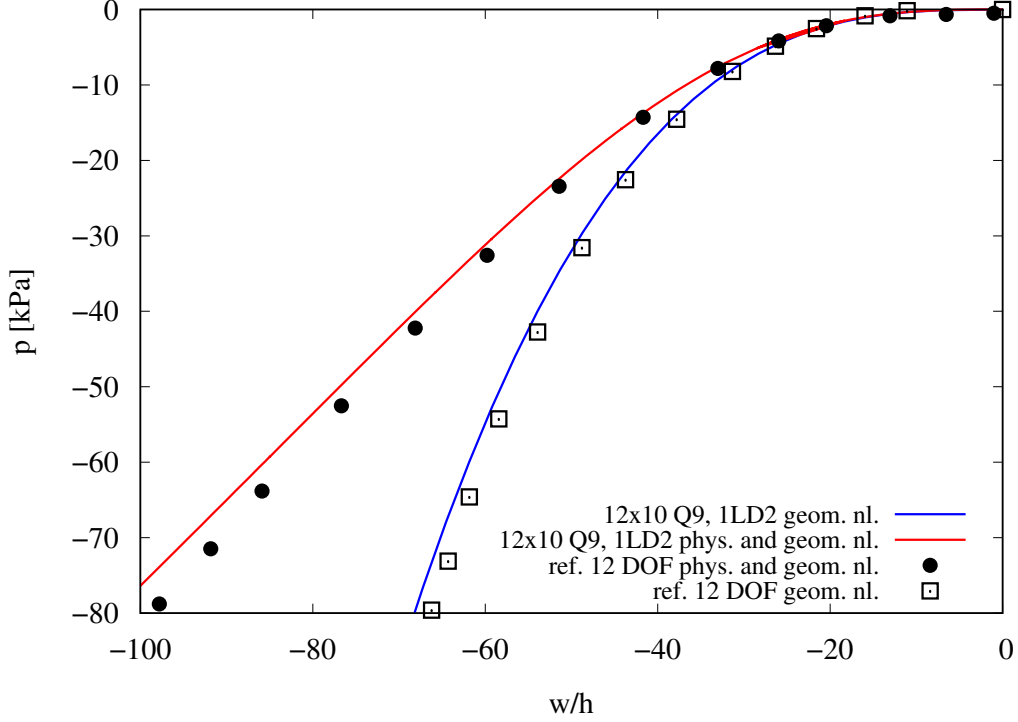


Figure 7: Middle point deflection-pressure curves for  $12 \times 10$  Q9 model and  $\nu = 0.4999$ . Comparison between solution with geometrical nonlinearities only and solution with both geometrical and physical nonlinearities. Comparison with 12 DOF Breslavsky's solution [16].

$\nu$	0.4999
$\mu$	$1.448 \times 10^6 \text{ Pa}$
$D_1 = 2/k$	$2.762 \times 10^{-10} \text{ Pa}^{-1}$

Table 4: Material parameters of silicone rubber clamped plate (see Fig. 1 and Fig. 10) and subjected to uniform transverse pressure.

parameters are obtained by a fitting procedure on the results of the uniaxial tension test. In [18], Amabili considered a Mooney-Rivlin material model with elastic strain energy function as  $\bar{\Psi} = C_{10}(\bar{I}_1 - 3) + C_{01}(\bar{I}_2 - 3)$ , where the two material parameters are  $C_{10} = 253216 \text{ Pa}$  and  $C_{01} = 470900 \text{ Pa}$ . In this paper, however, it is used a model of Neo-Hookean material dependent only on the first invariant, which is a special case of Mooney-Rivlin material [20]. Material parameters in Table 4 are considered where  $\mu$  is the shear modulus,  $\nu$  is the Poisson coefficient,  $D_1$  is the material incompressibility parameter. Therefore, it was considered an almost incompressible model and it will be compared with the solution obtained by Amabili in the incompressible case ( $\nu = 0.5$ ). For the convergence analysis, 4-node elements (Q4) and a different number of elements were used in the  $xy$  plane:  $8 \times 8$ ,  $10 \times 10$ ,  $14 \times 14$ ,  $18 \times 18$ . Along the thickness, however, three-nodes are sufficient for the accuracy of the solution. As shown in Fig. 11 and Table 5, the configuration with fewer degrees of freedom stands between the reference numerical solution, where a  $20 \times 20$  mesh was used, and the experimental solution. For the nearly incompressible Neo-Hookean model considered in this paper, the convergence is achieved with a  $14 \times 14$  Q4 model and a quadratic Lagrange expansion function (LD2) along the thickness. The solution is practically coincident with the experimental solution in the

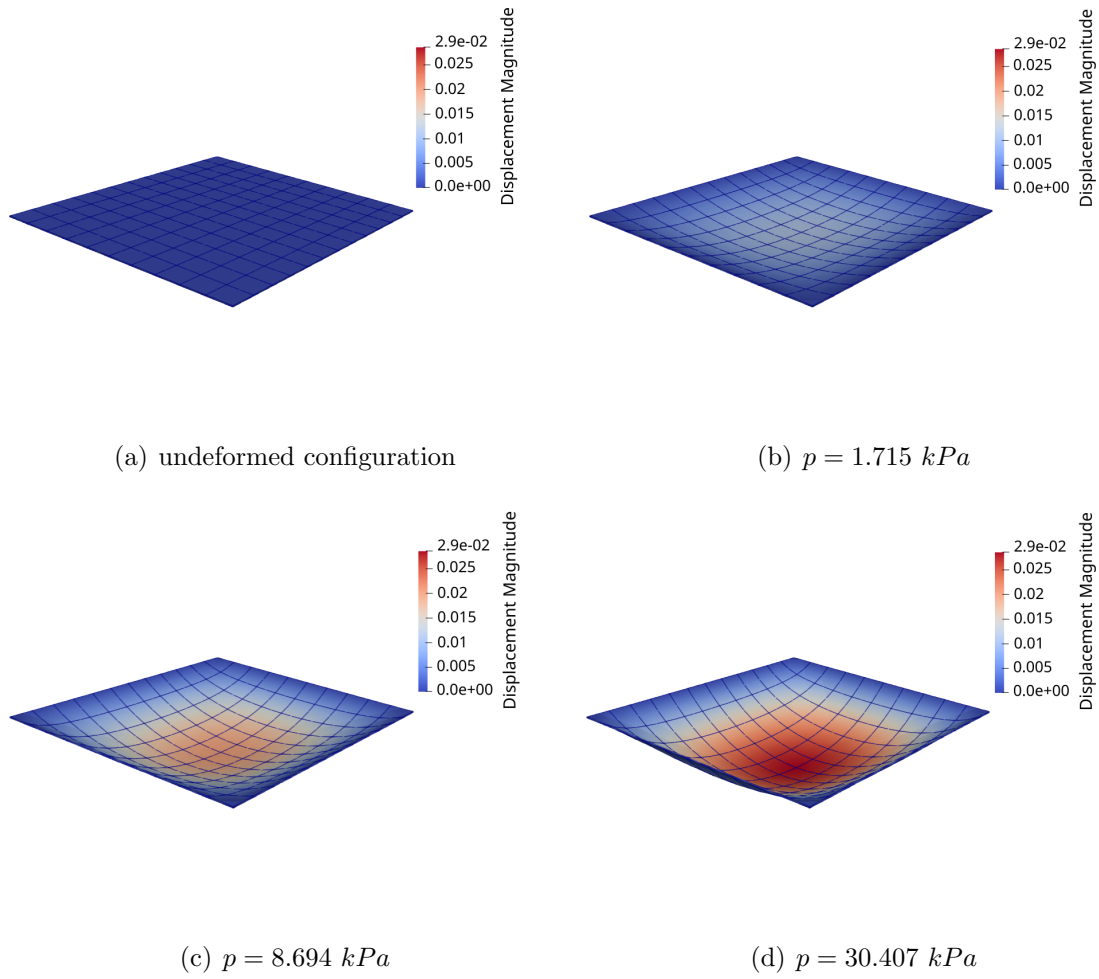


Figure 8: Undeformed and deformed states of the simply supported rectangular plate.  $12 \times 10$  Q9 model.

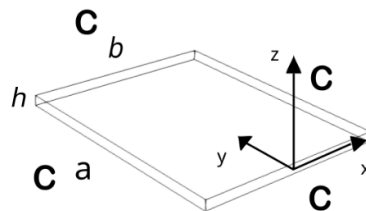


Figure 9: Boundary condition and geometry of the silicone rubber plate.

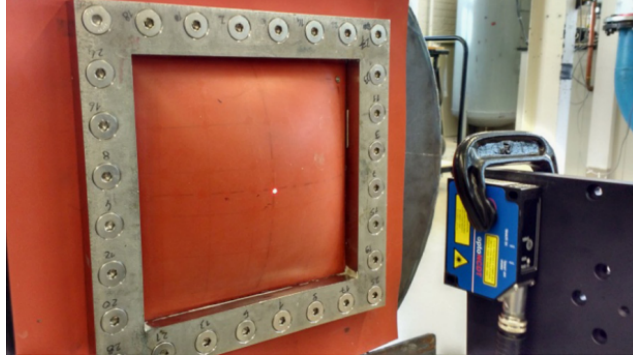


Figure 10: Silicone rubber plate under a pressure of 1 Psi. The deflection at the centre point is measured using a Micro-Epsilon triangulation laser sensor [18]. Adapted from [18] with permission from Elsevier.

$p[Psi]$	$w/h$			Ref. FEM	Ref. exp.
	$8 \times 8Q4$	$10 \times 10Q4$	$14 \times 14Q4$		
0.204	17.06	19.41	20.74	21.43	15.74
0.604	33.30	35.22	35.89	35.22	30.77
0.800	38.66	40.63	40.97	39.43	35.77
1.204	47.18	49.06	49.71	47.18	44.44
1.994	60.60	62.38	63.40	61.17	60.04

Table 5: Pressure-deformation values of the central point of the plate  $w/h$  for different mesh. Comparison with the reference solution in [18] of both FEM analysis and measured experimental data.



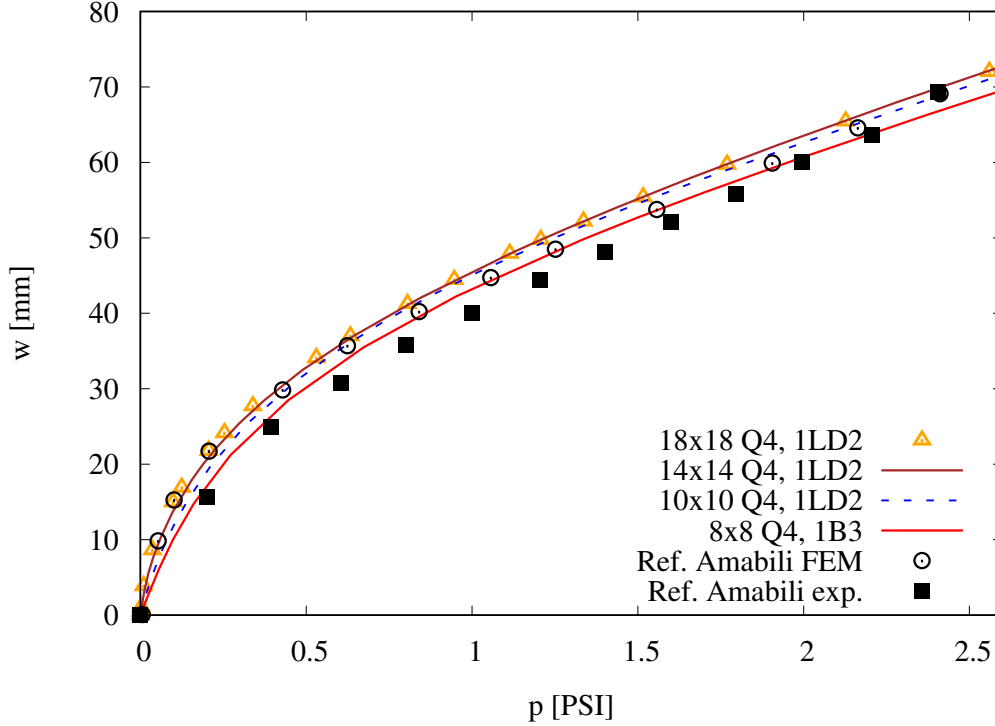


Figure 11: Static deflection of the silicone plate measured at the centre as function of the pressure. Comparison between different FEM models and experimental and FEM solutions of Amabili *et al* [18].

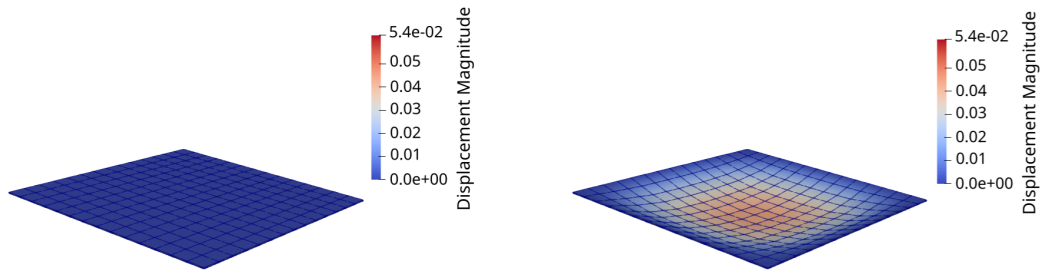
case of small deformations, while for displacements  $w > 35 \text{ mm}$  the solution slightly deviates from the FEM analysis carried out in [18]. Figure 12 shows the underformed and deformed states of the plate under two different load conditions.

## 6 Conclusions

This paper discussed two-dimensional (2D) high-order finite elements for the analysis of first-invariant hyperelastic Neo-Hookean plates. According to the Carrera Unified Formulation (CUF), it is possible to write the governing equations in terms of a few fundamental nuclei (FNs), which are invariant of the theory approximation order. Different problems were considered and the effect of the theory approximation order on the convergence and the accuracy of the solutions is studied in detail. The numerical investigation has demonstrated:

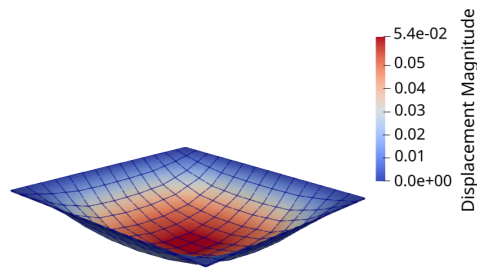
- the validity and accuracy of the theory provided for plates with both geometrical and physical nonlinearities considering a nearly-incompressible Neo-Hookean model.
- the accuracy of the CUF-FEM methodology compared with experimental data for a clamped silicone rubber plate.
- a model with a three-node quadratic Lagrange expansion along the thickness correctly described the large deflection of thin plates under uniform pressure.
- higher order model can help to overcome locking phenomena.

The research conducted provides enough confidence for future developments in this direction.



(a) undeformed configuration

(b)  $p = 1.200 \text{ psi}$



(c)  $p = 2.281 \text{ psi}$

Figure 12: Undeformed and deformed states of the silicone rubber plate.

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